

An Insight Software Consortium Tutorial: Medical Image Analysis with ITK and Related Open-Source Software

<http://www.InsightSoftwareConsortium.org>

This course introduces attendees to select open-source efforts in the field of medical image analysis. Opportunities for users and developers are presented.

The course particularly focuses on the open-source Insight Toolkit (ITK) for medical image segmentation and registration. The course describes the procedure for downloading and installing the toolkit and covers the use of its data representation and filtering classes. Attendees are shown how ITK can be used in their research, rapid prototyping, and application development.

LEARNING OUTCOMES

After completing this course, attendees will be able to:

- contribute to and benefit from open-source software for medical image analysis
- download and install the ITK toolkit
- start their own software project based on ITK
- design and construct an image processing pipeline
- combine ITK filters for medical image segmentation
- combine ITK components for medical image registration

INTENDED AUDIENCE

This course is intended for anyone involved in medical image analysis. In particular it targets graduate students, researchers and professionals in the areas of computer science and medicine. Attendees should have an intermediate level on object oriented programming with C++ and must be familiar with the basics of medical image processing and analysis.

COURSE LEVEL

Intermediate

COURSE LENGTH

Full-day (6.5 Hours)

COURSE OUTLINE

- 1) The Insight Software Consortium: contributing and using open-source
- 2) The architecture and installation of the Insight Toolkit
- 3) Segmentation methods of the Insight Toolkit
- 4) Registration methods of the Insight Toolkit
- 5) Image IO using the Insight Toolkit
- 6) The Image-Guided Surgery Toolkit: architecture overview
- 7) Using the Insight Toolkit with TK/TCL
- 8) Applications of the Insight Toolkit:
VTK/ITK, The Virtual Soldier, Industrial Research and NA-MIC's Slicer

CONTRIBUTORS

Many people contributed to the development of these presentations. The ISC is grateful to those peoples' support of open source software and education. Major contributors include the following:

Stephen Aylward is Chief Medical Scientist at Kitware, Inc. He joined Kitware in December 2005, after serving as a tenured Associate Professor of Radiology, Computer Science, and Surgery at the University of North Carolina at Chapel Hill. At Kitware, Stephen is working with leaders in the open-source movement on research and development for clinical image analysis software. Dr.

Aylward is also President of the Insight Software Consortium and an associate editor of IEEE Transactions on Medical Imaging. He has computer science degrees from Purdue (BS), Georgia Institute of Technology (MS), and UNC (PhD).

Luis Ibanez is a Research Engineer at Kitware, Inc. He received a BSc in Physics in 1989 and a MSc in Optics in 1994 from the Universidad Industrial de Santander (Bucaramanga, Colombia). He received a PhD in 2000 from the Universite de Rennes I (Rennes, France). From 1999 to 2001 he was Research Assistant Professor in the Division of Neurosurgery at the University of North Carolina at Chapel Hill. His current research interest the application of genomics paradigms to computation.

Josh Cates is a member of the research staff of the Scientific Computing and Imaging Institute at the University of Utah's School of Computer Science. He received his BS degree in Biology in 1995 and MS in Computer Science in 1999 from the University of Tennessee. His interests include software engineering and problems in computer vision, including image processing (differential geometry and p.d.e.-based methods), image segmentation, and computed tomography.

Lydia Ng is a member of the Informatics group at the Allen Institute for Brain Science. She received a BE in Electrical Engineering and a BSc in Computer Science in 1994 from The University of New South Wales (Sydney, Australia). She received a Ph.D. in 2000 from Macquarie University (Sydney, Australia). Her research interests include: image registration, PDE based image processing methods, motion estimation and development of software for medical image processing and analysis.

Julien Jomier is a research member at Kitware, Inc. He joined Kitware in December, 2005 after being a research faculty member in the Computer-Aided Diagnosis and Display Laboratory at the University of North Carolina at Chapel Hill. He has extensive C++ programming and software design experience as well as medical image analysis and data handling expertise. He is currently continuing his development of ITK's spatialObject library and his freely available spatial object viewer library. Julien is also contributing to the development of the Insight Journal, the Image Guided Surgery Toolkit, and numerous other open-source efforts.

William Lorensen is a Graphics Engineer in the Electronic Systems Laboratory at GE's Corporate Research and Development Center in Schenectady, NY. He has over 35 years of experience in computer graphics and software engineering. He is currently working on algorithms for 3D medical graphics and scientific visualization.

The Insight Software Consortium

<http://www.InsightSoftwareConsortium.org>

Educating users and developers
of open-source, medical image
analysis software

Insight Software Consortium
2005 Overview



Outline

- History of the ISC
- Charter of the ISC
- Contributing to and benefiting from
open-source...

Insight Software Consortium
2005 Overview



History

- Initiated by the original developers of the National Library of Medicine's Insight Toolkit
 - Drs. Terry Yoo, Bill Lorensen, Will Schroeder, ...
 - 2003 Developers' Meeting
- Motivation
 - Near term:
 - Hold the copyright of ITK
 - Long term:
 - Charter of the ISC...



Insight Software Consortium
2005 Overview

Charter

ISC incorporated in New York State in 2005.
A non-profit, educational consortium.

The purpose of this Consortium is to

- 1. support the maintenance of,*
- 2. guide the development of, and*
- 3. promote the use of*

*open-source, medical image analysis
software, data, and publications*

for teaching, research, and commercial endeavors

Insight Software Consortium
2005 Overview



What the ISC means to you...

- The ISC provides proven, documented, open-source software environments and data for developers and users involved in medical image analysis research.
- The haunting past of open-source:
“You get what you pay for...”
 - Open-source is poorly written code
 - Open-source is inefficient
 - Open-source is poorly documented
 - Users: My task is “special.”
...I can do “it” better myself...
 - Developers: Users are “annoying.”
...weird platforms, errors, emails...



Insight Software Consortium
2005 Overview

Process of ISC Open-Source

Ultimate goal: ISC certification



Steps:

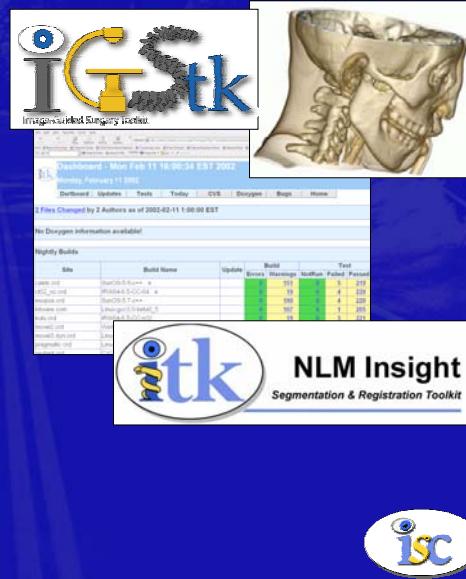
1. Use Development Environment
2. Contribute to Insight Software Journal
3. Participate in Community Review
4. Seek Protection
5. Support Distribution and Education
6. Benefit from Community support

Insight Software Consortium
2005 Overview



1. Development Environment

- ISC Certified
 - ITK
 - IGSTK
- Companion projects
 - CMake
 - Dart / Dashboards
 - Cable / CSwig
 - DCMTK
 - FLTK
 - Slicer
 - VTK



Insight Software Consortium
2005 Overview



Safety of development environment

Policies of the ISC:

- Programming style
- Backward compatibility
- Intellectual property
- Documentation
- Open-source
- Tested
- Maintained
- Cross-platform



Insight Software Consortium
2005 Overview



I can do “it” better myself...



Segmentation

- Statistical, Fuzzy Logic, Markov Random Fields, Mixture Modeling, Parzen Windows, Nearest Neighbor, K-Means, ...
- Level Set, Finite Element, Region Growing, Hybrid, Watershed, Connected Components, Parameterized Models, ...

Registration

- Rigid, Similarity, Affine, Vector Field, Hierarchical, Quaternion, Versor, Parameterized Deformation, Euler, 3D/2D, ...
- Mutual Information, Normalized Correlation, Demons, Mean Squared, Landmark, ...

- Mayo Clinic
- Harvard / Brigham and Women's Hospital
- Cognita, Inc.
- Imperial and King's College London
- University of Iowa
- Georgetown University
- Carnegie Mellon University
- GE Research / Harvard
- Kitware, Inc.
- Insightful / UPenn
- UNC / UPitt
- UPenn / Columbia
- University of Utah
- + Over 70 machine configurations recompile ITK every night
- 20,000+ downloads
- 30+ countries

Insight Software Consortium
2005 Overview



2. Insight Software Journal

<http://www.insight-journal.com>

- Initiated by Dr. Luis Ibanez (Kitware) and developed by Julien Jomier, Zack Galbreath, ...
- Open, online publication
 - Upload, download, and review
 - By-attribution distribution license – not copyright transfer
- Components of an open-science submission:
 1. Paper that describes and demonstrates the method
 2. Source code that implements the method
 3. The data needed to generate the demonstration

Insight Software Consortium
2005 Overview



3. Community Review

Insight Journal

- Review by peers
- Review by automated compilation process

Criterion

- Code
- Documentation
- Utility
- Adherence to policy



Iterative and only a component

- Revisions, respond to reviewers
- Cite in technical journals



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2005 Overview

4. Protection

Once consensus builds for incorporation into an ISC project...

- Transfer copyright to the ISC
 - A level of protection for developers
 - Ensure the open-source status of the software for users
 - Right to modify and distribute
 - Teaching, research, and commercial
- Challenges
 - Acquiring copyright from developers
 - Copyright infringement (known and unknown)
 - Patented code (known and unknown)

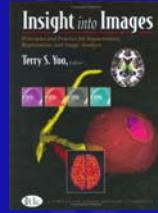


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2005 Overview

5. Distribution and Education

- Integration into ISC development environment
- Tutorials at international conferences:
SPIE Medical Imaging 2003-2005, MICCAI 2003-2004, IEEE Visualization 2003-2005, SIGGRAPH 2005
- Freely available courseware:
Developed collaboratively by CMU, UPitt, Rutgers, and Kitware Inc.
- Examples, Documentation, Users Lists
- Books:

Insight Software Consortium
2005 Overview



6. Community Support

www.InsightSoftwareConsortium.org

- Web portal
- Certification - not sourceforge
- Dedicated to medical image analysis
 - Jobs, News, Links
- Benefit from ISC certification and development environment...education...
- Needs
 - Contributions: Comments, Commented Code, ...
 - Long term dedication
 - Good of the community vs. dissertation / proposal / ...

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2005 Overview



Community Limitations

- FDA
 - FDA does not approve software libraries
 - FDA only approves applications
- GNU General Public License (GPL) software has limited distribution
 - Complicates corporate acceptance of and contribution to the open-source initiative
 - Consider instead the BSD or MIT license

Insight Software Consortium
2005 Overview



Open-Science

-- Dr. Terry S. Yoo, NLM

Open Source + Open Data = Open Science

- Share data
- Share code
- Understanding methods
 - Assumptions, parameters, & outputs
- Comparison of methods
- Extension of methods
- MICCAI 2006, Copenhagen: Open-Source Workshop

Insight Software Consortium
2005 Overview

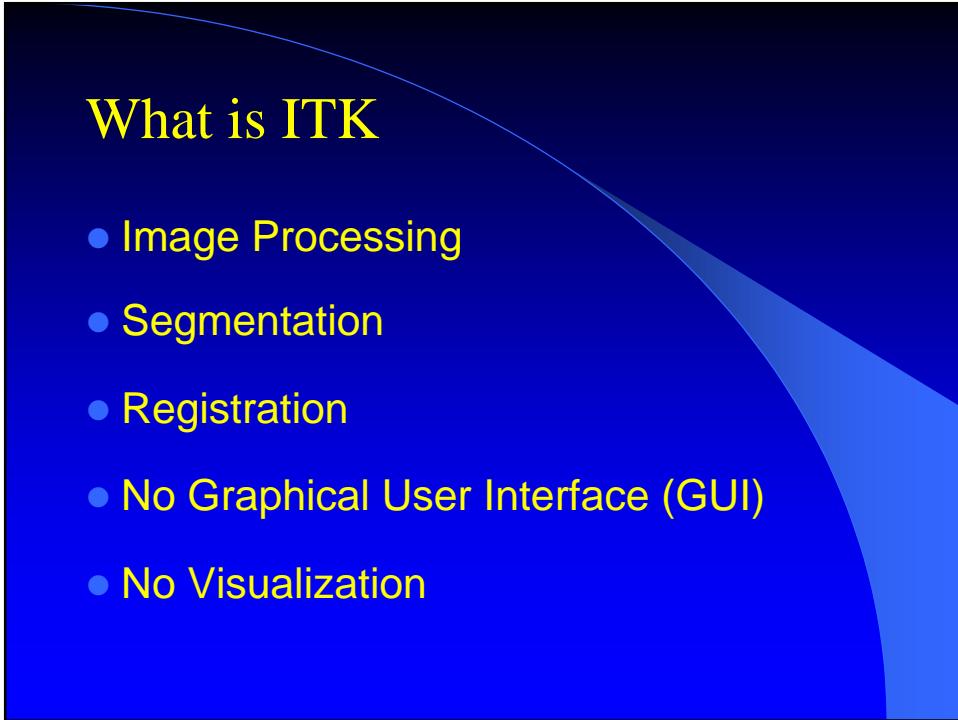


Board of the ISC

- Stephen Aylward
- Joshua Cates
- Luis Ibanez
- Bill Lorensen
- Dimitris Metaxas
- Jim Miller
- Lydia Ng
- Will Schroeder
- Ross Whitaker



Insight Software Consortium
2005 Overview



ITK Sponsors



The National
Institute for Dental and
Craniofacial Research



The National
Science
Foundation



The National Institute of Neurological
Disorders and Stroke



ITK Developers



GE Corporate Research
& Development



PENN VAST LAB



THE
UNIVERSITY
OF UTAH



PENN GRASP LAB

ITK Developers

GE CRD
Bill Lorensen

Insightful
Lydia Ng

U Penn
Dimitris Metaxas

Harvard BWH*
Ron Kikinis

U Penn*
Jim Gee

Columbia U.*
Celina Imielinska

Kitware
Will Schroeder

UNC-CH
Stephen Aylward

U Tennessee
Ross Whitaker

U Pittsburgh*
George Stetten

U Utah*
Ross Whitaker

* indicates a subcontractor.

ITK by the Numbers

- March 2000
 - First code check-in
- 1300
 - # of nightly builds
- 1062
 - tests run nightly
- 41
 - # of platforms (software + hardware)
- 700
 - # of classes
- 1600
 - # of files with code

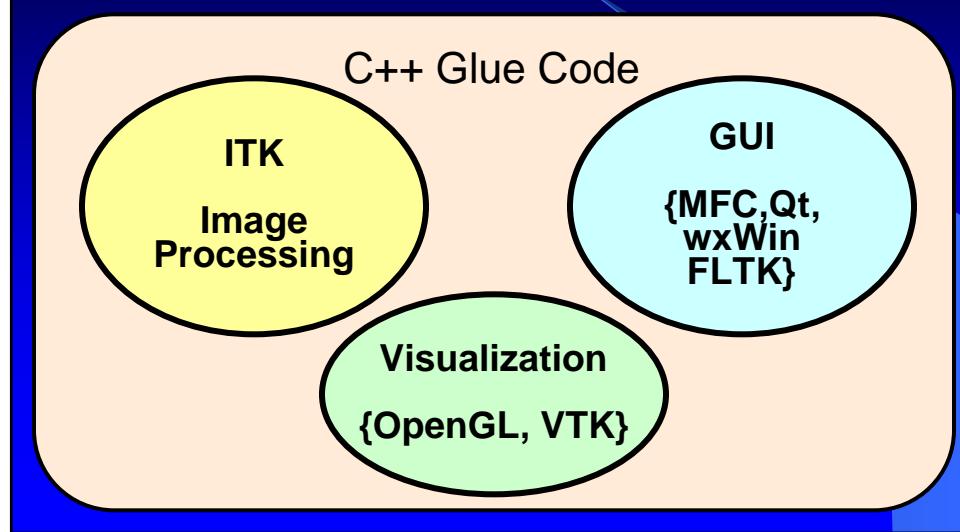
ITK by the Numbers

- 400K
 - # of lines of code
- 100K
 - # of lines of test code
- 35K
 - # of lines of examples
- 150K
 - # of lines of Applications
- 240
 - weekly t-cons
- 50
 - unique developers

ITK by the Numbers

- 1032
 - # of users subscribed to the mailing-list
- 400
 - # of emails posted monthly to the users-list
- 819
 - # of pages in the Software Guide PDF document
- 1800
 - # of monthly hits to the URL of the Software Guide PDF
- 1900
 - # of monthly hits to the URL of the Tutorial PDF
- 2400
 - # of monthly hits to the source code files (.zip + .tar.gz)

How to Integrate ITK in your application



What do I need ?

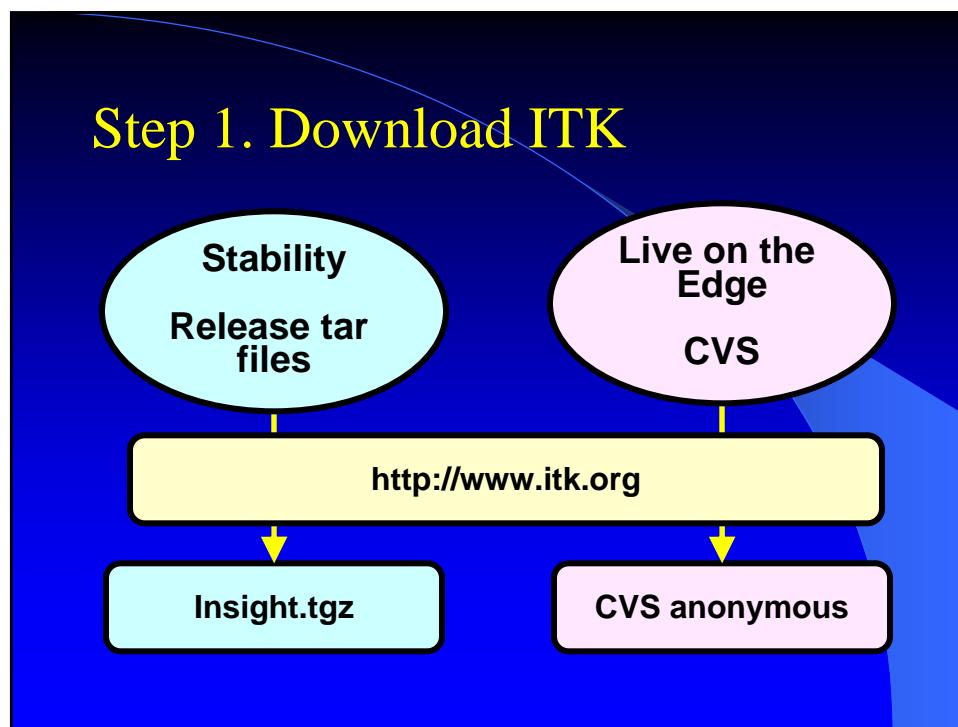
C++ Compiler

gcc 2.95 – 4.0
Visual C++ 6.0
Visual C++ 7.0
Visual C++ 7.1
Visual C++ 8.0
Intel 7.1
Intel 8.0
IRIX CC
Borland 5.5
Mac - gcc

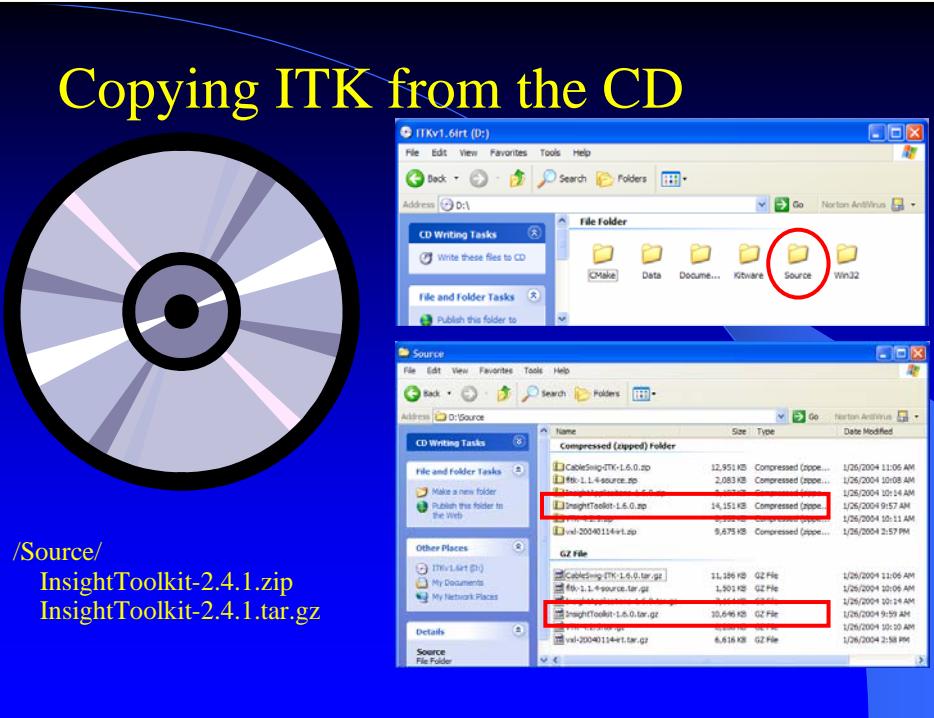
CMake

www.cmake.org

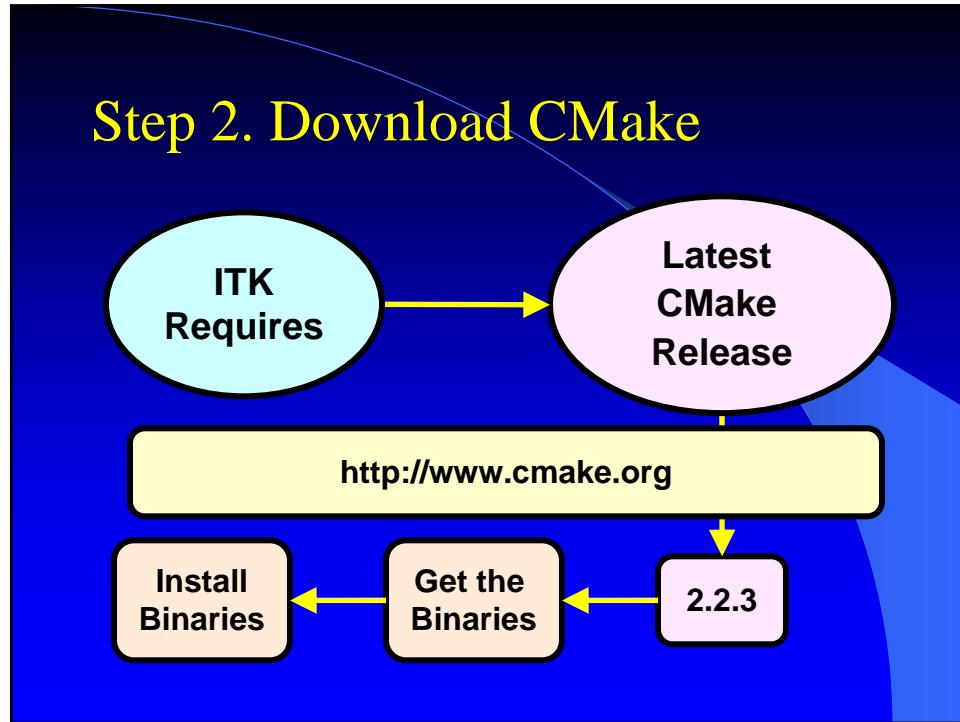
Step 1. Download ITK



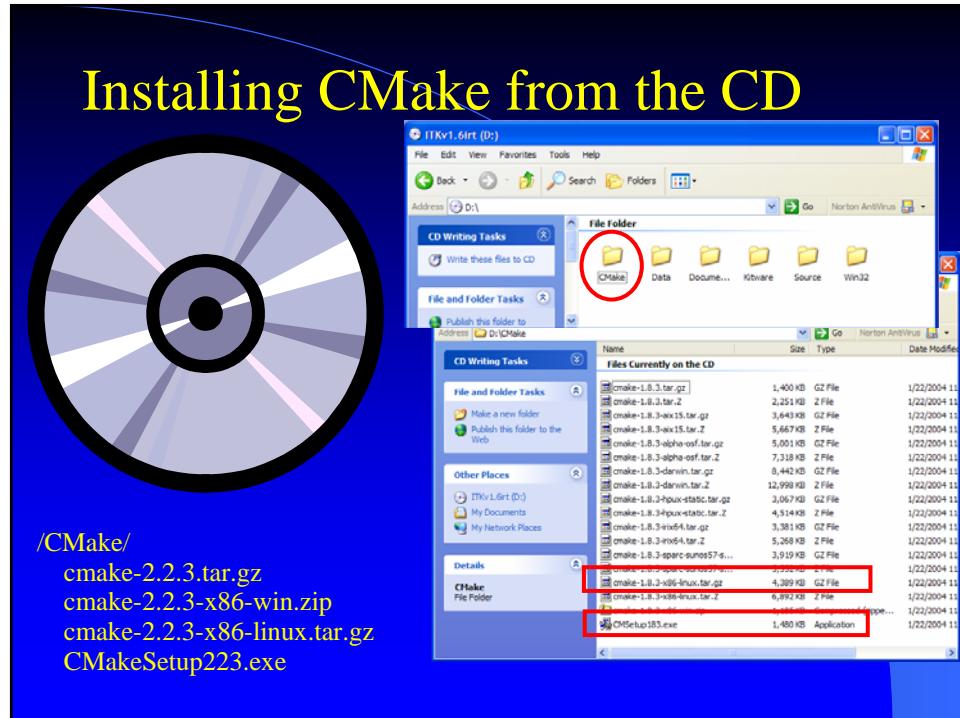
Copying ITK from the CD



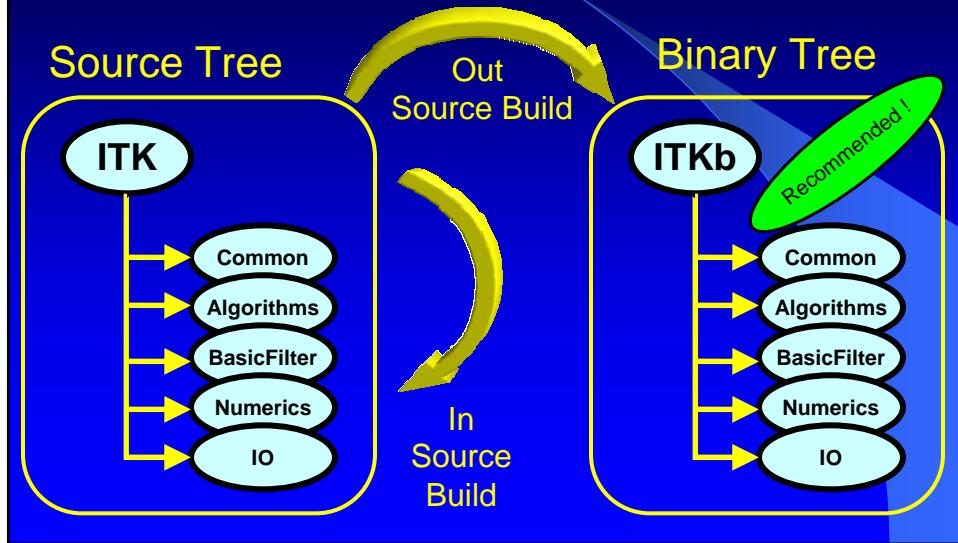
Step 2. Download CMake



Installing CMake from the CD



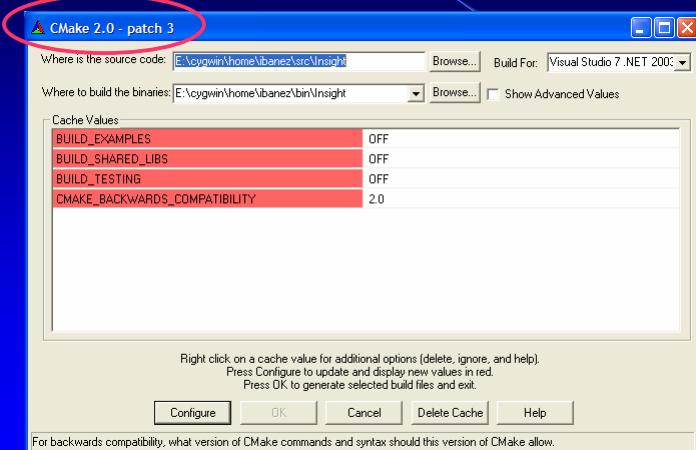
Step 3. Configure ITK



Configuring ITK – MS-Windows

- Run CMake
- Select the SOURCE directory
- Select the BINARY directory
- Select your Compiler

Configuring ITK – MS-Windows



Configuring ITK – MS-Windows

- Disable **BUILD_EXAMPLES**
- Disable **BUILD_SHARED_LIBS**
- Disable **BUILD_TESTING**

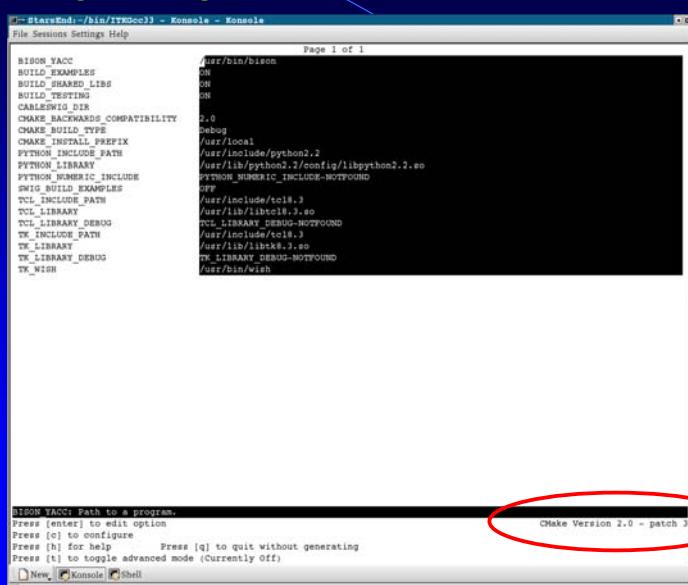
- Click “Configure” to configure
- Click “OK” to generate project files

Configuring ITK – Unix

- Create the **BINARY** directory (`mkdir`)
- Change directory to the **BINARY** directory (`cd`)
- Set the environment variables **CC** and **CXX**

```
setenv CC /usr/bin/gcc;      setenv CXX /usr/bin/g++  OR
export CC=/usr/bin/gcc;      export CXX=/usr/bin/g++
```
- Type `cmake` with argument the **SOURCE** directory

Configuring ITK – Unix



```
BISON YACC: /usr/bin/bison
BUILD_EXAMPLES: ON
BUILD_SHARED_LIBS: ON
BUILD_TESTING: ON
CMAKE_SOURCE_DIR: /usr/local/ITK/ITKv3.0
CMAKE_BACKWARDS_COMPATIBILITY: 2.6
CMAKE_BUILD_TYPE: Debug
CMAKE_INSTALL_PREFIX: /usr/local
PYTHON_INCLUDE_PATH: /usr/include/python2.2
PYTHON_LIBRARY: /usr/lib/python2.2/config/libpython2.2.so
PYTHON_NUMERIC_INCLUDE: /usr/include/python2.2
SWIG_BUILD_EXAMPLES: OFF
TCL_INCLUDE_PATH: /usr/include/tcl8.3
TCL_LIBRARY: /usr/lib/libtcl8.3.so
TCL_LIBRARY_DEBUG: /usr/lib/libtcl8.3.so
TCL_LIBRARY_RELEASE: /usr/lib/libtcl8.3.so
TK_LIBRARY: /usr/lib/libtk8.3.so
TK_LIBRARY_DEBUG: /usr/lib/libtk8.3.so
TK_LIBRARY_RELEASE: /usr/lib/libtk8.3.so
TK_WISH: /usr/bin/wish

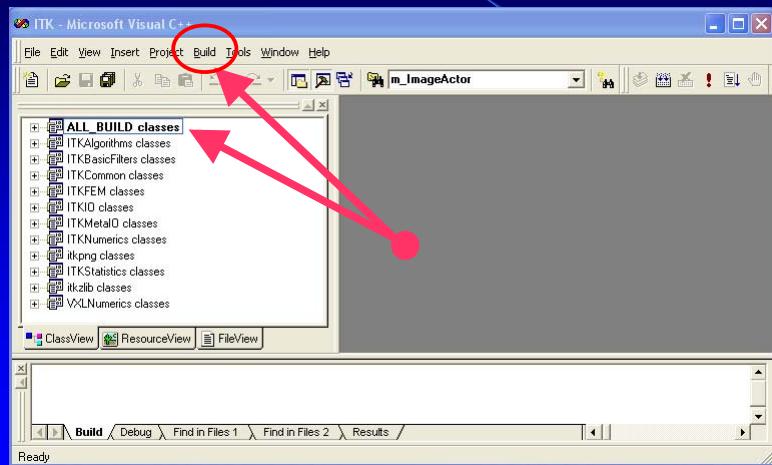
BISON YACC: Path to a program.
Press [enter] to edit option
Press [c] to configure
Press [h] for help      Press [q] to quit without generating
Press [t] to toggle advanced mode (Currently Off)
CMake Version 2.6 - patch 3
```

Configuring ITK – Unix

- Disable `BUILD_EXAMPLES`
- Disable `BUILD_SHARED_LIBS`
- Disable `BUILD_TESTING`

- Type “c” to configure
- Type “g” to generate the Makefiles
- Type “make” to start building

Building ITK



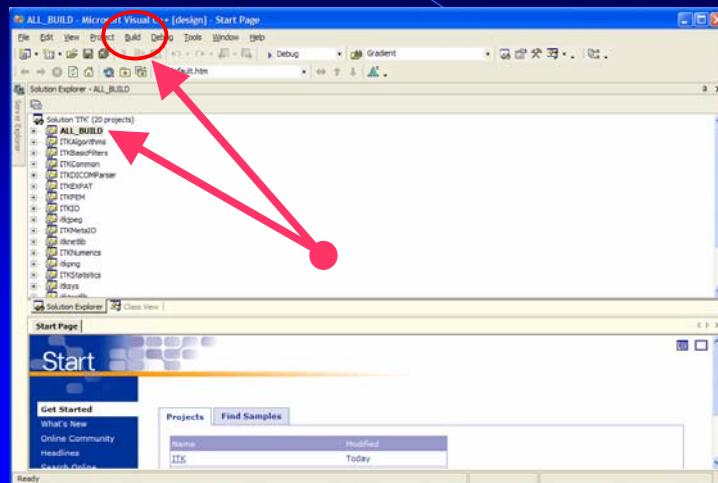
Building ITK

- Open `ITK.dsw` in the Binary Directory
- Select `ALL_BUILD` project
- Build it

...It will take about 15 minutes ...

...It will take about 15 minutes ...

Building ITK



Building ITK

- Open `ITK.sln` in the Binary Directory
- Select `ALL_BUILD` project
- Build it

...It will take about 15 minutes ...

Building ITK

- Most of `ITK` classes are C++ Templates
- Basic libraries are small
they only contain non-templated classes
- Basic libraries are built in about 15 min

Step 5. Verify the Built

Libraries will be found in

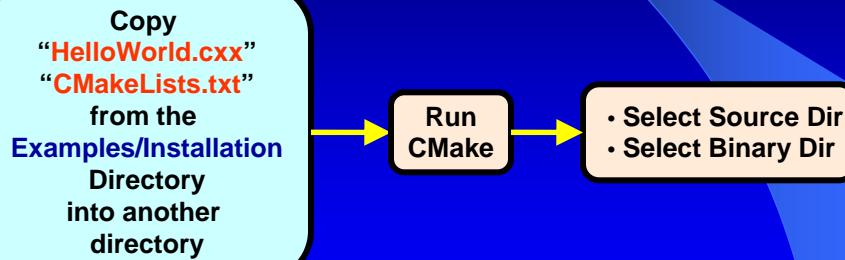
ITK_BINARY / bin / { Debug, Release }

Step 5. Verify the Build

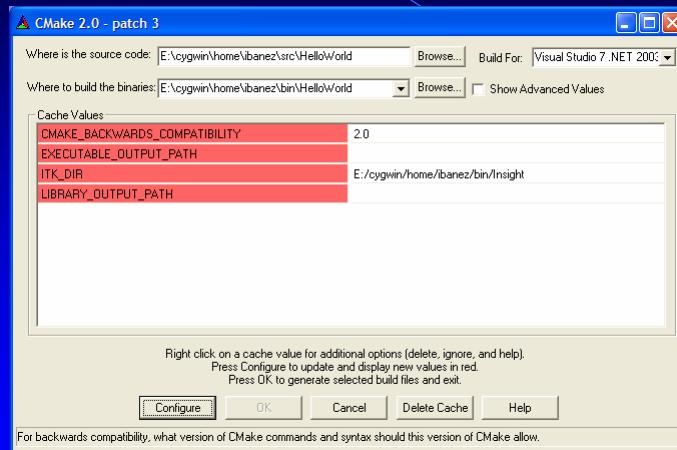
The following libraries should be there

- ITKCommon
- ITKBasicFilters
- ITKAlgorithms
- ITKNumerics
- ITKFEM
- ITKIO
- ITKStatistics
- ITKMetaIO
- itkpng
- itkzlib

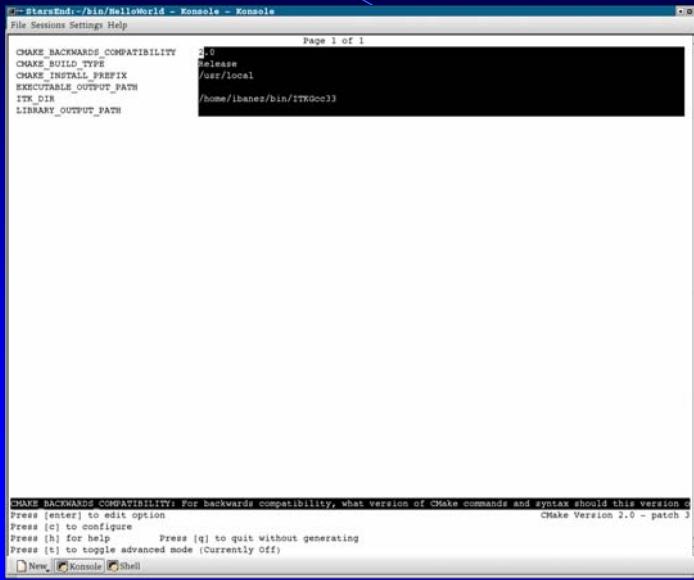
Step 6. Use ITK from an external Project



Using ITK – Hello World



Using ITK – Hello World



The screenshot shows a terminal window titled "StarsEndi-/bin/HelloWorld - Konsole - Konsole". The window displays the following CMake configuration options:

```
File Sessions Settings Help
Page 1 of 1
CMAKE_BACKWARD_COMPATIBILITY: 0
CMAKE_BUILD_TYPE: Release
CMAKE_INSTALL_PREFIX: /usr/local
EXECUTABLE_OUTPUT_PATH: /home/ibanez/bin/ITKHelloWorld
ITK_DIR: /home/ibanez/bin/ITKHelloWorld
LIBRARY_OUTPUT_PATH: /home/ibanez/bin/ITKHelloWorld
```

Below the configuration options, there is a message about CMAKE_BACKWARD_COMPATIBILITY:

```
CMAKE_BACKWARD_COMPATIBILITY: For backwards compatibility, what version of CMake commands and syntax should this version of CMake support? Press [enter] to edit option
Press [c] to configure
Press [h] for help
Press [q] to quit without generating
Press [t] to toggle advanced mode (Currently Off)
```

The terminal window is running CMake Version 2.8 - patch 3.

Step 6. Use ITK from an external Project

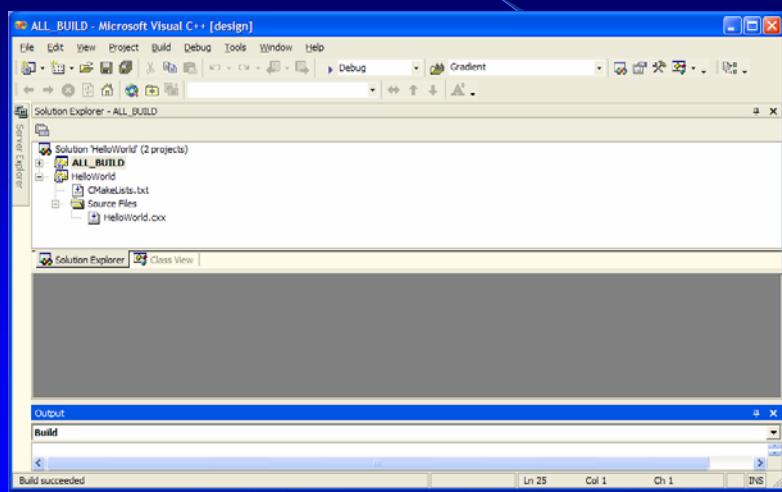
- accept the default in `CMAKE_BACKWARD_COMPATIBILITY`
- leave empty `EXECUTABLE_OUTPUT_PATH`
- leave empty `LIBRARY_OUTPUT_PATH`
- Set `ITK_DIR` to the binary directory where ITK was built

Step 7. Build Sample Project

- Open `HelloWorld.dsw` (or `.sln`) generated by CMake
- Select `ALL_BUILD` project
- Build it

...It will take about 3 seconds ...

Step 7. Build Sample Project



Step 8. Run the example

- Locate the file `HelloWorld.exe`
- Run it...
- It should produce the message:

`ITK Hello World !`

Starting your own project

- Create a clean new directory
- Write a `CMakeLists.txt` file
- Write a simple `.cxx` file
- Configure with `CMake`
- Build
- Run

Step 9. Writing CMakeLists.txt

```
PROJECT( myProject )

FIND_PACKAGE ( ITK )
IF ( ITK_FOUND )
    INCLUDE( ${ITK_USE_FILE} )
ENDIF( ITK_FOUND )

ADD_EXECUTABLE( myProject myProject.cxx )

TARGET_LINK_LIBRARIES ( myProject ITKCommon ITKIO)
```

Step 10. Writing myProject.cxx

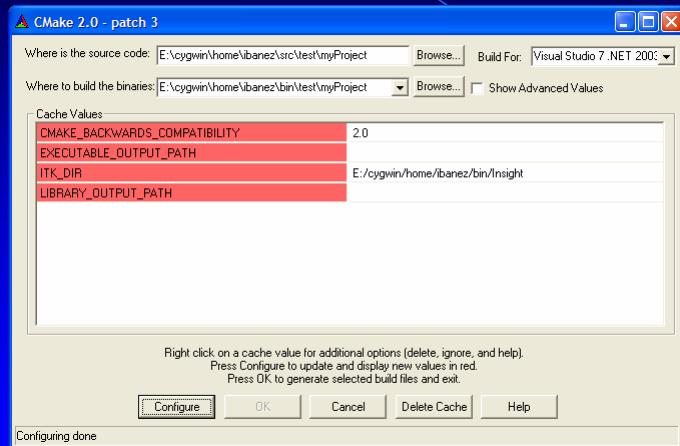
```
#include "itkImage.h"
#include "itkImageFileReader.h"
#include "itkGradientMagnitudeImageFilter.h"

int main( int argc, char **argv ) {
    typedef itk::Image<unsigned short,2>           ImageType;
    typedef itk::ImageFileReader<ImageType>           ReaderType;
    typedef itk::GradientMagnitudeImageFilter<
        ImageType,ImageType>           FilterType;

    ReaderType::Pointer reader = ReaderType::New();
    FilterType::Pointer filter = FilterType::New();

    reader->SetFileName( argv[1] );
    filter->SetInput( reader->GetOutput() );
    filter->Update();
    return 0;
}
```

Step 11. Run CMake

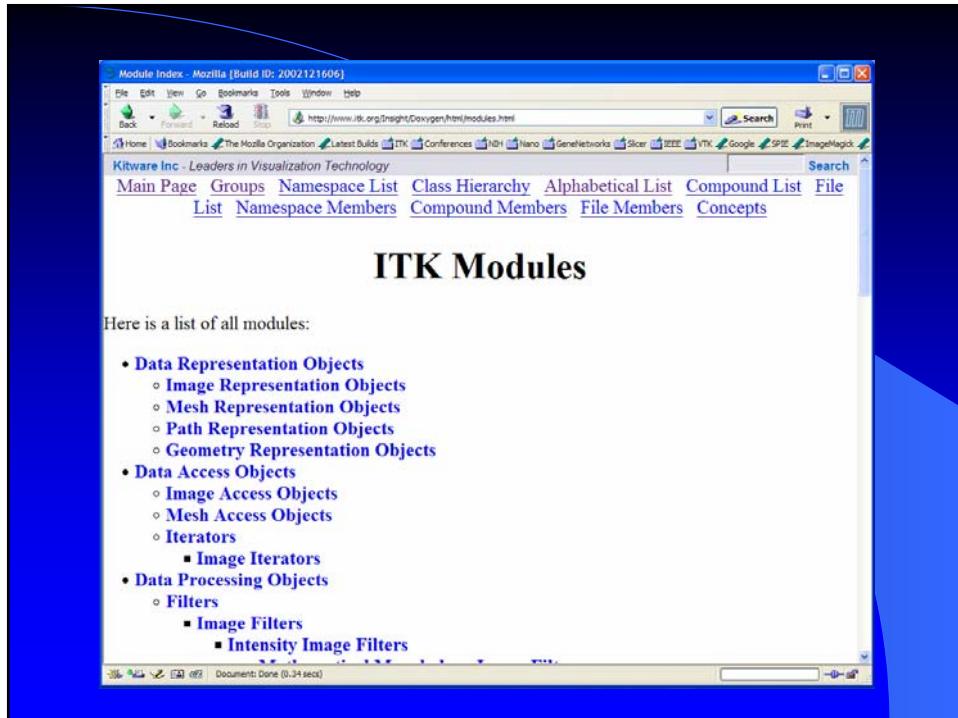
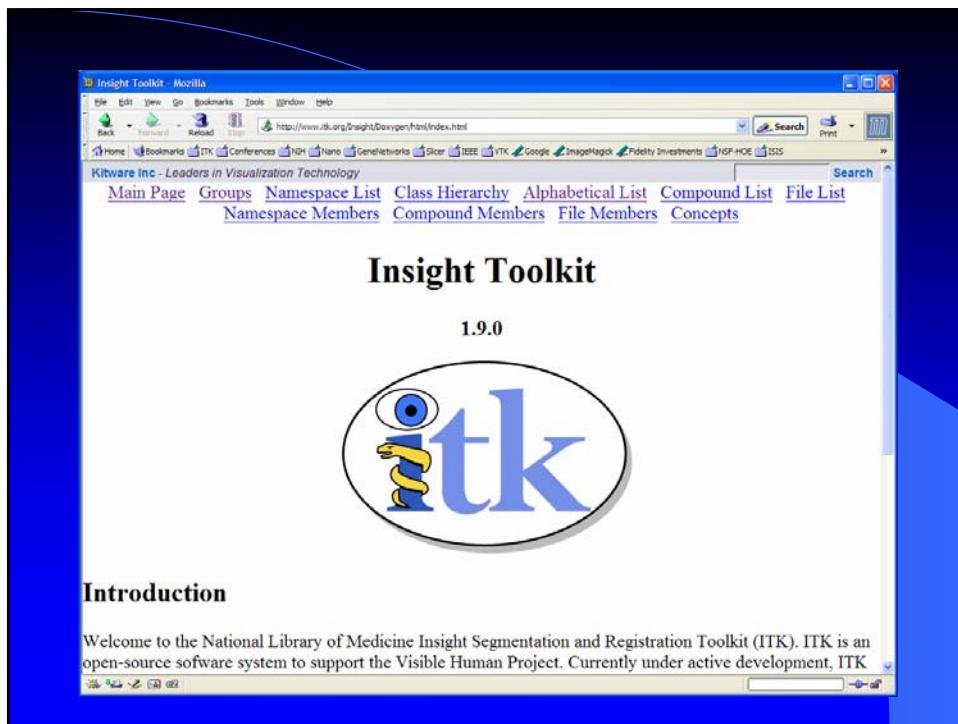


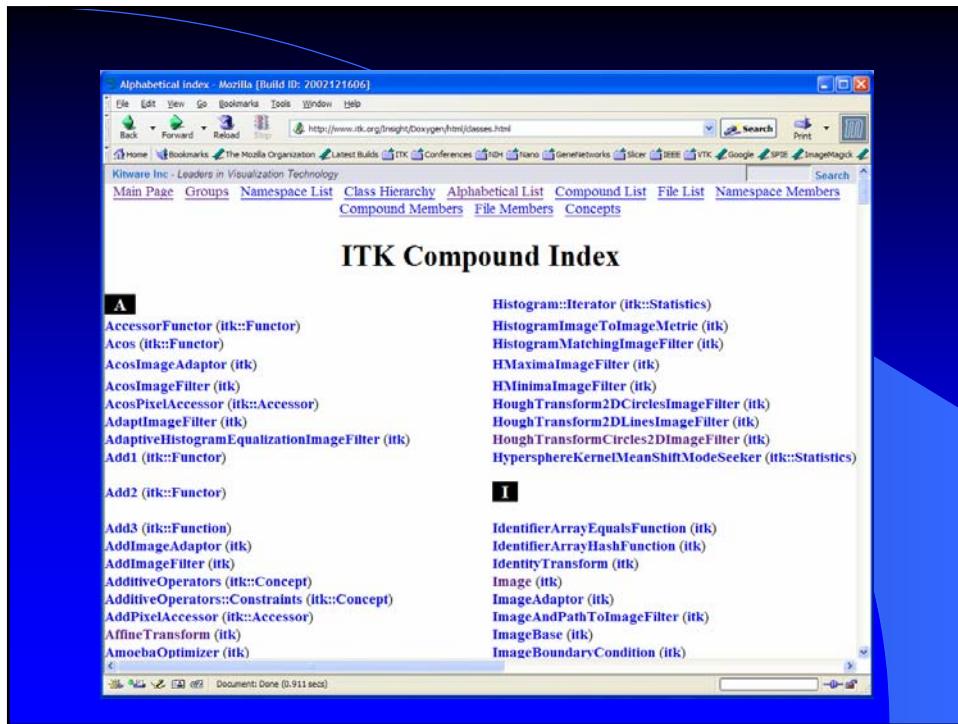
Step 12. How to find what you need

<http://www.itk.org/ItkSoftwareGuide.pdf>

<http://www.itk.org/Doxygen/html/index.html>

- Follow the link Alphabetical List
- Follow the link Groups
- Post to the [insight-users mailing list](#)

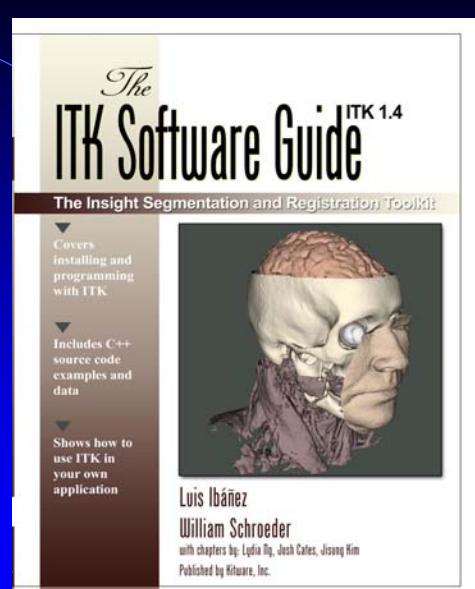




The ITK Software Guide is freely available as a PDF document at

[www.itk.org/
ItkSoftwareGuide.pdf](http://www.itk.org/ItkSoftwareGuide.pdf)

Its paper version can be ordered from Amazon.com and from Kitware's e-store.







Generic Programming

Example: **STL** Standard Template Library

Abstraction of Types and Behaviors

```
std::vector< T >

std::vector< int >
std::vector< double >
std::vector< char * >
std::vector< Point >
std::vector< Image >
```

itk::Image

```
itk::Image< PixelType , Dimension >
```

```
itk::Image< char , 2 >
itk::Image< char , 3 >
itk::Image< char , 4 >
itk::Image< float , 2 >
itk::Image< RGB , 3 >
itk::Image< unsigned short , 2 >
itk::Image< itk::Vector<float,2> , 2 >
```

namespaces

Avoid naming collisions

```
itk::  
itk::Statistics::  
itk::fem::  
itk::fem::itpack  
itk::bio
```

Your favorite keyword

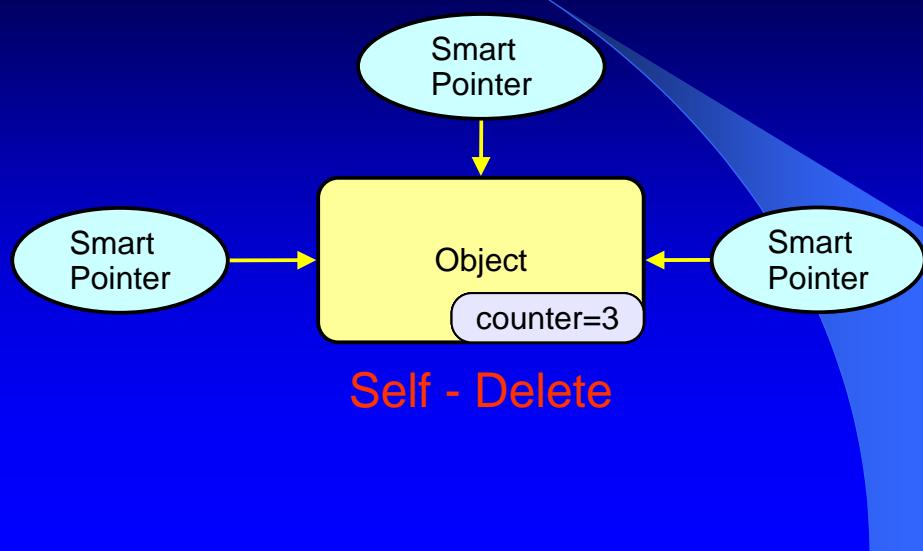
`typedef`

```
typedef itk::Image< char , 2 >  ImageType  
typedef itk::ImageFilter< ImageType , ImageType >  FilterType
```

otherwise...

```
itk::ImageFilter< Image< char , 2 > ,  
                Image< char , 2 > >  FilterType
```

Smart Pointers



SmartPointers

```
typedef itk::Image< char , 2 >  ImageType
typedef itk::ImageFilter< ImageType , ImageType >  FilterType
```

```
FilterType::Pointer filter = FilterType::New();
```

```
ImageType::Pointer image = filter->GetOutput();
```

Pointer notation

```
filter->Update();
```

NO NEED FOR

```
filter->Delete();
```

Const Correctness

Knowing constancy is Insight.

Not knowing constancy leads to disaster.

Tao Te Ching, XVI. Lao Tsu

Const Smart Pointers

```
typedef itk::Image< char , 2 >  ImageType
typedef itk::ImageFilter< ImageType , ImageType >  FilterType
```

```
FilterType::Pointer filter = FilterType::New();
```

```
ImageType::ConstPointer image = filter->GetOutput();
```

Can only invoke “const” methods

```
image->GetSpacing ();
```

Compiler error for “non-const” methods

```
image->SetSpacing ( spacing );
```

Creating an Image

```
typedef itk::Image< char , 3 > ImageType

ImageType::Pointer image = ImageType::New();

ImageType::SizeType size;
size[ 0 ] = 512; // x direction
size[ 1 ] = 512; // y direction
size[ 2 ] = 50; // z direction

ImageType::IndexType start;
start[ 0 ] = 0; // x direction
start[ 1 ] = 0; // y direction
start[ 2 ] = 0; // z direction
```

Creating an Image

```
ImageType::RegionType region;
region.SetSize( size );
region.SetIndex( start );

image->SetRegions( region );
image->Allocate();
image->FillBuffer( 0 );

ImageType::SpacingType spacing;
spacing[ 0 ] = 0.83; // x direction
spacing[ 1 ] = 0.83; // y direction
spacing[ 2 ] = 2.15; // z direction

image->SetSpacing( spacing );
```

Exercise 3

Streaming

Processing Large Images

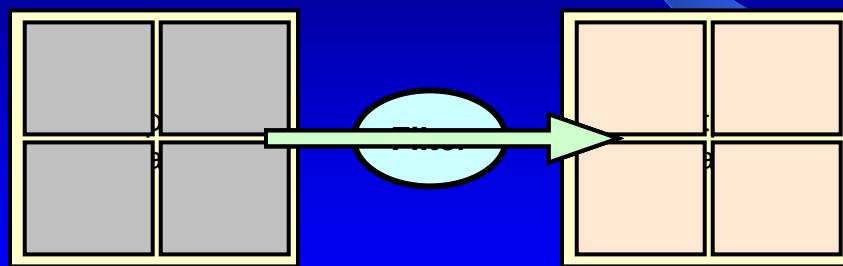


Image Regions

LargestPossibleRegion

BufferedRegion

RequestedRegion

Data Pipeline

Image → Filter

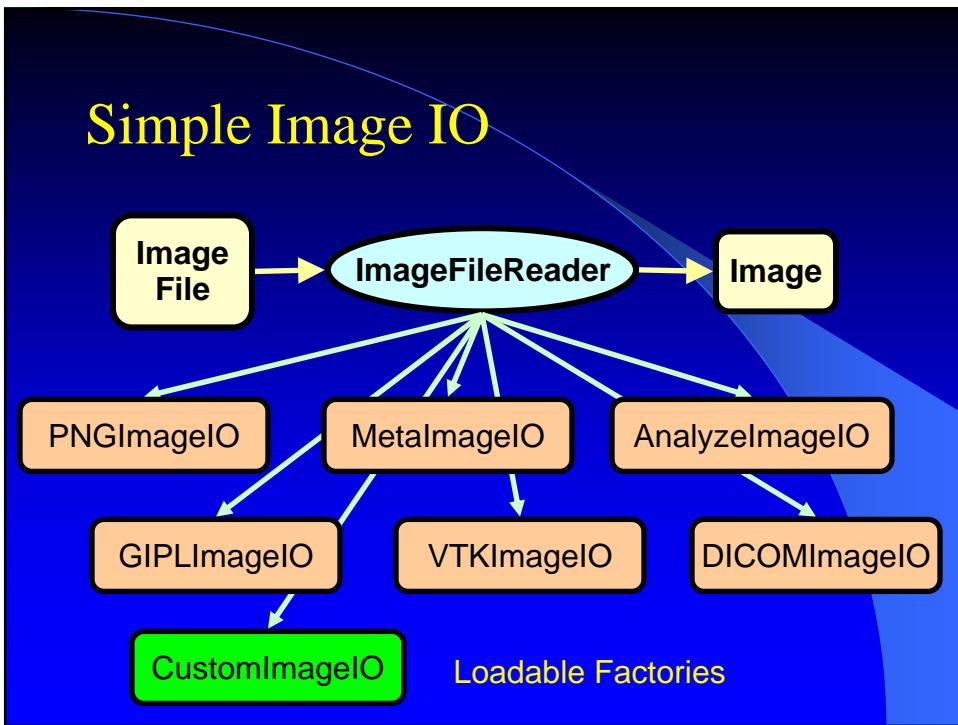
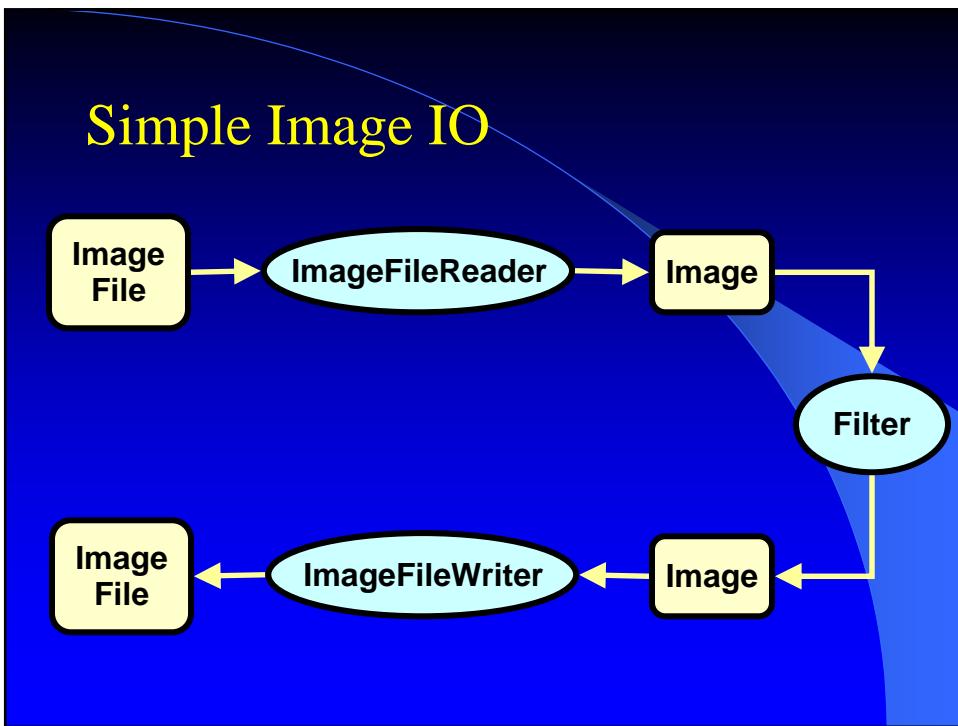
Image

Filter

Image

Image → Filter

Image



Simple Image IO

```
#include "itkImage.h"
#include "itkImageFileReader.h"
#include "itkImageFileWriter.h"

typedef itk::Image< char , 2 >  ImageType;
typedef itk::ImageFileReader< ImageType >  ReaderType;
typedef itk::ImageFileWriter< ImageType >  WriterType;

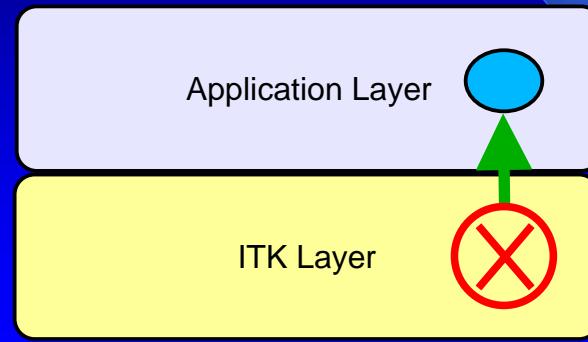
ReaderType::Pointer reader = ReaderType::New();
WriterType::Pointer   writer = WriterType::New();

reader->SetFileName( "inputImage.dcm" );    // DICOM
writer->SetFileName( "outputImage.hdr" );    // Analyze

writer->SetInput( reader->GetOutput() );
writer->Update();
```

Exceptions

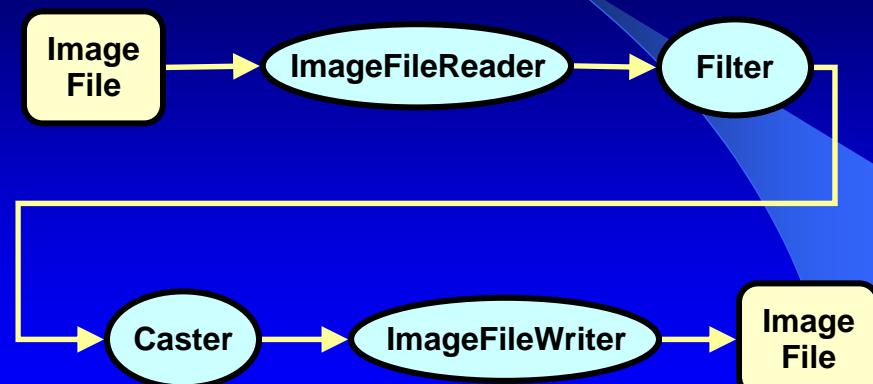
Error Management



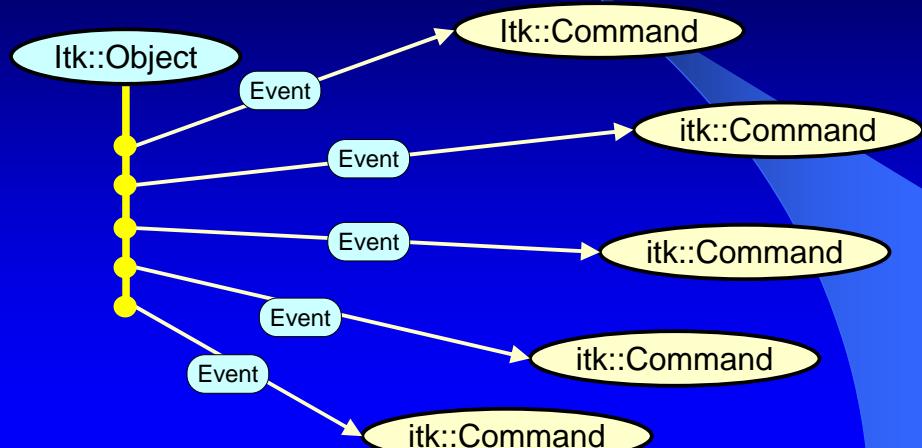
Exceptions

```
try
{
    filter->Update();
}
catch( itk::ExceptionObject & exp )
{
    std::cerr << exp << std::endl;
}
```

Exercise 4



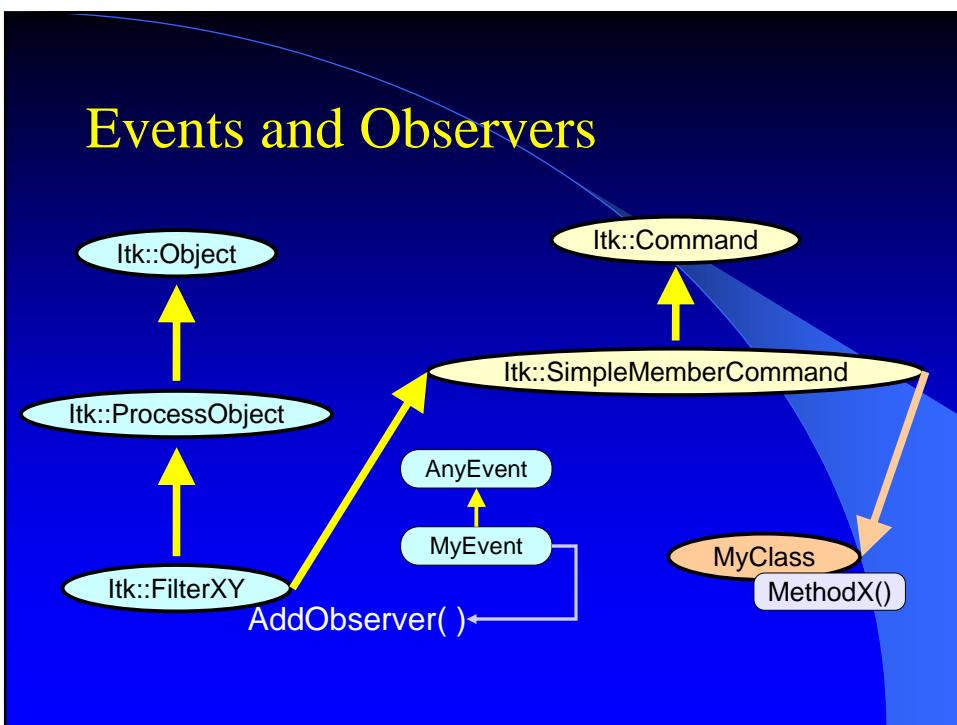
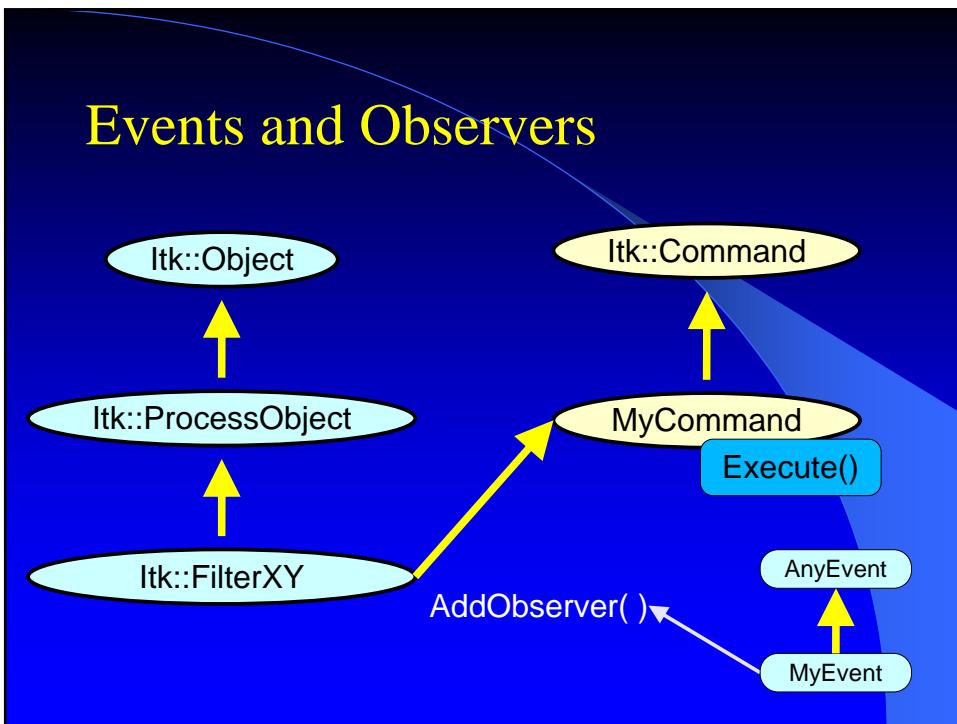
Events and Observers



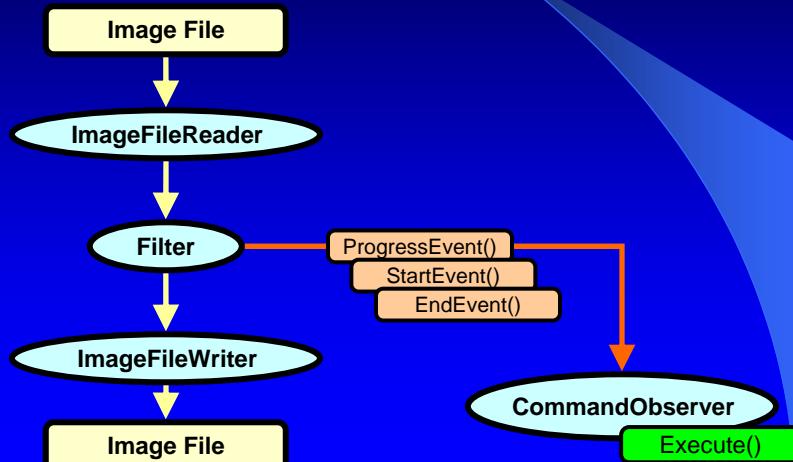
Events and Observers

Common Events

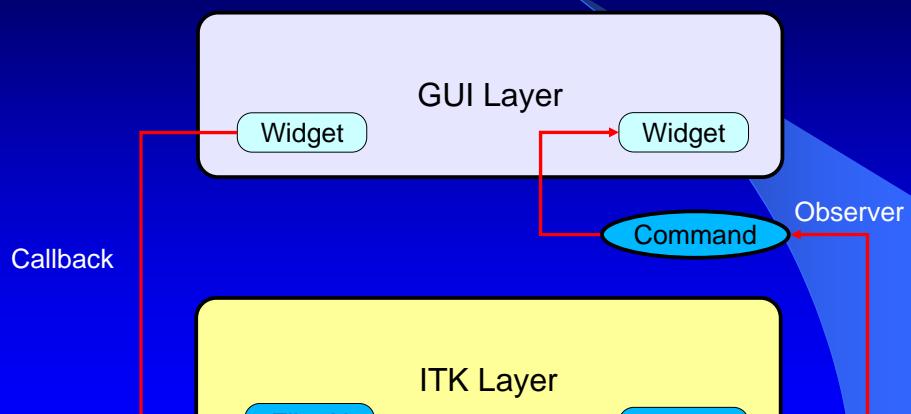
- AnyEvent()
- StartEvent()
- EndEvent()
- ProgressEvent()
- IterationEvent()



Exercise 5



GUI Communication





Introduction to ITK Segmentation



The Insight Consortium presented by Josh Cates

*Scientific Computing and Imaging Institute
University of Utah*



Session Objectives

- Review some important considerations when using ITK filters
- Overview of low-level image processing filters
 - denoising / scale space
 - feature extraction
- Overview some common segmentation filters
 - connected component
 - pixel classification
 - watersheds
 - level-set methods
- Brief introduction to image processing “frameworks” in ITK
- See examples
 - simple command line
 - full applications with user interaction

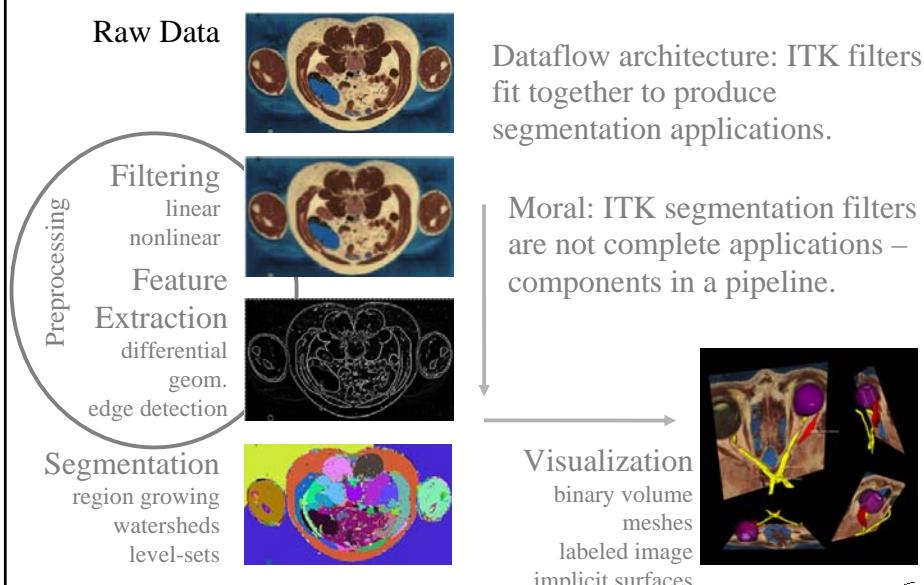


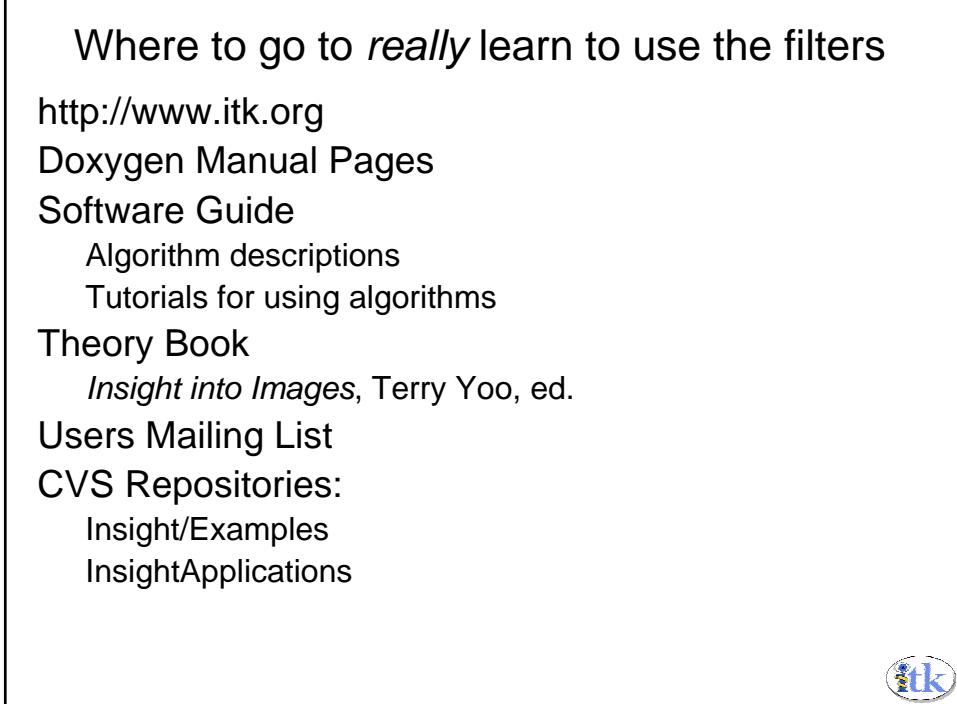
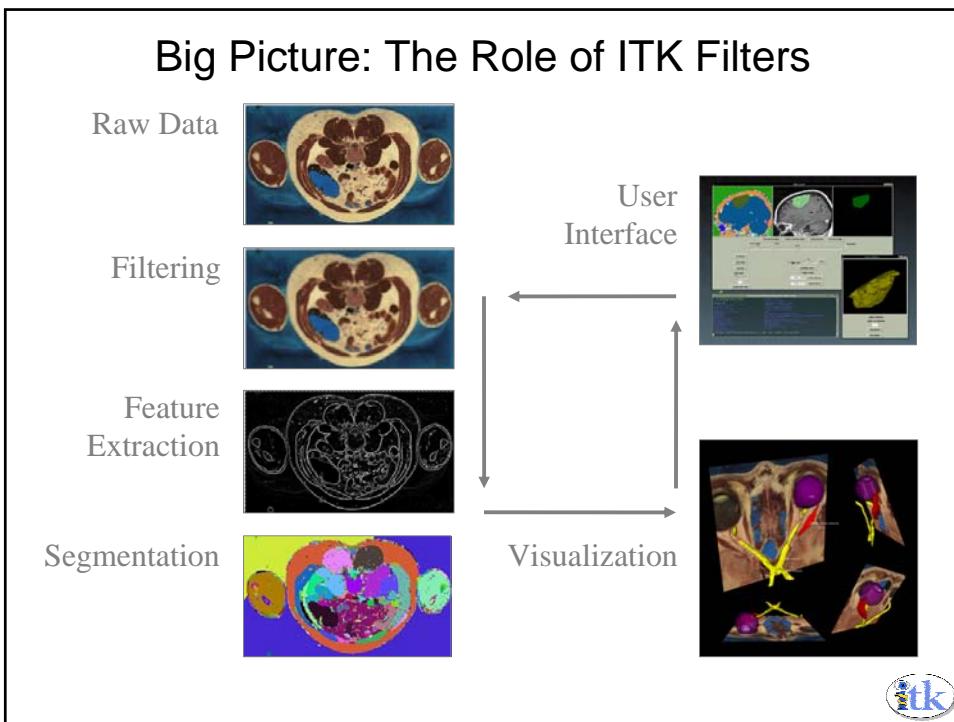
Important Facts about ITK Filters

1. Most filters are N dimensional
2. Many filters run multi-threaded
3. Filters are implemented within frameworks
4. Most filters are documented
5. Filters are regression tested
6. Data type matters
7. Pixel spacing matters
8. Filters are not full applications
9. Filters require parameter tuning



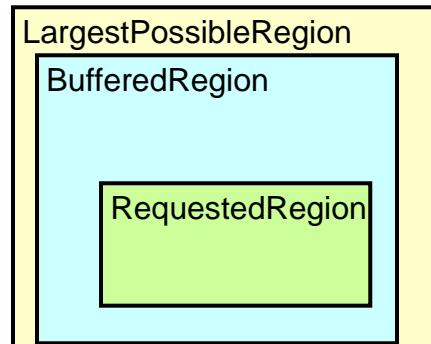
Big Picture: The Role of ITK Filters





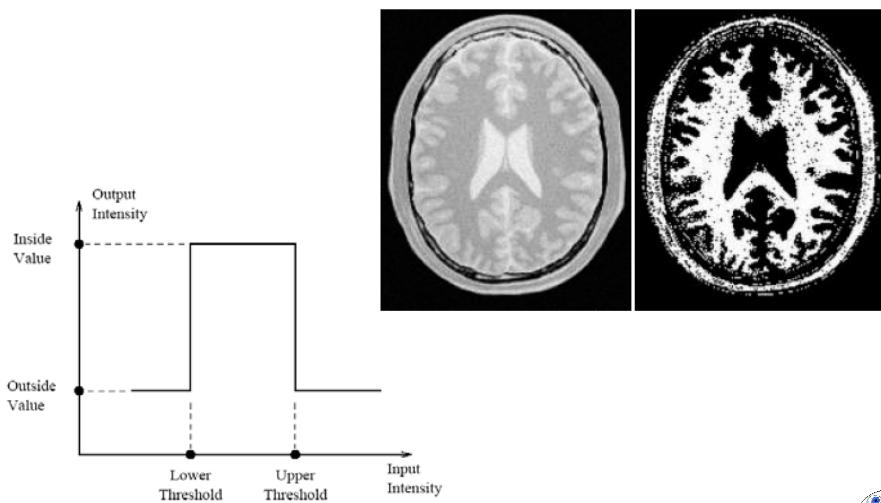
What is an ITK Image?

- Templated over data type
- May be vector-valued
- Templated over dimensionality
- Spacing, origin & orientation information
- Pixels may be addressed directly or through an assortment of iterators
- Interpolators may also be used
- In general, implemented as a flat, C++ array
- Buffers may be imported & exported



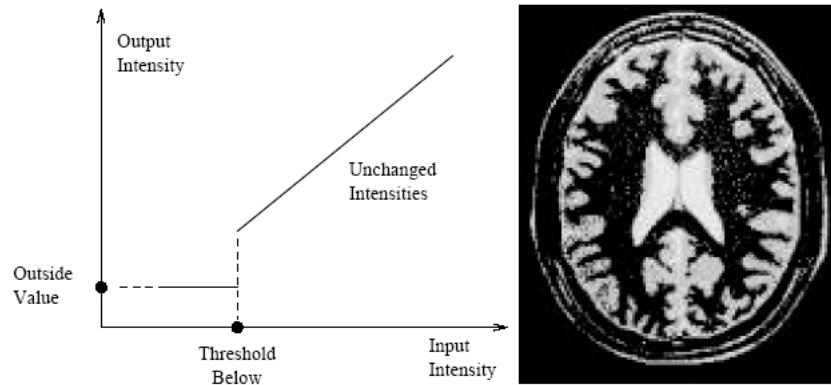
Thresholding

BinaryThresholdImageFilter



Thresholding

ThresholdImageFilter



Intensity Transformations

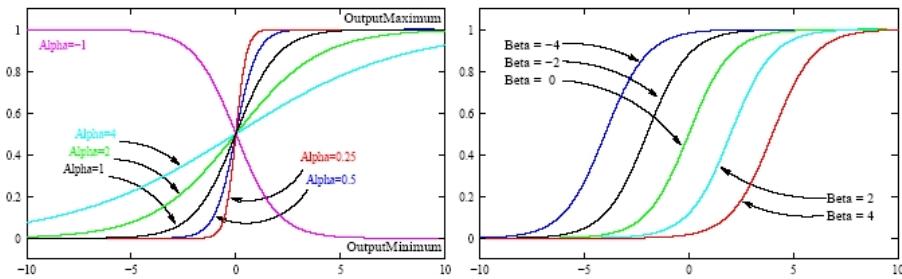
CastImageFilter

RescaleIntensityImageFilter

ShiftScaleImageFilter

NormalizeImageFilter

SigmoidImageFilter



Intensity Transformations

SigmoidImageFilter

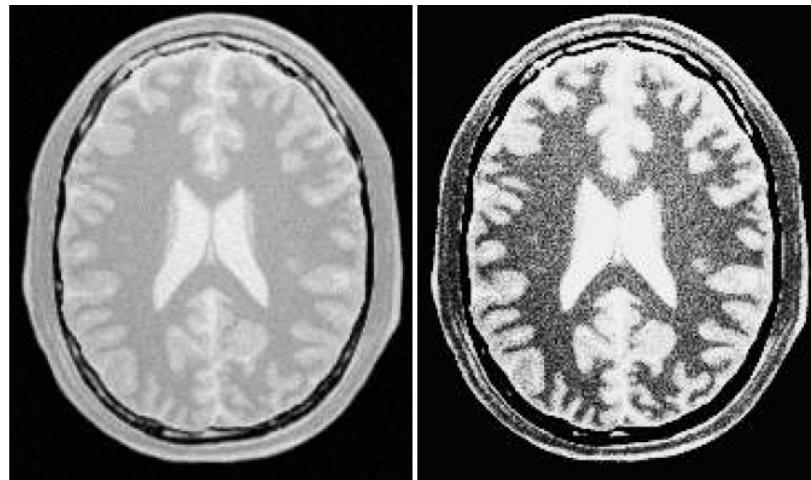


Image Morphology

BinaryErodeImageFilter

BinaryDilateImageFilter

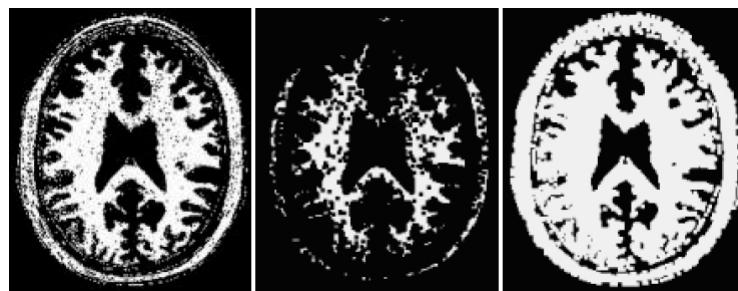
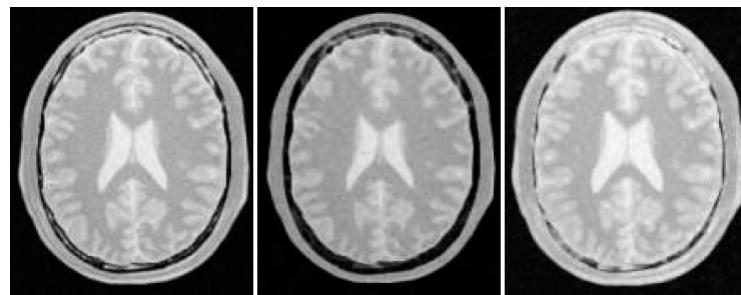


Image Morphology

GrayscaleErodeImageFilter

GrayscaleDilateImageFilter

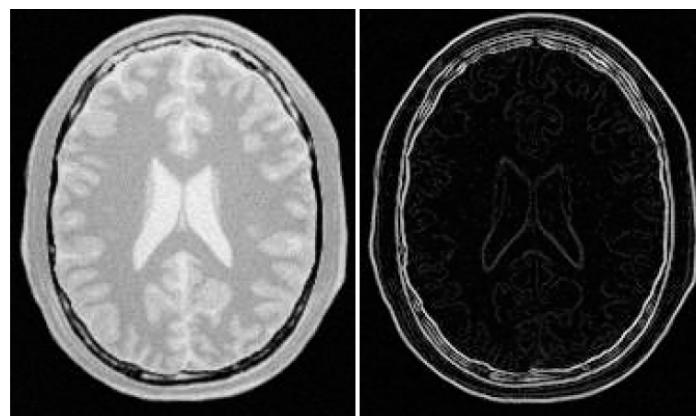


Edge Detection & Feature Extraction

CannyEdgeDetectionImageFilter

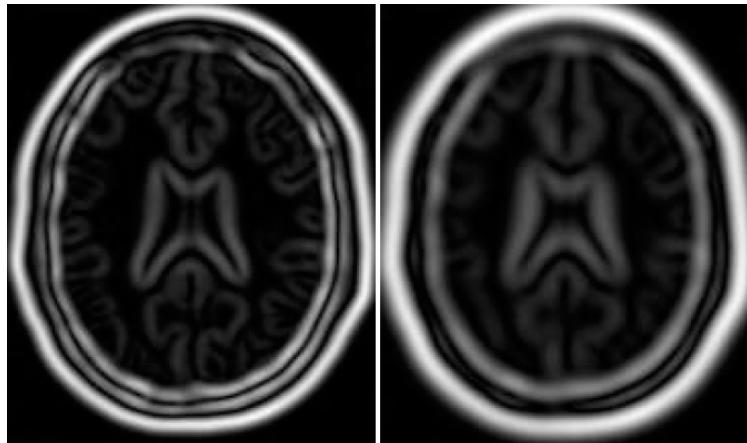
LaplacianImageFilter

GradientMagnitudeImageFilter



Edge Detection & Feature Extraction

GradientMagnitudeRecursiveGaussianImageFilter



Edge Detection & Feature Extraction

DerivativeImageFilter

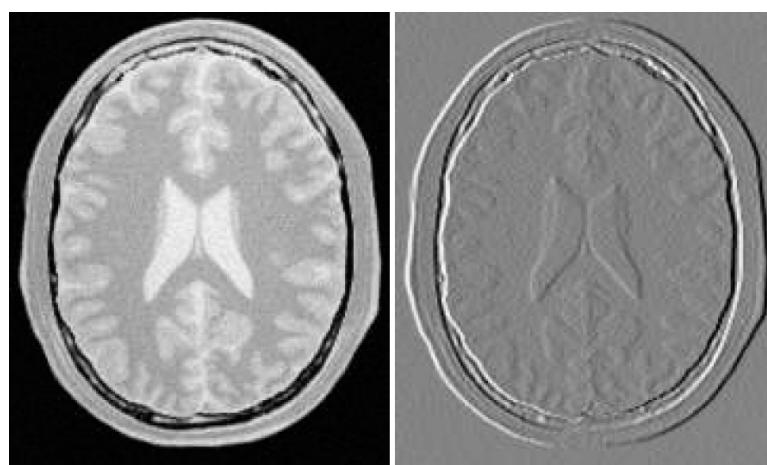


Image Denoising: Linear

MeanImageFilter

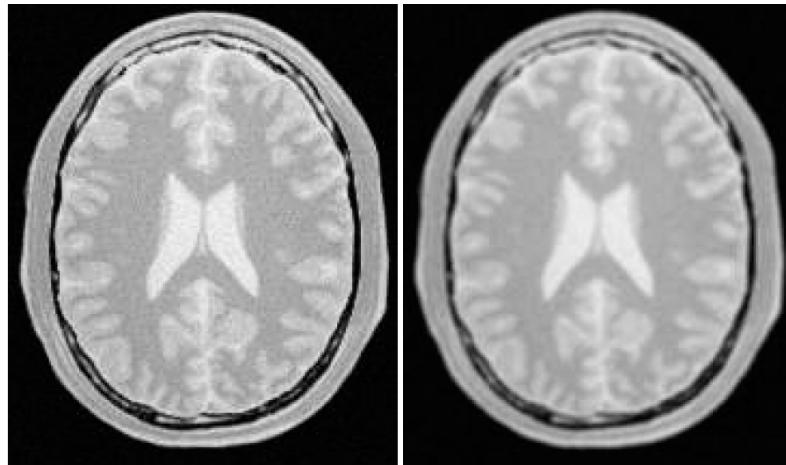


Image Denoising: Linear

MedianImageFilter

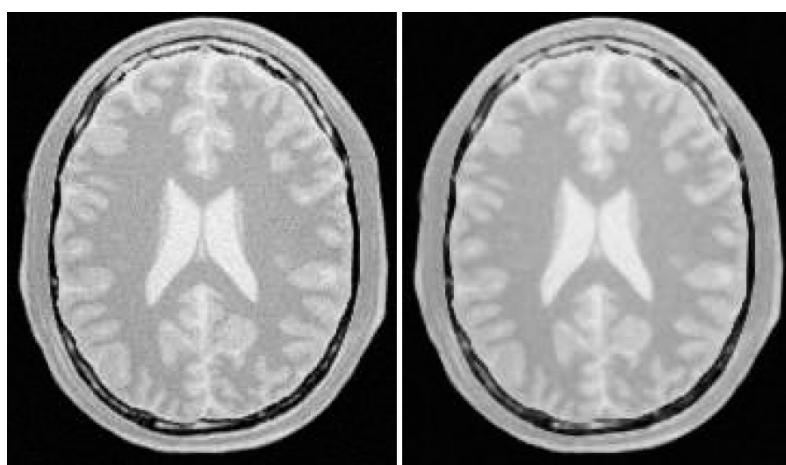


Image Denoising: Linear

BinomialBlurImageFilter
RecursiveGaussianImageFilter
DiscreteGaussianImageFilter

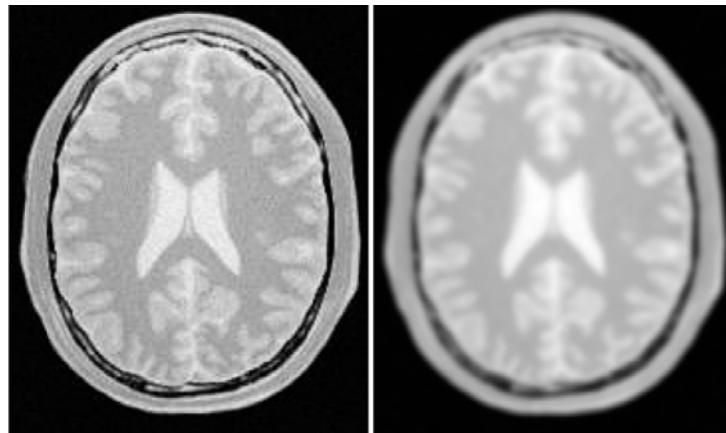


Image Denoising: Nonlinear

BilateralImageFilter
CurvatureFlowImageFilter
GradientAnisotropicDiffusionImageFilter
CurvatureAnisotropicDiffusionImageFilter

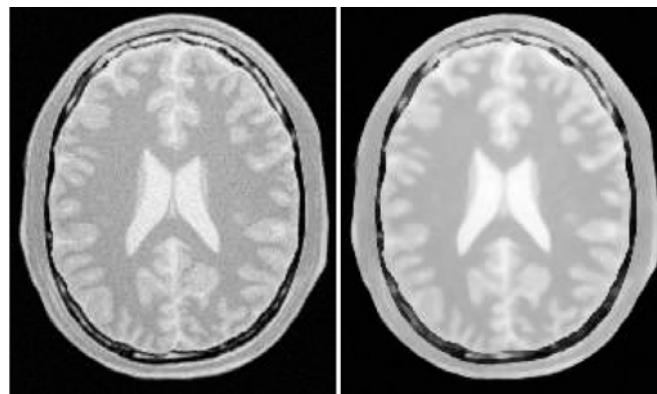
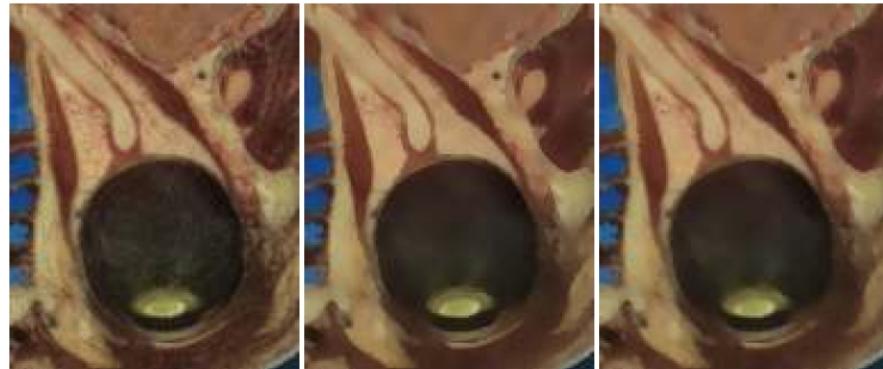


Image Denoising: Nonlinear

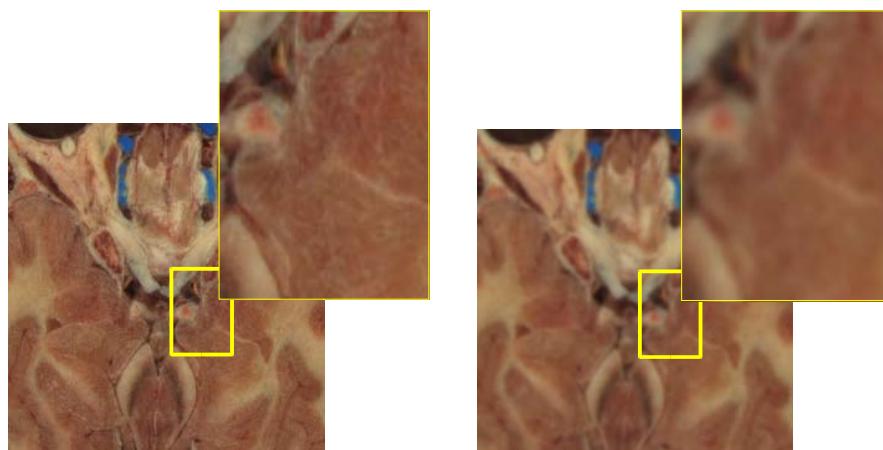
VectorGradientAnisotropicDiffusionImageFilter

VectorCurvatureAnisotropicDiffusionImageFilter



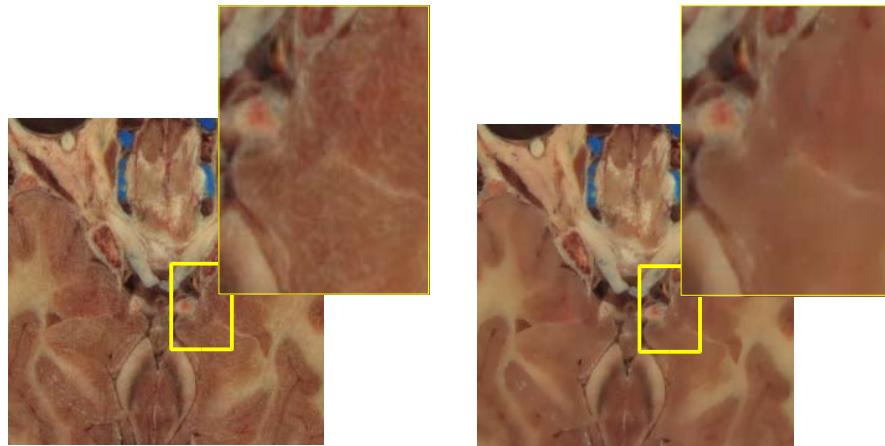
Linear Diffusion

Destroys and moves edges



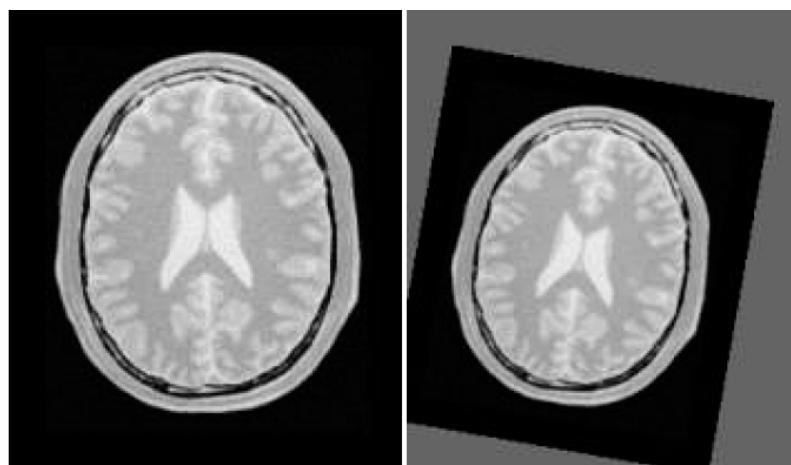
Nonlinear Diffusion

Preserves Edges



Geometric Transformations

TransformImageFilter



Remember

Filters generalize to N dimensions

Filters “work” on arbitrary data types, but only some data types make sense

Filters are implemented within *extensible* frameworks



Image Neighborhood Framework

Neighborhood is a set of pixels local adjacent to one another

Used to implement algorithms where result at pixel i is based on some computation within the neighborhood of i

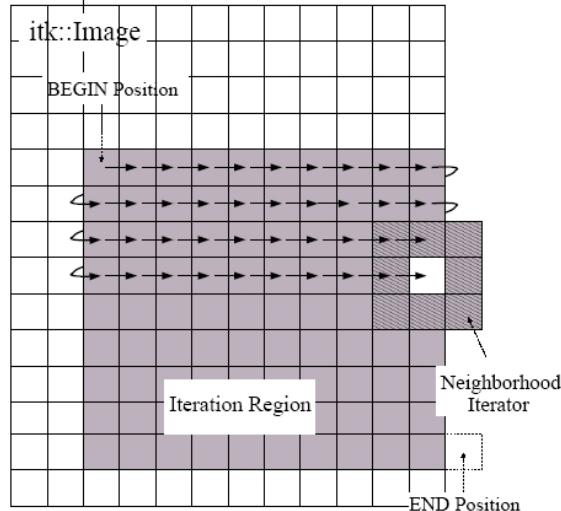
Iterators abstract the API for working with a neighborhood of pixels in arbitrary dimensions

Operators are applied to image neighborhood to perform various calculations

Boundary conditions are handled automatically



Neighborhood Iterator Framework



Neighborhood Iterators

0 (-1, -1)	1 (0, -1)	2 (1, -1)
3 (-1, 0)	4 (0, 0)	5 (1, 0)
6 (-1, 1)	7 (0, 1)	8 (1, 1)

radius = [1,1]
size = [3,3]

0 (-1,-2)	1 (0,-2)	2 (1,-2)
3 (-1,-1)	4 (0,-1)	5 (1,-1)
6 (-1,0)	7 (0,0)	8 (1,0)

radius = [1,2]
size = [3,5]

0 (-1,0)	1 (0,0)	2 (1,0)
radius = [1,0] size = [3,1]		

0 (0,-2)
1 (0,-1)
2 (0,0)
3 (0,1)
4 (0,2)

0 (-3,-1)	1 (-2,-1)	2 (-1,-1)	3 (0,-1)	4 (1,-1)	5 (2,-1)	6 (3,-1)
7 (-3,0)	8 (-2,0)	9 (-1,0)	10 (0,0)	11 (1,0)	12 (2,0)	13 (3,0)
14 (-3,1)	15 (-2,1)	16 (-1,1)	17 (0,1)	18 (1,1)	19 (2,1)	20 (3,1)

radius = [3,1]
size = [7,3]



ITK Segmentation Algorithms

Classification / Thresholding

Region Growing

Watersheds

Level-set Methods

“Hybrid” Methods



Statistical Pattern Classification

Idea

Find disjoint regions in a feature space

Classify image pixels according to feature vectors

Classifier

Multiple membership functions (each represents one possible class) return scores from feature vectors

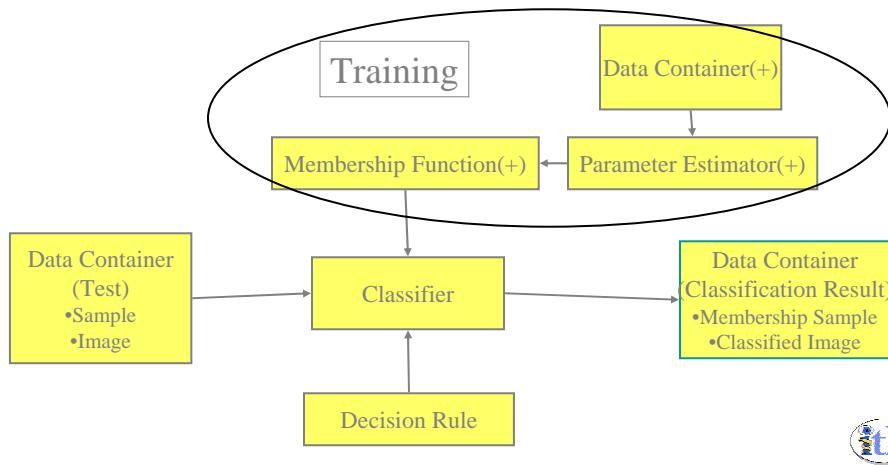
Decision rule based on scores

Implemented using the ITK statistics subsystem
(framework)



Statistical Pattern Classification Framework

1. Measurement vectors are input to membership functions
2. Membership functions feed scores to decision rule
3. Decision rule compares scores and returns a class label



Classifier Framework Example

Segmentation of gene expression images of the mouse brain
at the Allen Institute for Brain Science, Seattle WA*

Designed with ITK components

`Itk::ImageModelEstimatorBase & related classes`
`itk::Statistics::MembershipFunctionBase & related classes`
`itk::DecisionRuleBase & related classes`
Other filters: morphological, connected component labeling, threshold filters etc.

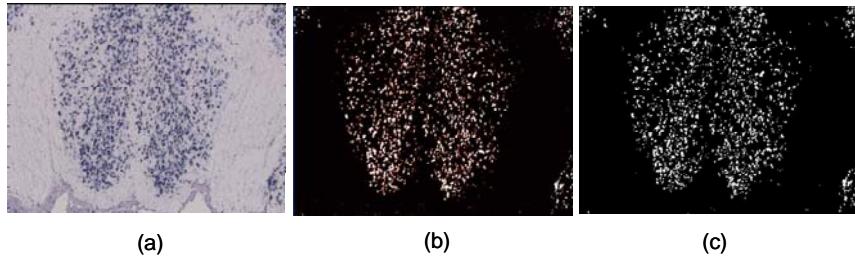
Requirements

Modular design / code reuse
Careful memory usage (each 2D image is on the order of 150 MPixels)
Robust and adaptable to change in image quality

*Courtesy of Dr. Lydia Ng, Allen Institute for Brain Science, www.brainatlas.org.



Classifier Framework Example



(a) Original ISH stained image; (b) heat map representing the membership values of each pixel representing expression, and (c) the final threshold mask generated from the heat map



Region Growing

Idea

Start with set of **seed pixels** – region

Iteratively include neighboring pixels that satisfy
membership criteria

Membership criteria – similarity based metrics

Intensity interval, Regional statistics

Algorithms

Simple to complex variations

Easy to write using ND neighborhood tools

Several strategies

Connected Threshold, Otsu Threshold, Neighborhood

Connected, (Vector) Confidence Connected, Isolated

Connected

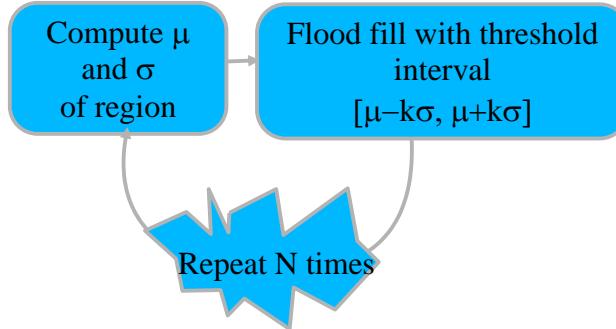


Confidence Connected Filter

Threshold based region growing

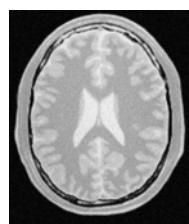
Mean and standard deviation of region determine
upper and lower thresholds

Recomputes thresholds at intervals



Region Growing Segmentation

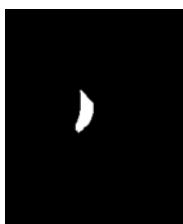
ConfidenceConnectedImageFilter



original



white matter
(60,116)



ventricle
(81,112)



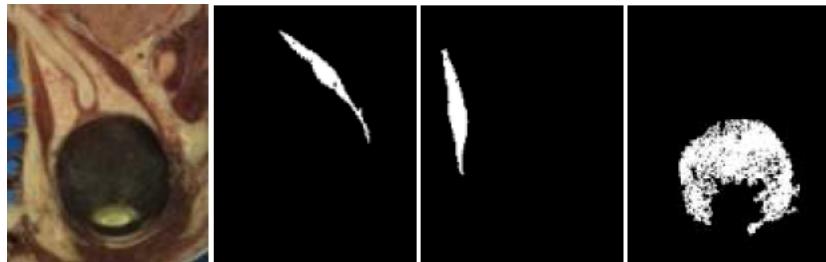
gray matter
(107,69)

smoothing iterations 5
smoothing time step 0.125
C.C. multiplier 2.5
C.C. iterations 5



Region Growing Segmentation

VectorConfidenceConnectedImageFilter



Watershed Segmentation

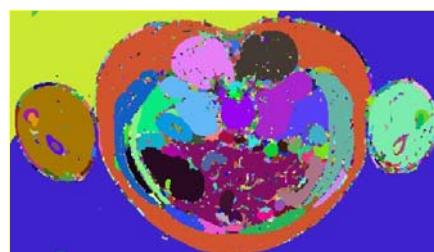
Image treated as a topological relief map – intensity represents height

Gradient descent defines ***segmented regions***

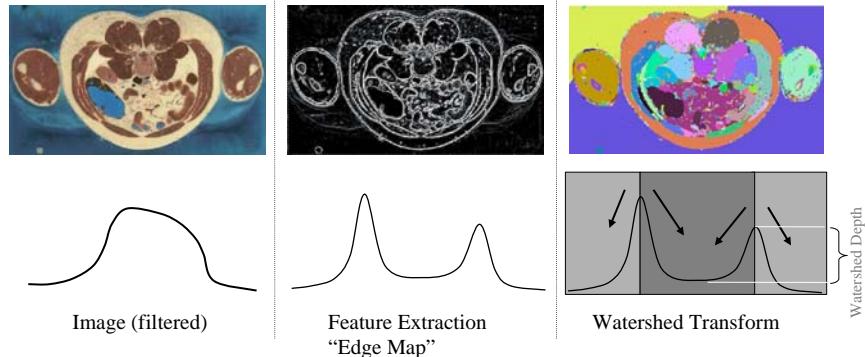
Set of all pixels whose paths of steepest descent terminate in same local minimum

Bounded by image features

“No parameters”



ITK Watershed Transform



The Oversegmentation Problem

Watershed transform produces too many regions

One per local minimum

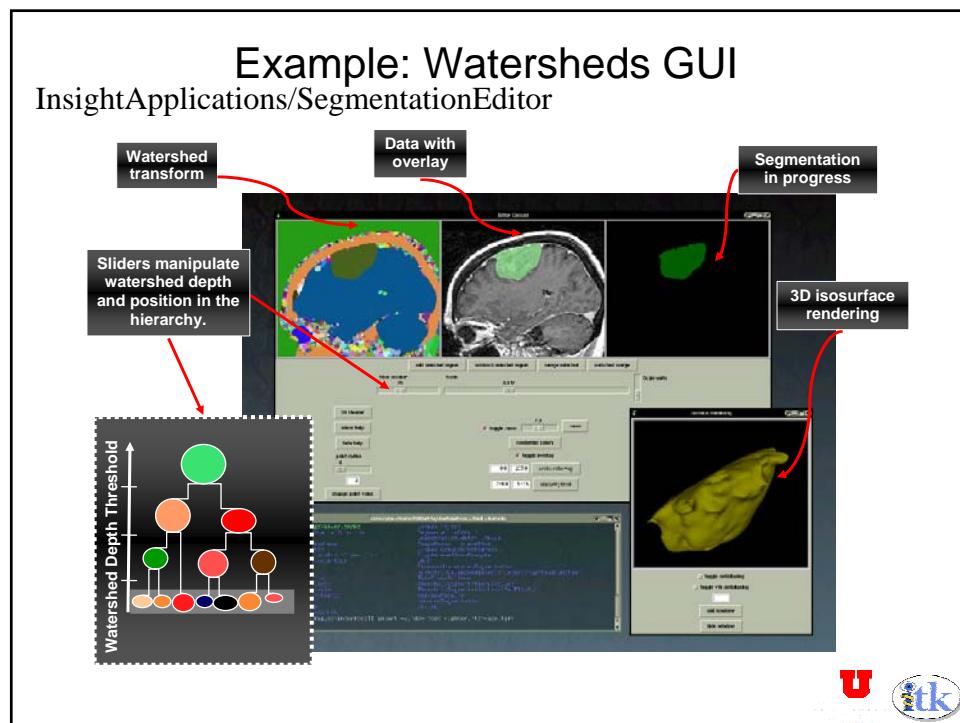
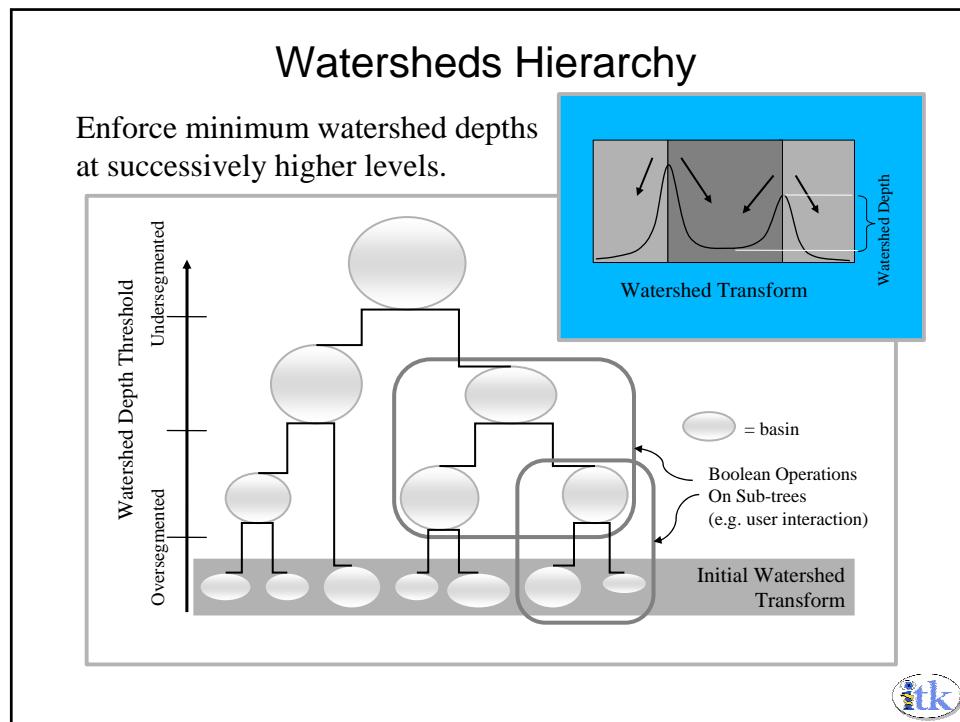
Especially in noisy or highly detailed data

To alleviate oversegmentation

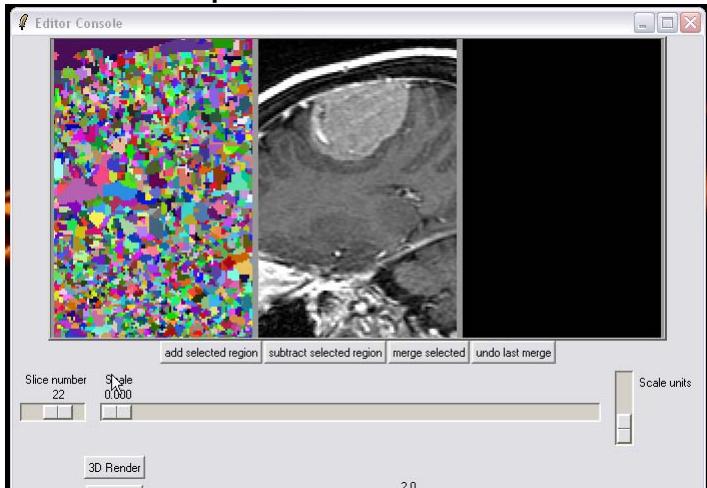
Hierarchical approach – merge adjacent regions according to increasing *watershed depth*

A. P. Mangan, R. T. Whitaker, Partitioning 3D surface meshes using watershed segmentation, IEEE Transactions on Visualization and Computer Graphics 5 (4) (1999) 308–321.

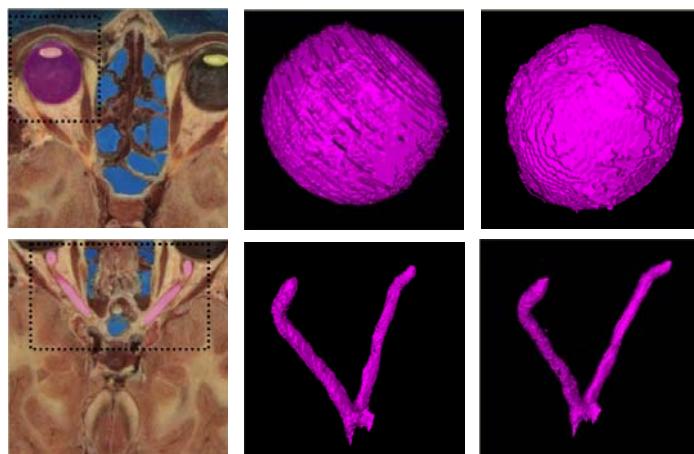




Example: Watersheds GUI



Example: Watersheds GUI

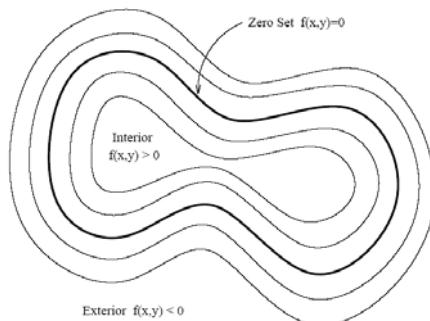


LevelSet Surface Modeling Theory

k^{th} Level Set: set of all points of value k

Embed N dimensional surface as ZERO level set of $N+1$ dim. volume

Model N dim. surface movement as evolving wavefront – forward differences solution to PDE



Ψ								
-2.4	-1.3	-0.6	-0.7	-0.8	-1.8			
-2.4	-1.4	0.3	0.4	0.3	0.2	-0.8	-1.8	
-2.4	-1.4	-0.4	0.6	1.6	1.3	1.2	0.3	-0.8
-1.2	-0.2	0.8	1.8		2.3	1.3	0.3	-0.7
-1.1	-0.1	0.9	0.7	1.7		1.2	0.2	-0.8
-2.5	-1.5	-0.5	0.3	0.7	2.4	1.4	0.4	-0.6
-2.5	-1.5	-1.3	-0.4	1.3	0.3	0.4	-0.6	
			-1.6	-0.6	0.4	-0.7	-0.6	-1.6
				-1.6	-0.6	-1.7		



Segmentation Using Level Sets

Define speed term(s) to go to zero at edges – data fitting term

Surface motion/speed based on intensity-based features

Solve the level-set equation where

$$\tilde{\Gamma}(\mathbf{X}, \mathbf{t}) = \{\psi(\mathbf{X}, \mathbf{t}) = 0\}$$

$$\frac{d}{dt}\psi = -\alpha \mathbf{A}(\mathbf{x}) \cdot \nabla \psi - \beta P(\mathbf{x}) |\nabla \psi| + \gamma Z(\mathbf{x}) \kappa |\nabla \psi|$$



PDE Solver Framework

Purpose

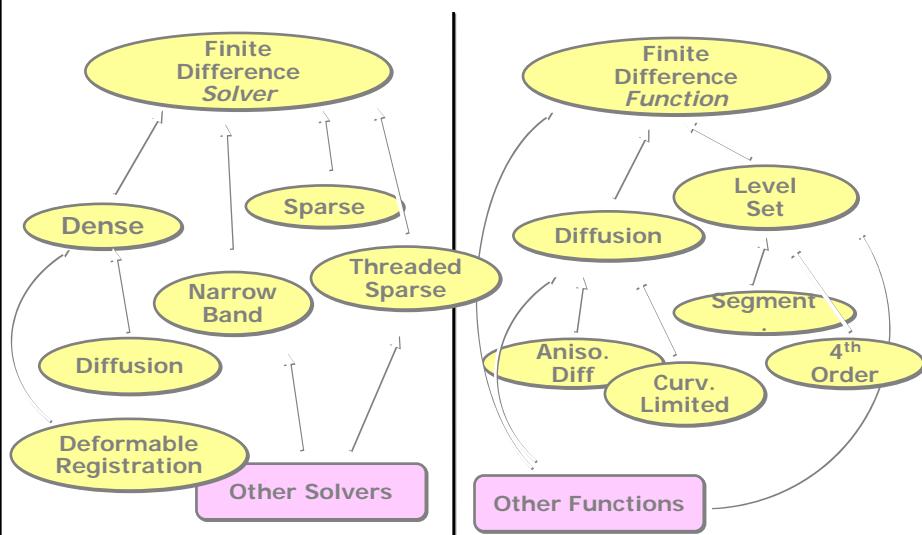
- Nonlinear image processing – e.g. anisotropic diffusion
- Moving wave fronts – level set models
- Deformable registration

Generic framework

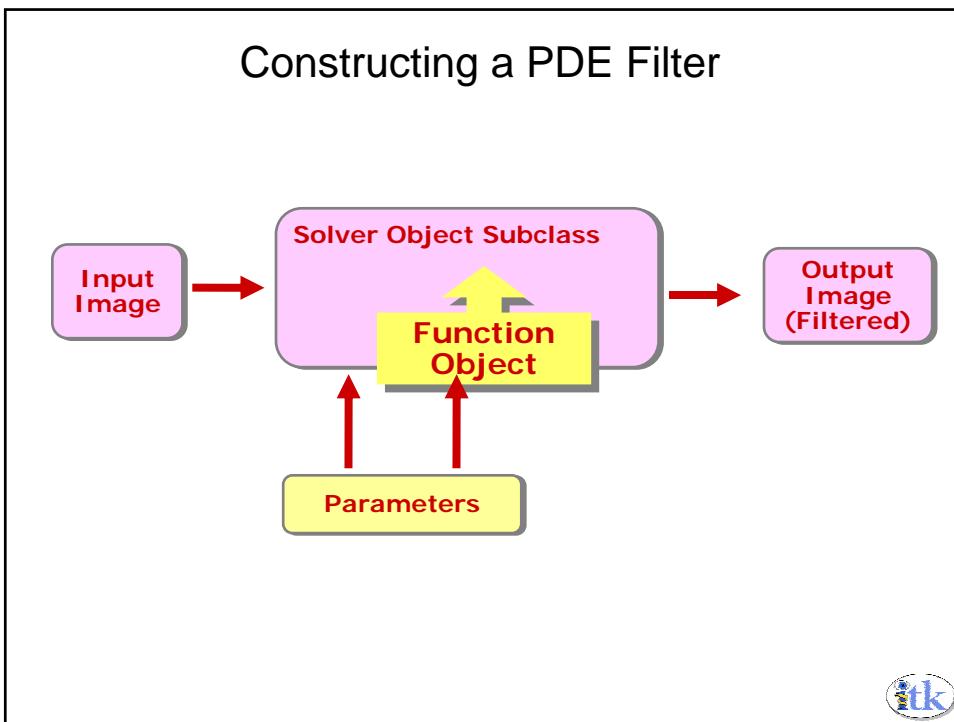
- Separate solvers from equations – *interchangeable* code objects



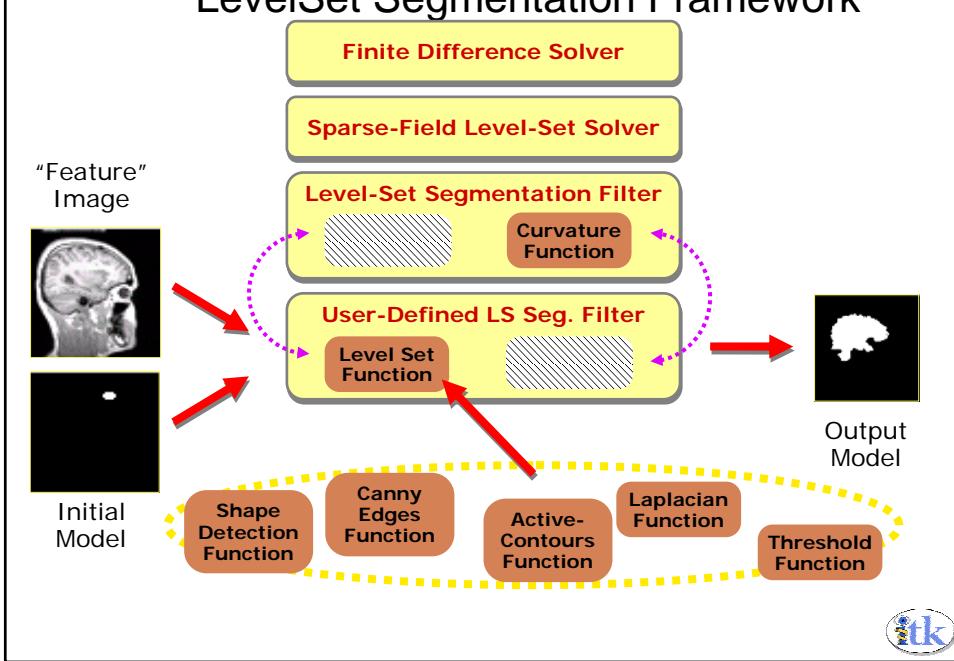
PDE Solver Hierarchy



Constructing a PDE Filter



LevelSet Segmentation Framework



LevelSet Segmentation Algorithms in ITK

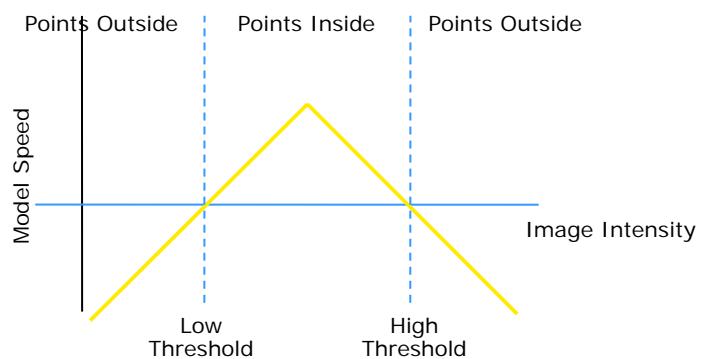
Fast marching
Geodesic active contours
CURVES (vessel segmentation)
Intensity interval (scalar and vector)
Canny edge distance
Laplacian edges

... and more.



Example: Threshold based LS Segmentation

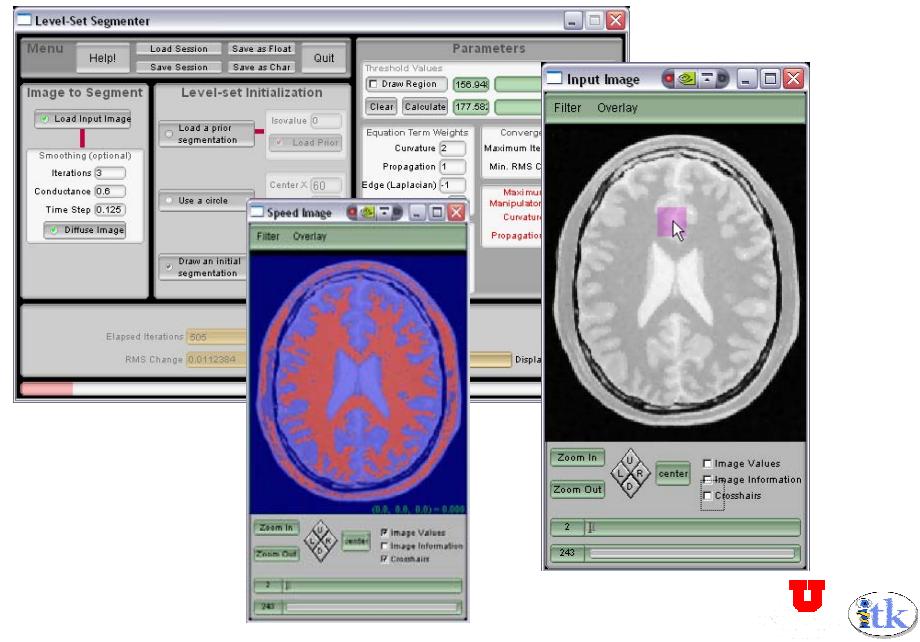
Speed function (positive inside object)
Similar to confidence connected filter



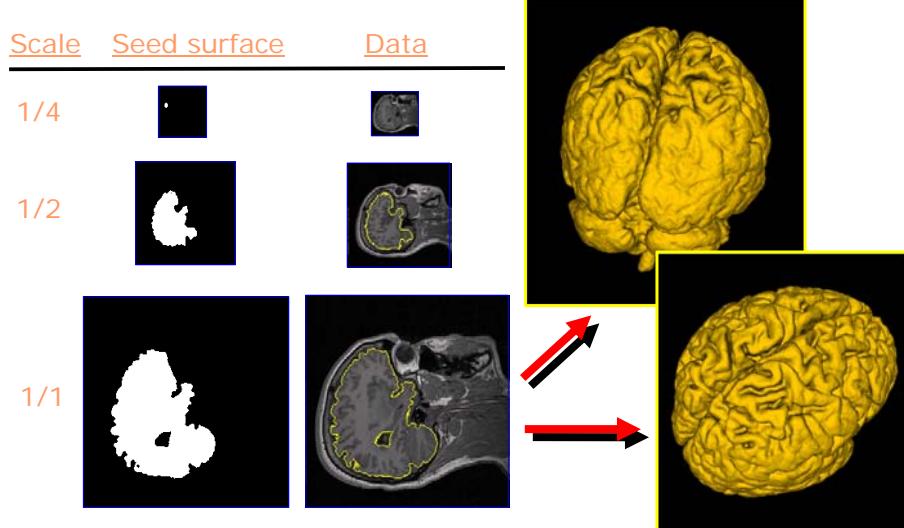
- Lefohn, Kniss, Hansen, Whitaker, "GPU-Based, Interactive, Level-Set Models for Volume Visualization and Analysis", IEEE Vis 2003
- Lefohn, Whitaker, Cates, "Interactive Level-Set Models for Brain Tumor Segmentation", MICCAI 2003



Example: LevelSet Segmentation GUI

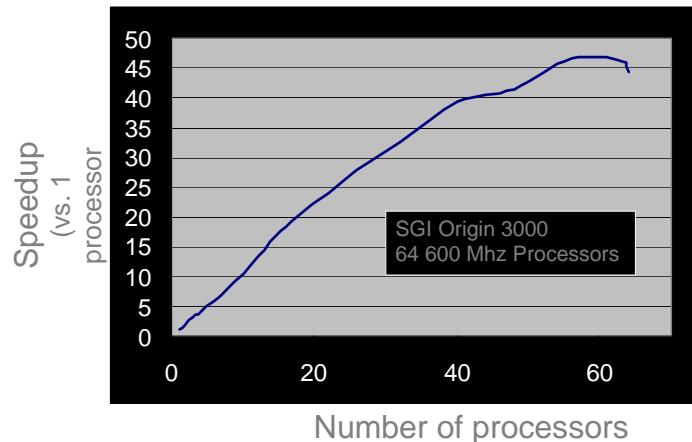


Multiscale LevelSet 3D Segmentation

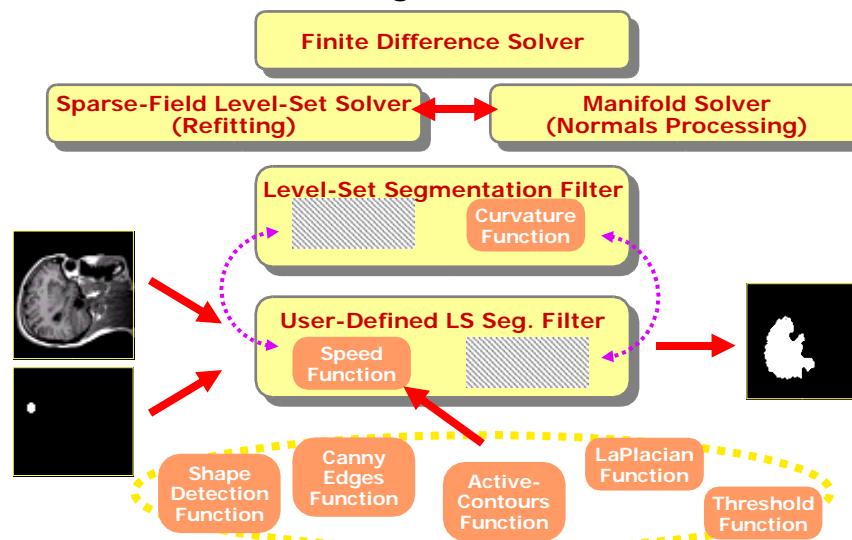


Advanced Features in the PDE Framework

Parallel Solvers – Narrowband,
Sparse field

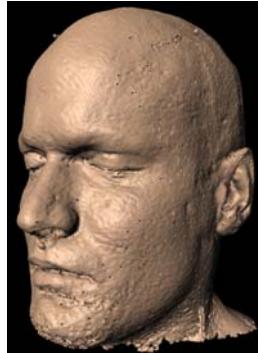


4th Order Flow Segmentation Framework

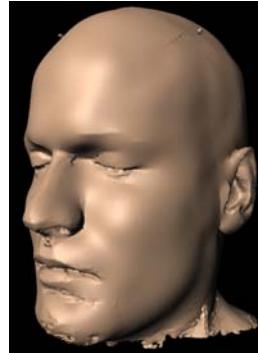


Segmentation Using 4th Order Flows

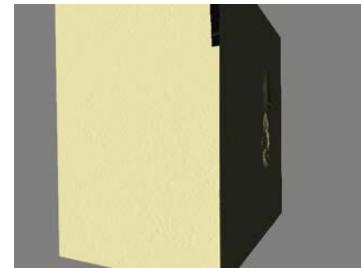
Special 4th order solver plugs into LS segmentation framework – no change in function objects.



Speed term only



Speed + Anisotropic
4th order terms



(not real-time)



SNAP Tool

Aimed at clinical users – easy to learn and use

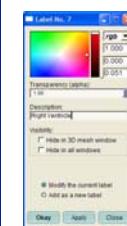
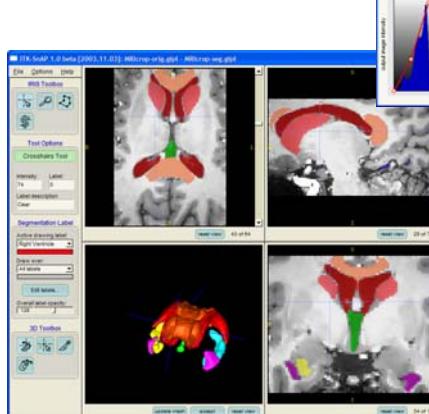
Implements various ITK level set algorithms

Implements both edge-based and

region competition

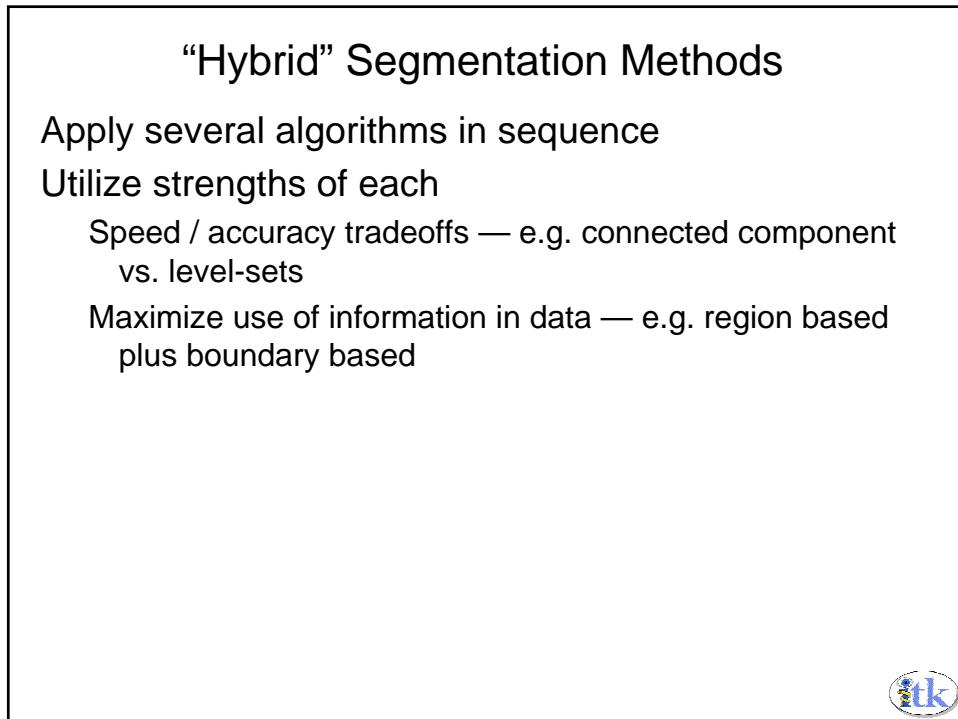
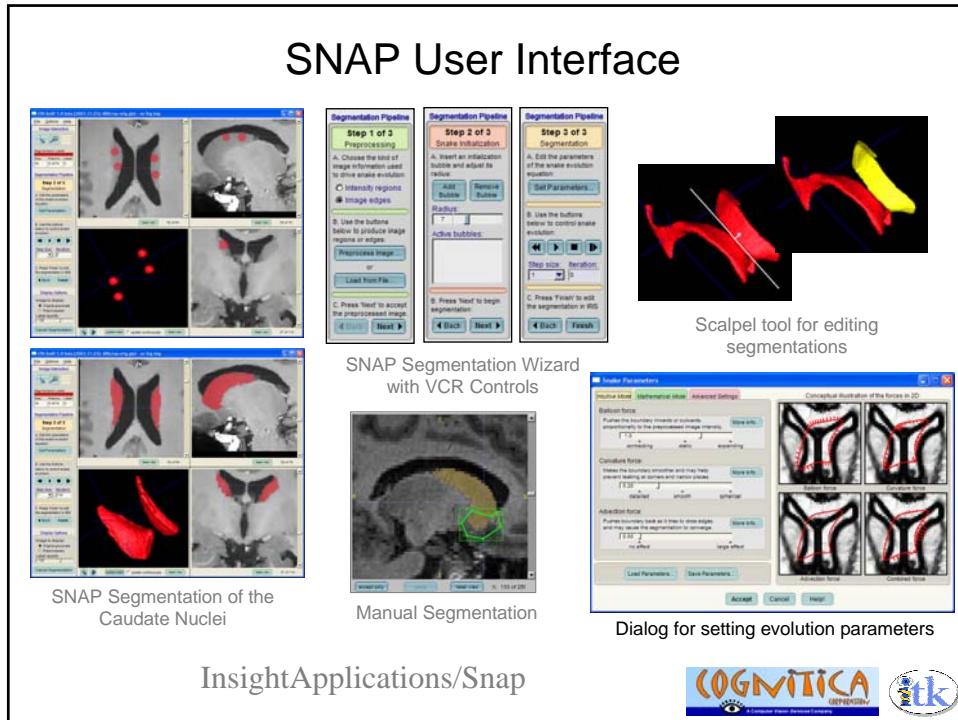
geodesic snake

methodology



InsightApplications/Snap

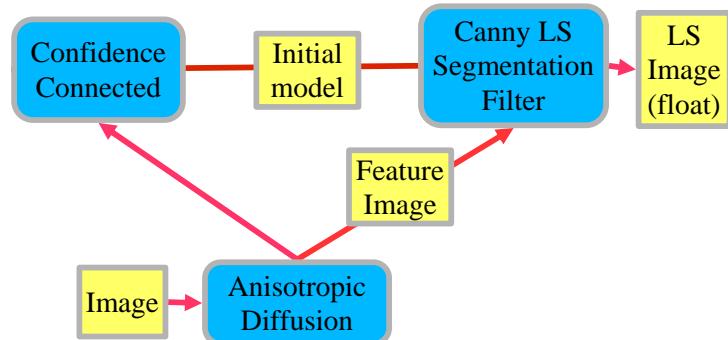




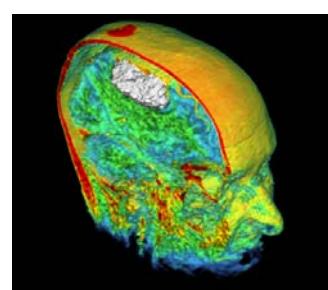
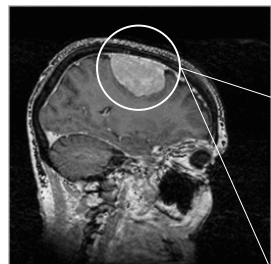
Hybrid Method: Region Growing + Level Sets

Generate initial model using confidence connected filter

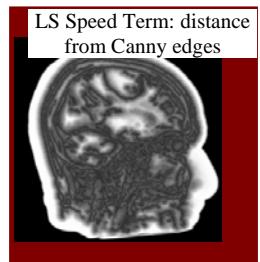
Fit to data using level-set methods – minimize distance to Canny edges



Confidence Connected + LevelSet Result



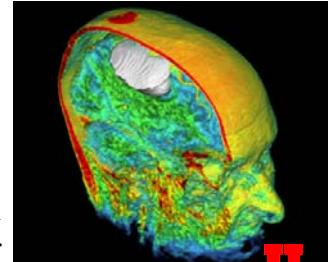
Initial confidence-connected result



LS Speed Term: distance from Canny edges



Post-processing with Canny LS segmenter



Data: Warfield, Nabavi, Butz, Tuncali, Silverman, "Intraoperative segmentation and nonrigid registration for image guided therapy, in: MICCAI'2000, SpringerVerlag, 2000, pp.176-185."





enjoy ITK!

<http://www.itk.org>





Overview: ITK Registration Methods

Lydia Ng

Allen Institute for Brain Science

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1

Overview

- Introduction
- ITK Registration Framework
 - Component Overview
 - Registration Strategies
 - GUI Communication
- Deformable Registration in ITK
- Resources
- Application: Allen Brain Atlas



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Introduction

- **Image registration**

- Process of finding the spatial transform that maps all points from one image to their homologous points in another image

- **Medical applications**

- Monitoring change in an individual
 - Fuse information from multiple sources to aid clinical interpretation
 - Compare one subject to another



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Intra-subject Registration

- Repeated image scans of the same subject can be used to capture the effect of disease development, treatment progress, contrast bolus propagation etc.
- Registration can be used to compensate for differences in patient placement
- Subtraction/overlay of registered images can be used for visualization and quantification



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3D Breast MR Contrast Uptake Deformable Registration

Unregistered:

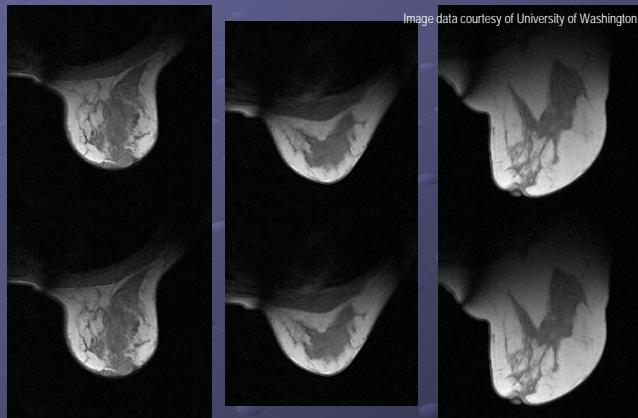


Image data courtesy of University of Washington.

Registered:

Image Data: 192 x 192 x 13 pixels, 0.94 x 0.94 x 8.00 mm
Registration: 2 levels, MI, LBFGS, B-spline deformation



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Inter-subject Registration

- Creation of mean images and atlases
 - Useful for objective and quantitative assessment of abnormalities
 - Computed deformation field used to encode pattern of anatomic variability within a population
- Atlas based segmentation
 - Automatic segmentation by mapping to a labeled atlas



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3D Inter-subject MR-PD Deformable Registration

Image data courtesy of N. C. Andreasen, University of Iowa, Psychiatry Dept.

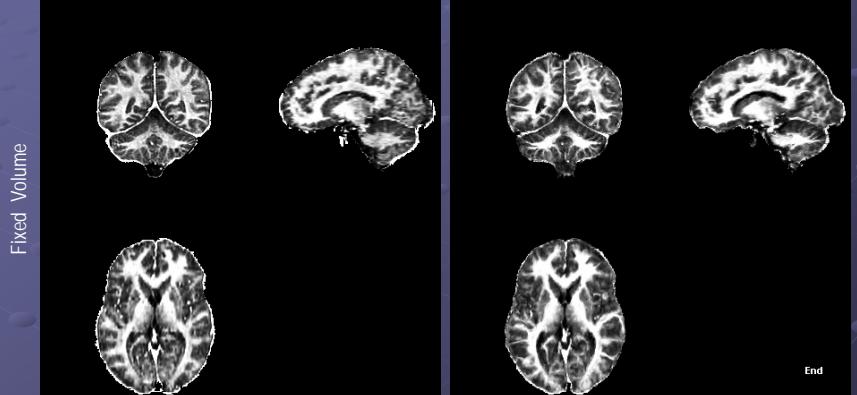


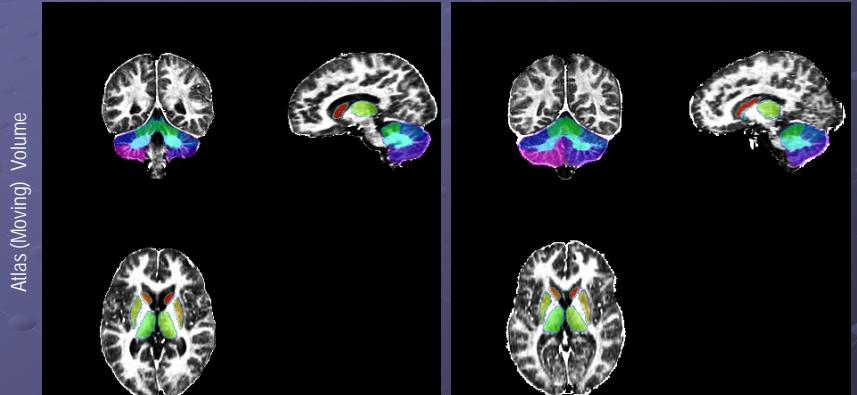
Image Data: 256 x 256 x 192 pixels, 1.02 x 1.02 x 1.02 mm
Registration: 3 levels, Demons algorithm, histogram matching



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3D Atlas-based Segmentation

Image data courtesy of N. C. Andreasen, University of Iowa, Psychiatry Dept.



8

Multi-modality Registration

- Combine or fuse information from multiple sources to aid clinical interpretation
- Some modalities
 - MR: soft tissue discrimination; lesion identification
 - CT: bone localization; surgical guidance
 - PET/SPECT: functional information; tumor localization

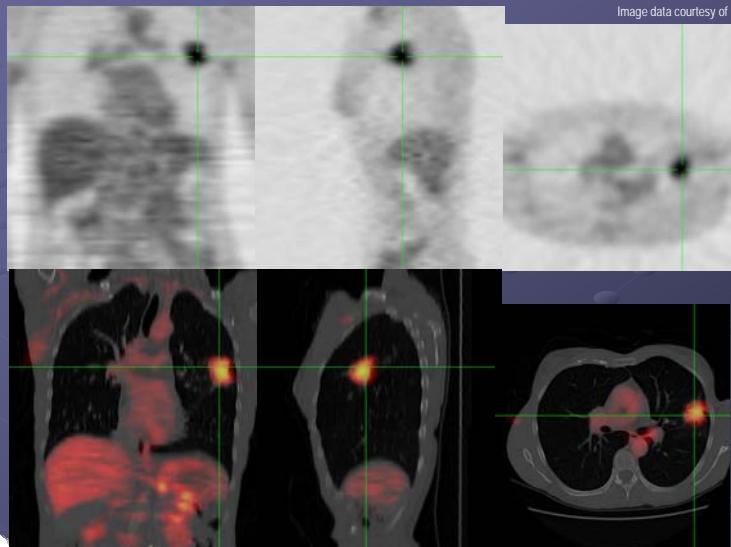


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PET/CT Fusion

Image data courtesy of University of Washington.



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Image Registration Classification

- Registration criteria
 - Quantitative measure of a “good match”
 - Focus on intensity based measures
- Spatial transform type
 - Allowable mapping from one image to another
 - Rigid versus non-rigid
- Optimization algorithm used
 - Optimize transform parameters with respect to match criteria
- Image interpolation method
 - Value of image at non-grid position



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ITK Registration Framework



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ITK Registration Framework

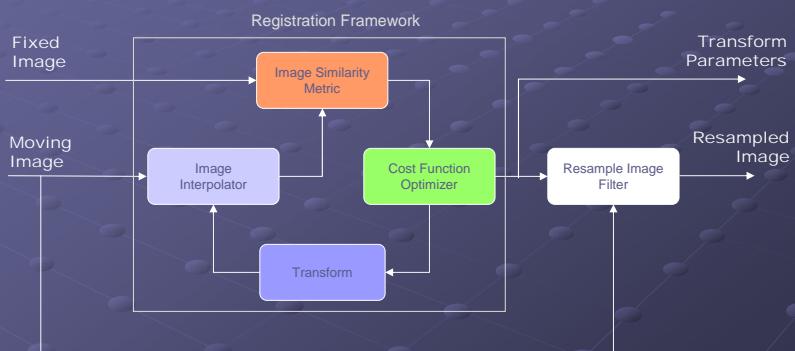
- Generic framework for building intensity based registration algorithms
- Each functionality encapsulated as components
- Components are inter-changeable allowing a combinatorial variety of registration methods
- Components are generic
 - Can be used outside the registration framework



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Registration Framework Components



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itk::ImageRegistrationMethod

- Simple helper driver class that connects up the components and starts the optimizer
- Examples in Software Guide



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Examples/Registration

- Declare types
- Instantiate objects via New()
- Connect components and images to the driver using Set methods
- Set initial transform parameters
 - Don't forget!
- Setup each component
 - optimization parameters: step length, convergence ...
 - MI parameters: number of samples,
- Connect up observers
- StartRegistration()
 - Should do this inside try/catch block
- Get the last transform parameters
- Create registered image using ResampledImageFilter



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Component Overview

- **Transforms**
 - Forward versus inverse mapping
 - Rigid and non-rigid
- **Interpolators**
- **Image to image similarity metrics**
 - Intra-modality
 - Inter-modality (information-theoretic methods)
- **(Optimizers)**



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itk::Transform

- Encapsulates the mapping of points and vectors from an “input” space to an “output” space
- ITK provides a variety of transforms from simple translation, rotation and scaling to general affine, kernel and B-spline transforms
- Forward versus inverse mapping
- Parameters representation
- “Transform Jacobians”



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Forward and Inverse Mappings

- Relationship between points of two images can be expressed in two ways:
 - Forward: pixel of input (moving) image mapped onto the output (fixed) image
 - Inverse: output (fixed image) pixels are mapped back onto the input (moving) image

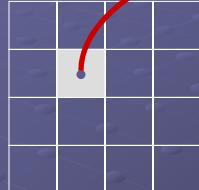


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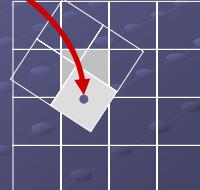
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Forward Mapping

Input Image



Output Image



- Input image pixel is mapped onto the output image
- Output pixels with more than one hit: overlap
 - Value must be accumulated from overlapping pixels
- Output pixels with no hits: hole

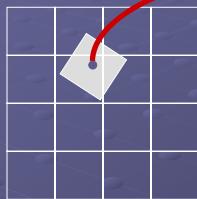


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Inverse Mapping

Input
Image



Output
Image

- Output pixels are mapped back onto the input image
- Output pixel value must be interpolated from a neighborhood in the input image
- Scheme avoids any holes and overlaps in the output image because all pixels are scanned sequentially



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Registration and Inverse Mapping

- The registration framework uses **inverse** mapping
- The transform component maps points from the **fixed** image space to the **moving** image space

$$\mathbf{x}' = \mathbf{T}(\mathbf{x}|\mathbf{p})$$

Point in moving image space

Point in fixed image space



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Transform Parameters

- Each transform class is defined by a set of parameters
 - Translation, angle of rotation etc
- Represented as a flat array of doubles to facilitate communication with generic ITK Optimizers
- Transform parameters define the search space for the optimizer
- Goal of registration
 - Find the set of transform parameters that result in the best value of an image similarity metric



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Transform Jacobian

- Some metrics require the knowledge of the “transform Jacobian” in order to compute metric derivatives
- The “transform Jacobian” is a matrix whose elements are the partial derivatives of the output point with respect to the transform parameters

$$J_{ij} = \frac{\partial x'_i}{\partial p_j}$$



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itk::TranslationTransform

- Maps all points by adding a constant vector:

$$\mathbf{x}' = \mathbf{x} + \mathbf{t}$$

- Parameters:

- i-th parameter represent the translation in the i-th dimension

$$\mathbf{p} = \mathbf{t}$$

- Jacobian in 2D:

$$\mathbf{J} = \begin{bmatrix} 1 & 0 \\ 0 & 1 \end{bmatrix}$$



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itk::Euler2DTransform

- Represents a rotation and translation in 2D

$$\begin{bmatrix} x' \\ y' \end{bmatrix} = \begin{bmatrix} \cos \theta & -\sin \theta \\ \sin \theta & \cos \theta \end{bmatrix} \begin{bmatrix} x \\ y \end{bmatrix} + \begin{bmatrix} t_x \\ t_y \end{bmatrix}$$

- Parameters:

$$\mathbf{p} = \{\theta, t_x, t_y\}$$

- Jacobian:

$$\mathbf{J} = \begin{bmatrix} -(\sin \theta)x - (\cos \theta)y & 1 & 0 \\ +(\cos \theta)x - (\sin \theta)y & 0 & 1 \end{bmatrix}$$



Don't forget TRANSFORM
CENTERING and PARAMETER SCALING!

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Center of Transformation/Rotation

- Transformation/rotation is about the origin {0,0}
- Can represent rotation at arbitrary rotation center but at the expense of optimization performance, especially for large auxiliary translation

$$\begin{aligned}\mathbf{x}' - \mathbf{c}_m &= \mathbf{M}(\mathbf{x} - \mathbf{c}_f) + \mathbf{t} \\ \mathbf{x}' &= \mathbf{M}\mathbf{x} + \underbrace{(\mathbf{t} + \mathbf{c}_m - \mathbf{M}\mathbf{c}_f)}_{\mathbf{t}'}\end{aligned}$$

- Alternatives:
 - center of image
 - center of mass of an object



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Parameter Scaling

- Different type of parameters (translation vs. angle vs. scaling) have different dynamic ranges
 - E.g. a unit change in rotation has a much larger impact than a unit change in translation
- Differences in scale appears as long narrow valleys in the search space making optimization difficult
- Rescaling the parameters can help fix this problem



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itk::Euler3DTransform

- Represents 3D rotation and translation
 - Rotation about each coordinate axis
 - Ordering matters!

$$\mathbf{x}' = \mathbf{R}_z \mathbf{R}_y \mathbf{R}_x \mathbf{x} + \mathbf{t}$$

or

$$\mathbf{x}' = \mathbf{R}_z \mathbf{R}_x \mathbf{R}_y \mathbf{x} + \mathbf{t}$$

- Parameters:

$$\mathbf{p} = \{\theta_x, \theta_y, \theta_z, t_x, t_y, t_z\}$$



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Alternative 3D Rigid Transforms

- itk::QuaternionRigidTransform
 - 3D rotation represented by a quaternion
 - Represented by 4 numbers
 - Similar to axis/angle representation
 - Unit quaternion is equivalent to pure rigid
 - Does not suffer from “Gimbal lock”
- itk::VesorRigidTransform
 - Strictly the rotational part of a quaternion (always rigid)
 - Represented by 3 numbers
- Both quaternion and vesor components do not form vector spaces
 - Specialized optimizers required!



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I will not register images in pixel space
I will not register images in pixel space



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Image Spacing and Origin

- Medical image volume are typically anisotropic
 - In-plane pixel size smaller than inter-slice spacing
- A transform is rigid only with respect to physical coordinates and not pixel coordinates
 - $\text{PhysCoord} = \text{PixelCoord} \times \text{ImageSpacing} + \text{ImageOrigin}$
- The registration is always with respect to physical coordinates
- Make sure spacing and origin information is set correctly in the images!



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itk::AffineTransform

- General affine transform can represent rotation, scaling, shearing and translation
- Parameters: matrix coefficient + translation (6 in 2D, 12 in 3D)
- Parallel lines are preserved



Don't forget TRANSFORM
CENTERING and PARAMETER SCALING!



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itk::BSplineDeformableTransform

- Represent a low-dimensional smooth deformable warp
- Deformation field represented by B-splines coefficient on a regular grid
- Parameters: B-spline coefficient for each dimension at each grid position

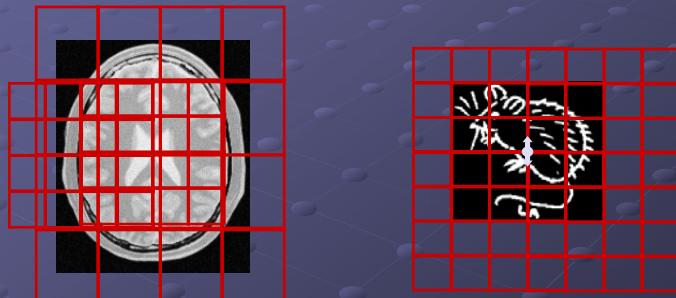


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B-Spline Grid Placement

- Grid defined by origin, spacing, size



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itk::InterpolateImageFunction

- When a point is mapped from one image space to another image space, it will generally be mapped to a non-grid position
- Interpolation is needed to compute the intensity value at the mapped position



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Choice of Interpolation Method

- Interpolation affects smoothness of metric space
- Interpolations computed 1000's of times in a single optimization cycle
- Trade-off efficiency with ease of optimization



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Interpolation Schemes

- `itk::NearestNeighborInterpolateFunction`
 - Assumes image is piecewise constant
- `itk::LinearInterpolateFunction`
 - Assumes image is piecewise linear
- `itk::BSplineInterpolateFunction`
 - Underlying image represented using B-spline basis functions
 - On connection, image of B-spline coefficients is computed



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itk::ImageToImageMetric

- Measures how well a transformed moving image “matches” the fixed image
- The most critical component
- Scalar function of the transform parameters
 - For given, fixed image, moving image, transformation type and interpolation type

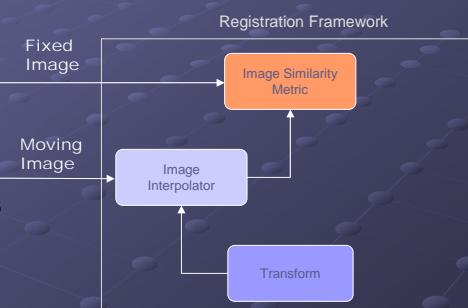


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Metrics, Transforms and Interpolators

- The **metric** typically samples points within a defined region of the fixed image
- For each point, the corresponding moving image point is obtained using the **transform** component
- The **interpolator** component is then used to compute the moving image intensity at the mapped position

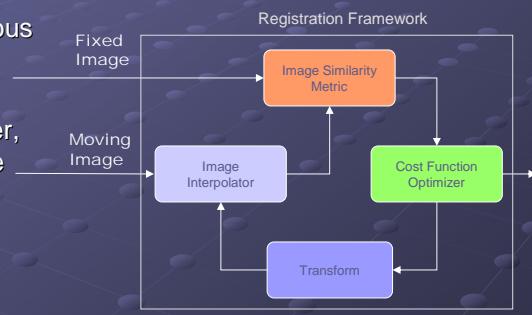


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Metrics and Optimizers

- The **metric** is used by the **optimizer** to evaluate the quantitative criterion at various positions in the transform parameter search space
- For gradient-based optimizer, the metric must also provide the metric derivatives w.r.t each transform parameter
 - Use chain rule with moving image derivatives and transform Jacobian



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Choice of Metric

- Highly dependent on the registration problem to be solved
 - Single-modality
 - Multi-modality
 - Large capture range
 - Requires close initialization
- Examples:
 - Mean squares, normalized correlation and mutual information



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Mean Squares Metric

Interpolate the moving image

$$S(\mathbf{p}|F, M, \mathbf{T}) = \frac{1}{N} \sum_i^N (F(\mathbf{x}_i) - M(\mathbf{x}'_i))^2$$

where

Transform from fixed image point to moving image point

Over a user specified fixed image region

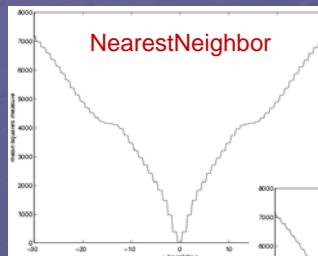
- Simple to compute
- Large capture range
- Restricted to mono-modality applications
- Linear differences in intensity results in poor similarity measure



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Mean Squares Metric

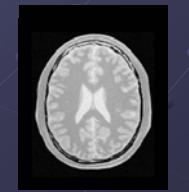


Optimal Value at Zero

BSpline

Linear

Metric range:
image dependent



Translations



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Normalized Correlation Metric

$$S(\mathbf{p}|F, M, \mathbf{T}) = -1 \times \frac{\sum_i^N F(\mathbf{x}_i)M(\mathbf{x}'_i)}{\sqrt{\sum_i^N F^2(\mathbf{x}_i) \sum_i^N M^2(\mathbf{x}'_i)}}$$

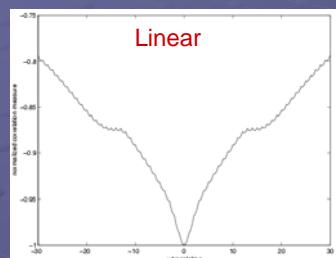
- Pixel-wise cross-correlation between fixed and moving image intensity
- Factor -1 added to work with minimum seeking generic optimizers
- Insensitive to multiplicative difference



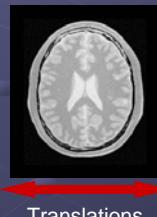
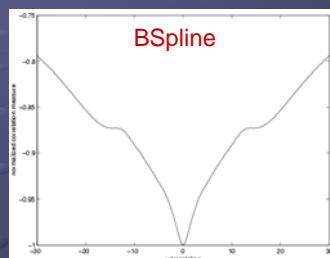
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Normalized Correlation Metric



Optimal Value at
-1
Metric range:
1 to -1



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Mutual Information Metric

- Information theoretic entity that qualitatively measures how much information is gained about one RV (intensity in one image) by the knowledge of another RV (intensity in another image)



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Mutual Information Metric

- Introduced in the context of multi-modality registration by two different groups: Viola and Wells (1997) and Collignon et al. (1995)
- MI well suited since actual form of dependency between the two RVs does not have to be specified
- MI defined in terms of entropy
 - Measure of information contained in a piece of data



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Entropy

- Two RVs: A and B
- Marginal entropies:

$$H(A) = - \int p_A(a) \log p_A(a) da$$

$$H(B) = - \int p_B(b) \log p_B(b) db$$

- Joint entropy:

$$H(A, B) = - \int p_{AB}(a, b) \log p_{AB}(a, b) da db$$



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Mutual Information

- If A and B independent:

$$H(A, B) = H(A) + H(B)$$

- If A and B not independent:

$$H(A, B) < H(A) + H(B)$$

- The difference is MI:

$$I(A, B) = H(A) + H(B) - H(A, B)$$



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Estimating the Probabilistic Models

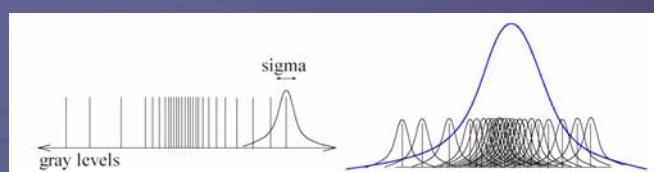
- Entropy is defined in context of a probabilistic model of the data source
 - Typically there is no direct access to these models
- Marginal and joint densities has to be estimated from the image data
 - Parzen windowing
 - Kernel density estimate
 - Histogram binning



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Parzen Windowing



- Density function is constructed by superimposing kernel functions centered on the intensity samples obtained from the image
- Kernel type
 - Gaussian, boxcar, B-Spline
- Kernel width (crucial)
 - Depend on dynamic range of data
 - Normalize data
- Number of samples



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Estimating Entropy

- Using the density estimate, approximate entropy integral by a sum
 - Evaluate at discrete positions/bins uniformly spread within dynamic range
 - Computing a sampled mean using another set of intensity samples randomly drawn from image



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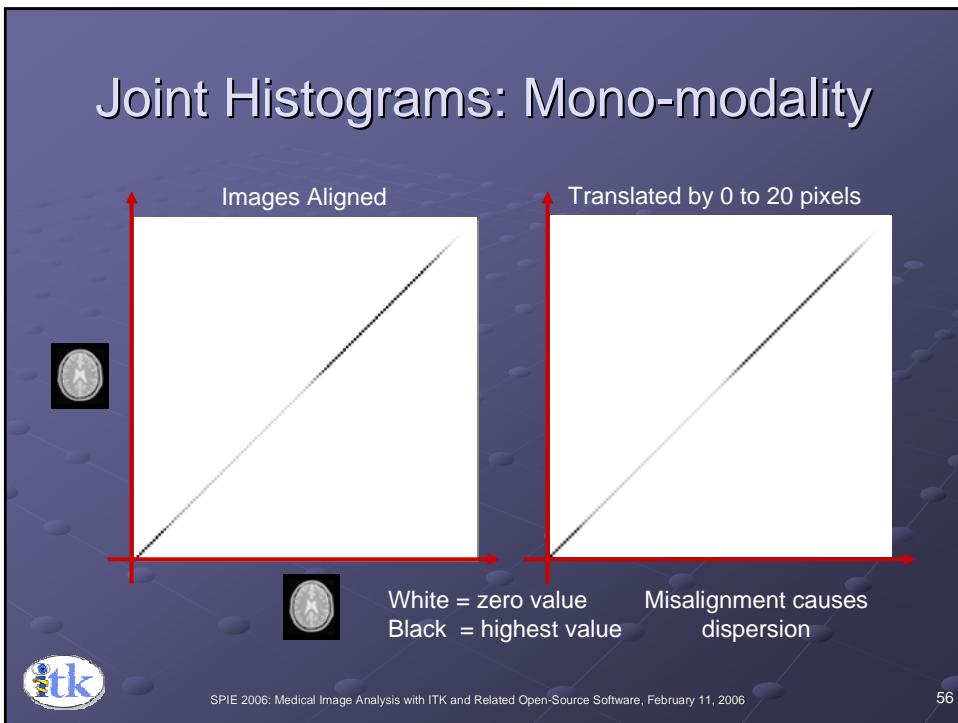
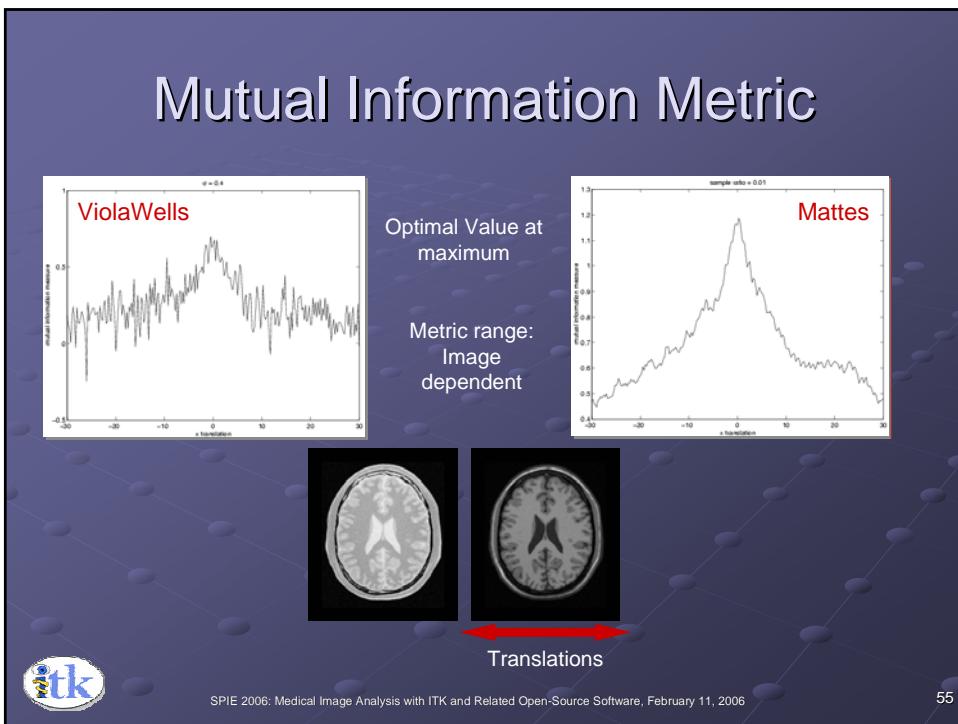
Flavors of Mutual Information

- `itk::MutualInformationImageToImageMetric`
 - Viola and Wells
 - New samples (50-100) each iteration
- `itk::MattesMutualInformationImageToImageMetric`
 - Mattes et al, Thevenaz and Unser
 - One set of samples (5-10% of image)
- `itk::MutualInformationHistogramImageToImageMetric`
 - Use all pixels

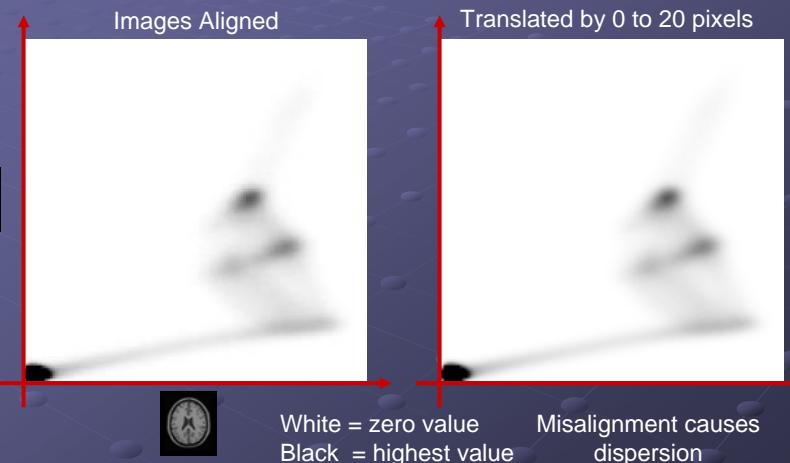


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Joint Histograms: Multi-modality



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Joint Histograms and Registration

- Seek transform that produces a small number of high value bins and as many zero bins as possible == minimizing joint entropy
- Joint entropy metric favors transforms which causes the images to be far apart as possible (i.e. minimum overlap)
- MI overcomes this problem by also trying to maximize the information contributed by each image in the overlap region



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Registration Strategies

- Naive application of registration may not work
- Coarse to fine strategy
 - Improves computational speed and robustness
- Low to high dimensional transform
 - Translation to rigid to deformable
 - Sparse to fine grid

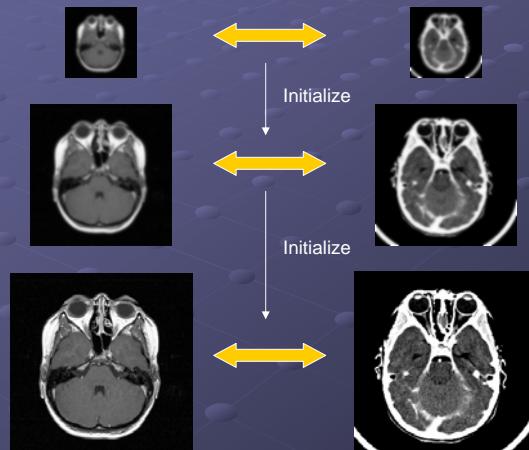


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itk::MultiResolutionImageRegistrationMethod

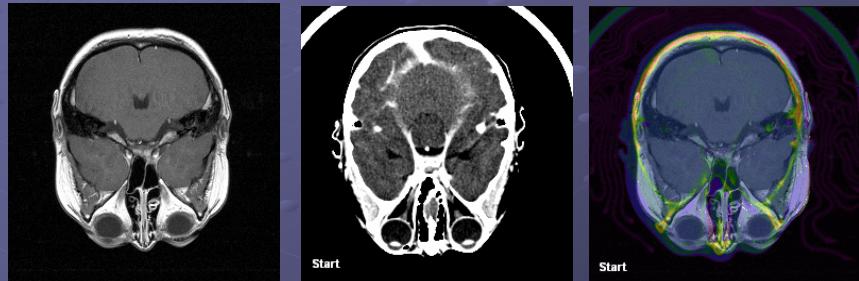
- Helper driver class to perform multi-resolution registration



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3D CT to MR-T1 Rigid Registration



Fixed Image: MR-T1, 256 x 256 x 52 pixels, 0.78 x 0.78 x 3.00 mm

Moving Image: CT, 512 x 512 x 44, 0.41 x 0.41 x 3.00 mm

Registration: 4 levels, MI, gradient descent, quaternion rigid

Images provided as part of the project: "Retrospective Image Registration Evaluation",
NIH, Project No. 8R01EB002124-03, Principal Investigator, J. Michael Fitzpatrick, Vanderbilt University, Nashville, TN.

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3D PET to MR-T2 Rigid Registration



Fixed Image: MR-T2, 256 x 256 x 26 pixels, 1.25 x 1.25 x 4.00 mm

Moving Image: PET, 128 x 128 x 15, 1.94 x 1.94 x 8.00 mm

Registration: 3 levels, MI, gradient descent, quaternion rigid

Images provided as part of the project: "Retrospective Image Registration Evaluation",
NIH, Project No. 8R01EB002124-03, Principal Investigator, J. Michael Fitzpatrick, Vanderbilt University, Nashville, TN.

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Registration To GUI Communication

- Drive progress bar
- Observe registration progress
 - Interrogate metric values
 - Interrogate current parameters
 - Display current results
 - Resample and display ROI
- Change component parameters
- Terminate registration



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ITK Observers/Commands

- `itk::Object` can invoke events
 - Start, End, Progress, Iteration
- `itk::Object` maintains a linked list of event observers
- Observers register themselves to an object and declare the type of events they are interested in



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Observing Registration

- ITK Optimizers typically execute an iterative process
- Most Optimizers invoke an IterationEvent at the end of each iteration
- Observing IterationEvents provide periodic communication facilitating progress feedback and opportunity to control the registration
- `itk::MultiResolutionImageRegistrationMethod` also invokes an IterationEvent between levels to give the GUI an opportunity to change components and/or parameters



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ITK Registration Examples

- ITK Software Guide
 - 9+ examples
- InsightApplications
 - ImageRegistration
 - MRIRegistration
 - MultiResMIRegistration
 - MutualInformationEuler2DRegistration
- Landmark Initialized 3D Registration Tool
 - CADD Lab, UNC



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Deformable Registration in ITK

- Low dimensional transformations can be handled in the basic registration framework
- For high dimensional transformations:
 - Finite Element Methods (FEM)
 - Finite Different Methods
- Metric optimization
 - Mean squares, normalized correlation, MI
- FEM framework additionally supports regularization and landmark constraints:
 - Diffeomorphic constraints
 - Linear elastic and large deformation (fluid and transient-quadratic) models
- Simple examples in Software Guide



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Resources

- ITK Software Guide
- "Insight into Images",
 - Yoo (ed), 2004
- "A Survey of Medical Image Registration"
 - Maintz and Viergever, Medical Image Analysis, 1998
- "Handbook of Medical Imaging: Medical Image Processing and Analysis"
 - Fitzpatrick et al (eds), SPIE, 2000
- "Handbook of Medical Imaging: Processing and Analysis"
 - Bankman (ed.), Academic Press, 2000
- "Medical Image Registration"
 - Hajnal et al (eds), CRC Press, 2001
- "Mutual-Information-Based Registration of Medical Images: A Survey"
 - Pluim et al, IEEE-TMI, 22(8), 2003
- IEEE Transaction of Medical Imaging Special Issue
 - November 2003



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Data for Registration Testing

- Retrospective Registration Project
 - <http://www.vuse.vanderbilt.edu/~image/registration/>
 - Multi-modality images of the brain
- Internet Brain Segmentation Repository
 - <http://www.cma.mgh.harvard.edu/ibsr/>
 - MR-T1 images of brain with segmentations
- BrainWeb
 - <http://www.bic.mni.mcgill.ca/brainweb/>
 - Simulated brain database
- International Consortium For Brain Mapping (ICBM)
 - http://www.loni.ucla.edu/ICBM/ICBM_Databases.html



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Application: Allen Brain Atlas

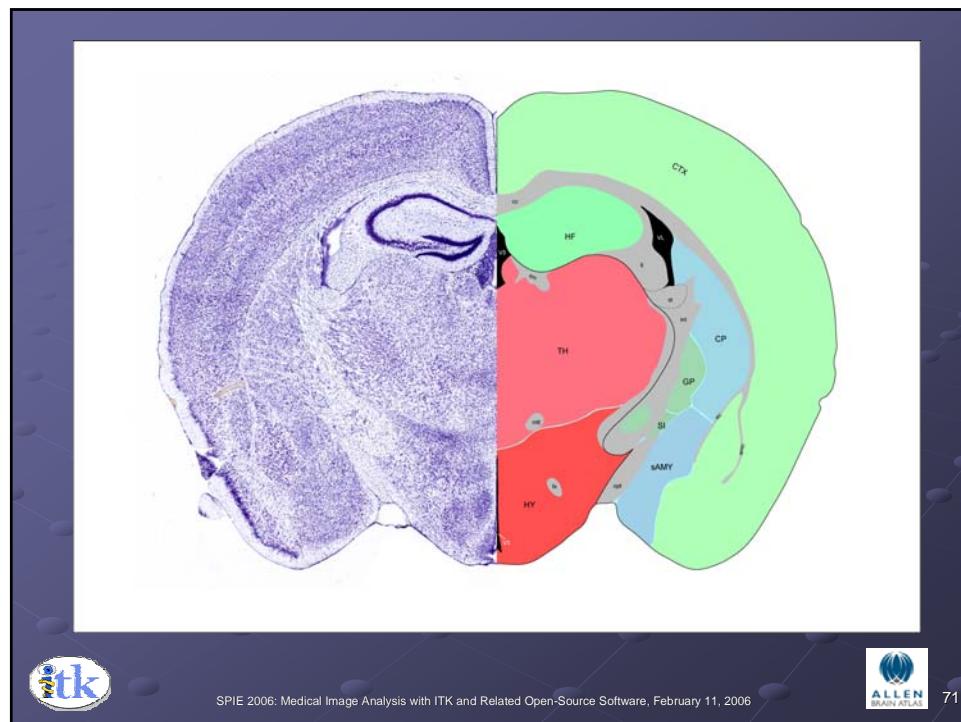
- Detailed, cellular-resolution, genome-wide map of gene expression in the mouse brain
 - <http://www.brain-map.org>
- The Allen Reference Atlas is being developed to allow comparison of the gene expression data in a common anatomic framework
 - Created from 528 coronal sections from fresh frozen tissue
 - 3D reconstruction is needed to take into account differences between specimens and slicing orientation



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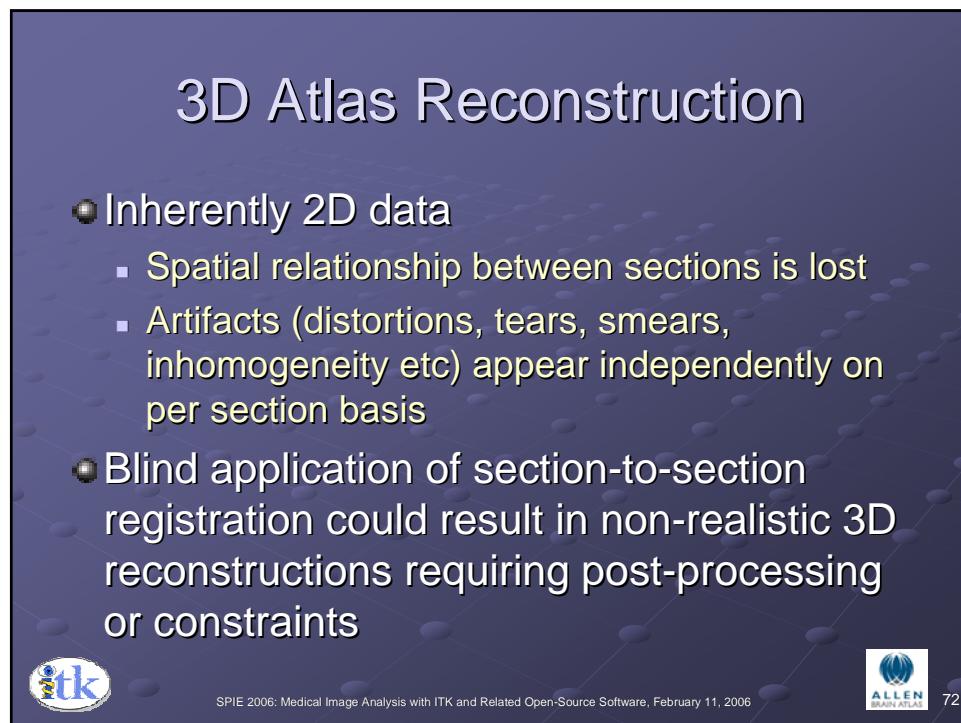
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3D Atlas Reconstruction

- Inherently 2D data
 - Spatial relationship between sections is lost
 - Artifacts (distortions, tears, smears, inhomogeneity etc) appear independently on per section basis
- Blind application of section-to-section registration could result in non-realistic 3D reconstructions requiring post-processing or constraints



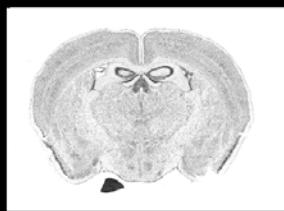
ITK logo

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ALLEN BRAIN ATLAS logo

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Initialization



- 528 coronal images were converted to grayscale, downsampled, cropped and padded to same size
- Brain tissue mask were created to direct from where registration samples information
- Badly damaged sections were removed

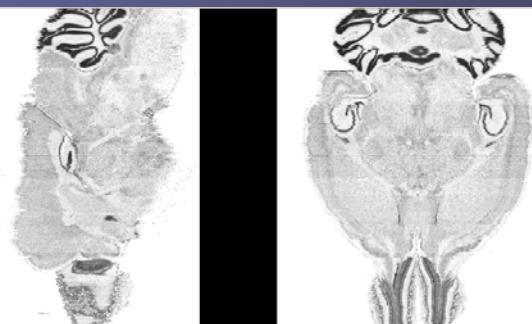
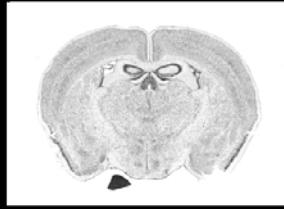


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Rigid Registration



- Section to section rigid registration results in a 3D volume which is fairly self-consistent
- Volume appears bent as registration tend to straighten high gradient features (e.g hippocampus, cerebellum)



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Unbending Rigid Registration



- Unbend the volume by applying the inverse of the smoothed transform series
- Result is then used as initialization for the next step: affine registration

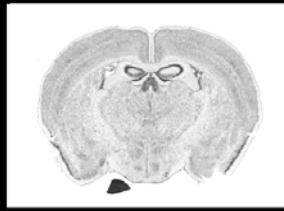


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Affine Registration



- Section to section affine registration results in very smooth structures but causes severe warping
 - Due to straightening out of the hippocampus and cerebellum

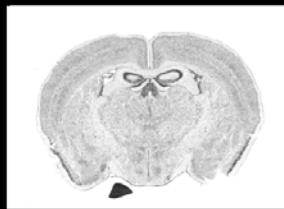


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De-warping Affine Registration



- De-warp the volume by applying the inverse of the smoothed transform series
- Result is then used as initialization for the next step: deformable registration

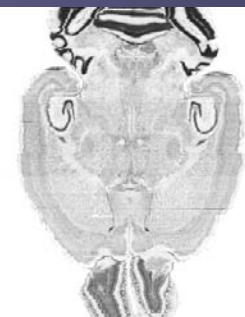
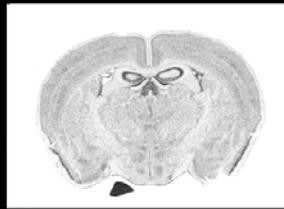


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Deformable Registration



- Section to section deformable registration
 - Constraint movement to less than 125 microns
 - Cleaned up jags in hippocampus and cerebellum
 - Appearance of very fine line structures

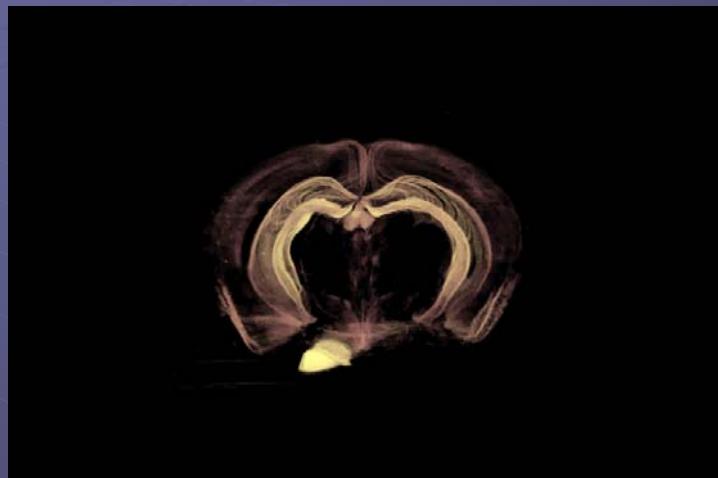


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Hippocampus (Azimuth)

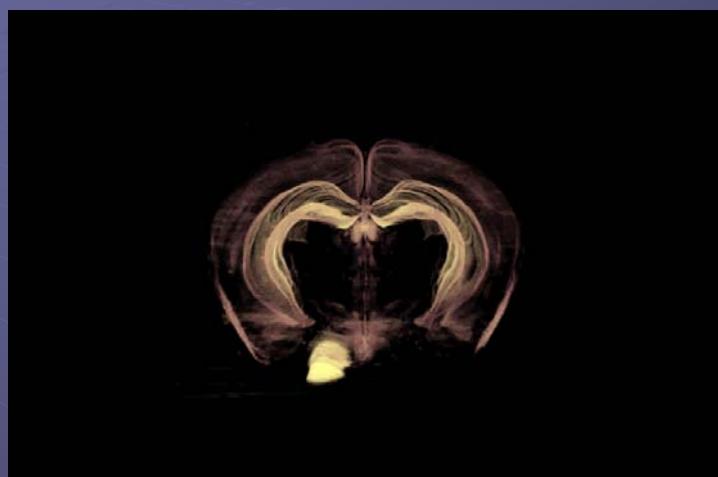


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Hippocampus (Elevation)



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Cerebellum (Elevation)



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Ventricles (Elevation)



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Overview

- IO Factory Mechanism
- Image File IO
- Transform File IO
- SpatialObject File IO
- Logger

IO Factory Mechanism

Why do we need a Factory?

How many file formats can you list?

...

(and many more exist...)

Supported file formats

2D Only

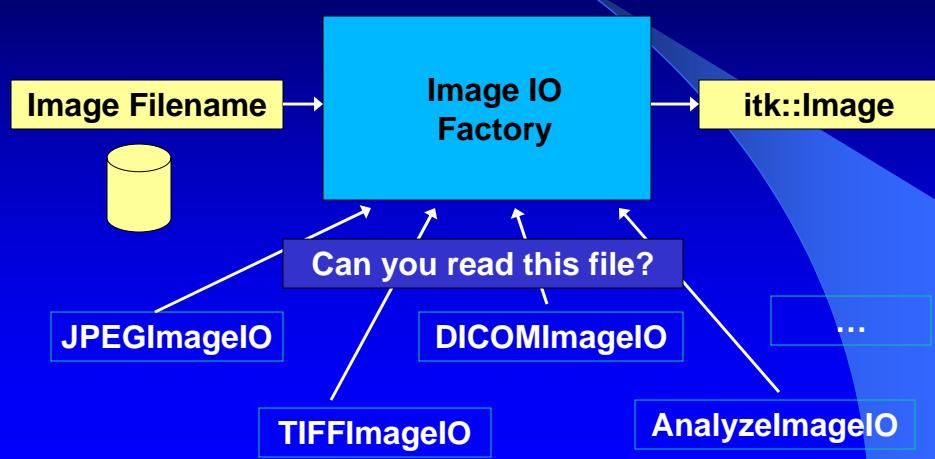
- JPEG (.jpg/.jpeg)
- Bitmap (.bmp)
- PNG (.png)

2D/3D

- Analyze 3.5	- Siemens
- GIPL (.gipl)	- Stimulate
- RAW (.raw)	- TIFF
- DICOM	- VTKImage
- GE 4x,5x	- NRRD
- IPLCommon	- LSM
- MetaImage (.mha/.mhd)	- NIFTI

How does the Factory work?

reading



How does the Factory work?

writing

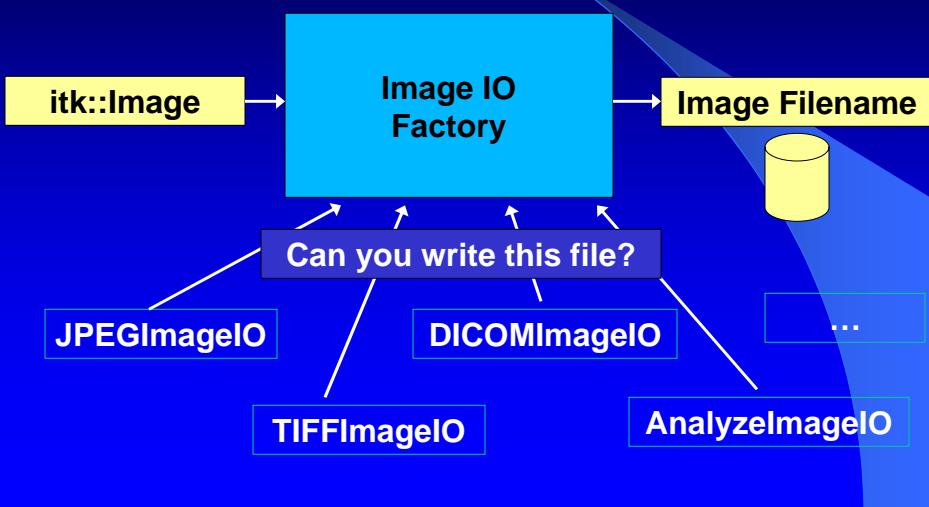


Image File IO

Reading my first image

```
#include <itkImageFileReader.h>

typedef unsigned char PixelType;
typedef itk::Image<PixelType, 2> ImageType;

itk::ImageFileReader<ImageType>::Pointer reader
    = itk::ImageFileReader<ImageType>::New();

reader->SetFileName("lena.jpg");

try
{
    reader->Update();
}
catch (itk::ExceptionObject & e)
{
    std::cerr << e.GetDescription() << std::endl;
    return EXIT_FAILURE;
}

ImageType::Pointer image = reader->GetOutput();
```

Writing my first image

```
#include <itkImageFileWriter.h>

typedef unsigned char PixelType;
typedef itk::Image<PixelType, 2> ImageType;

itk::ImageFileWriter<ImageType>::Pointer writer
    = itk::ImageFileWriter<ImageType>::New();

writer->SetFileName("lena.jpg");
writer->SetInput(image);

try
{
    writer->Update();
}
catch (itk::ExceptionObject & e)
{
    std::cerr << e.GetDescription() << std::endl;
    return EXIT_FAILURE;
}
```

My file format converter

```
itk::ImageFileReader<ImageType>::Pointer reader
= itk::ImageFileReader<ImageType>::New();

itk::ImageFileWriter<ImageType>::Pointer writer
= itk::ImageFileWriter<ImageType>::New();

reader->SetFileName("myImage.jpg")
writer->SetFileName("myImage.tiff");
writer->SetInput(reader->GetOutput());

try
{
    writer->Update();
}
catch (itk::ExceptionObject & e)
{
    std::cerr << e.GetDescription() << std::endl;
    return EXIT_FAILURE;
}
```

How to avoid using the Factory?

- I know the type of images I want to read/write
- Factory can be slow

```
#include <itkTIFFImageIO.h>

itk::TIFFImageIO::Pointer tiffImageIO = itk::TIFFImageIO::New();

reader->Setfilename("myimage.tif");
reader->SetImageIO(tiffImageIO);
reader->Update();
```

Reading RAW images

```
#include <itkRawImageIO.h>

itk::RawImageIO<unsigned short,2>::Pointer io;
io = itk::RawImageIO<unsigned short,2>::New();

io->SetFileName("myimage.raw");
unsigned int dim[2] = {800,60};
double spacing[2] = {0.8, 0.8};
double origin[2] = {0.0,0.0};
for(unsigned int i=0; i<2; i++)
{
    io->SetDimensions(i,dim[i]);
    io->SetSpacing(i,spacing[i]);
    io->SetOrigin(i,origin[i]);
}
io->SetHeaderSize(0);
io->SetByteOrderToLittleEndian();
io->SetPixelType(itk::ImageIOBase::SCALAR);
io->SetNumberOfComponents(1);
```

Reading RAW images (2)

```
itk::ImageFileReader<ImageType>::Pointer reader
    = itk::ImageFileReader<ImageType>::New();

reader->SetFileName("myImage.raw");
reader->SetImageIO(io);

try
{
    reader->Update();
}
catch (itk::ExceptionObject & e)
{
    std::cerr << e.GetDescription() << std::endl;
    return EXIT_FAILURE;
}
```

Creating a MetaImage Header

- Create a simple text file with the .mhd extension
- Set the appropriate MetaData
- Example:

```
NDims = 3
DimSize = 100 200 300
ElementSpacing = 1.2 1.2 1.0
ElementType = MET_UCHAR
ElementByteOrderMSB = False
ElementDataFile = HeadMRVolume.raw
OR
ElementDataFile = HeadMRVolume%04d.raw 0 10 1
```

Dealing with DICOM images

- Often consists of several files
- Uses the GDCM library
- **GDCMSeriesFileNames** to construct the serie:
 1. Image Orientation & Image Position
 2. 'Image Number'
 3. Lexicographical order

Reading DICOM images

```
// Select the correct files from the directory
typedef itk::ImageSeriesReader< ImageType > ReaderType;
ReaderType::Pointer reader = ReaderType::New();

typedef itk::GDCMSeriesFileNames NamesGeneratorType;
NamesGeneratorType::Pointer nameGenerator = NamesGeneratorType::New();
nameGenerator->SetUseSeriesDetails( true );

nameGenerator->SetDirectory( "./MyDirectory/" );
typedef std::vector< std::string > FileNamesContainer;
FileNamesContainer fileNames;
fileNames = nameGenerator->GetFileNames( seriesIdentifier );

reader->SetFileNames( fileNames );

// Set the DicomIO
typedef itk::GDCMImageIO ImageIOType;
ImageIOType::Pointer dicomIO = ImageIOType::New();
reader->SetImageIO( dicomIO );
reader->Update();
```

More on Series Filenames

- NumericSeriesFilenames
 - ordered sequence of filenames
 - unique, non-negative, integral value
 - Set(Start/End)Index and SetIncrementIndex()
- RegularExpressionSeriesFilenames
 - ordered sequence that matches RegEx
 - ordered by submatch or numerically

Metadata

- Extra information attached to an image
- `itk::Image` defines:
 - Spacing (size of the voxels in mm)
 - Origin (physical location of (0,0,0))
 - Size (size of the largest region of the image)
 - Orientation (direction cosines)

MetaData Dictionary

- `itkMetaDataDictionary`
- Filled in by the reader (when available)
- Not passed through the filters
- Accessing the dictionary:

```
ImageType::Pointer image = reader->GetOutput();
typedef itk::MetaDataDictionary DictionaryType;
DictionaryType & dictionary = image->GetMetaDataDictionary();
```

Transform File IO

Transform IO

- Special ITK File format
- Uses IO Factory
- Write Parameters of the transforms as well as Fixed Parameters
- Concatenation of transforms in a single file

Write Transform Example

```
#include "itkTransformFileWriter.h"
#include "itkAffineTransform.h"

typedef itk::AffineTransform<double,3> AffineTransformType;
AffineTransformType::Pointer affine = AffineTransformType::New();
itk::TransformFileWriter::Pointer writer;
writer = itk::TransformFileWriter::New();

writer->AddTransform(affine);
writer->SetFileName( "AffineTransform.txt" );
try
{
    writer->Update();
}
catch( itk::ExceptionObject & excp )
{
    std::cerr << excp << std::endl;
    return EXIT_FAILURE;
}
```

Read Transform Example

```
#include "itkTransformFileReader.h"

itk::TransformFileReader::Pointer reader;
reader = itk::TransformFileReader::New();

reader->SetFileName( "AffineTransform.txt" );
reader->Update();

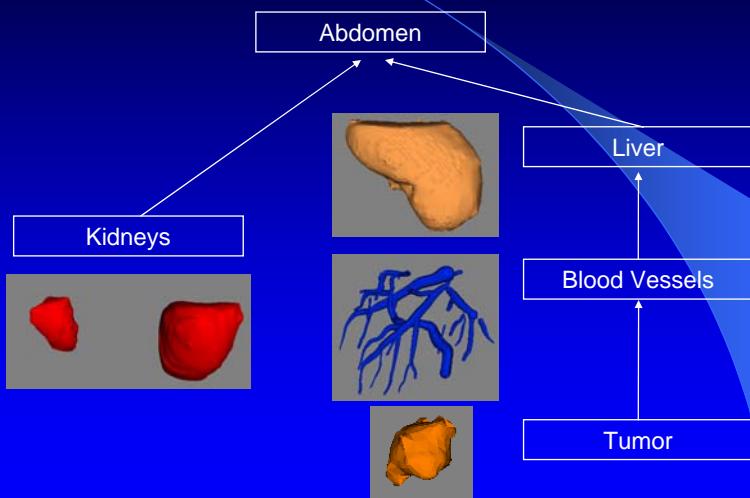
typedef itk::TransformFileReader::TransformListType * TransformListType;
TransformListType transforms = reader->GetTransformList();
itk::TransformFileReader::TransformListType::const_iterator it;
it = transforms->begin();
if(!strcmp((*it)->GetNameOfClass(),"AffineTransform"))
{
  AffineTransformType::Pointer affineTransform =
    static_cast<AffineTransformType*>((*it).GetPointer());
}
```

Object File IO

Spatial Objects

- Represents Physical Objects (not only images)
- Scene Graph Concept
- Common coordinate frame
- Support a common IO framework through MetalIO

Spatial Object Example



Spatial Objects IO

- Uses the IO Factory
- Uses MetaIO file format
- Conversion is done internally
- Concatenation of objects in a single file
- Easy to extend

Writing Spatial Objects

```
#include "itkSpatialObjectWriter.h"
#include "itkEllipseSpatialObject.h"

typedef itk::EllipseSpatialObject<3> SphereType;
SphereType::Pointer sphere = SphereType::New();
sphere->SetRadius(2);

typedef itk::SpatialObjectWriter<3> WriterType;
WriterType::Pointer writer = WriterType::New();
writer->SetInput(sphere);
writer->SetFileName("ellipse.meta");
writer->Update();
```

Reading Spatial Objects

```
#include "itkSpatialObjectReader.h"

typedef itk::SpatialObjectReader<3> ReaderType;
ReaderType::Pointer reader = ReaderType::New();
reader->SetFileName("ellipse.meta");
reader->Update();

// Return an itk::SceneSpatialObject with all the objects in the file
ReaderType::ScenePointer scene = reader->GetScene();

// Return an itk::GroupSpatialObject with all the objects in the file
ReaderType::GroupPointer group = reader->GetGroup();

ReaderType::SceneType::ObjectListType * sceneChildren = scene->GetObjects(999);
ReaderType::SceneType::ObjectListType::const_iterator objectIterator;
objectIterator = sceneChildren->begin();
if(strcmp((*objectIterator)->GetTypeName(),"EllipseSpatialObject"))
{
    SphereType::Pointer sphere = dynamic_cast<SphereType*>((*objectIterator).GetPointer());
}
```

Writing an itkMesh

```
#include "itkSpatialObjectWriter.h"
#include "itkMeshSpatialObject.h"

typedef itk::DefaultDynamicMeshTraits< float , 3, 3 > MeshTrait;
typedef itk::Mesh<float,3,MeshTrait> MeshType;

MeshType::Pointer mesh = MeshType::New();

// Create the mesh Spatial Object
MeshSpatialObjectType::Pointer meshSO = MeshSpatialObjectType::New();
meshSO->SetMesh(mesh);

// Writing the file
typedef itk::SpatialObjectWriter<3, float, MeshTrait> WriterType;
WriterType::Pointer writer = WriterType::New();
writer->SetInput(meshSO);
writer->SetFileName("metamesh.txt");
writer->Update();
```

Logging Capabilities

Logger

- Record output information and send the output to a stream (or multiple streams)
- Priority Level (Fatal, Critical, Warning, Info, Debug...)
- AddLogOutput() : attach an output stream to the logger
- Write() : send information to the logger

Logger in use

```
#include <itkLogger.h>
#include <itkStdStreamLogOutput.h>

itk::Logger::Pointer logger = itk::Logger::New();
itk::StdStreamLogOutput::Pointer output =
    itk::StdStreamLogOutput::New();
output->SetStream(std::cout);

logger->SetName("MyLogger");
logger->SetPriorityLevel(itk::LoggerBase::INFO);
logger->SetLevelForFlushing(itk::LoggerBase::CRITICAL);

logger->AddLogOutput(output);

logger->Write(itk::LoggerBase::INFO, "This is the INFO message.\n");
```

Logger Manager

- Centralize several loggers
- AddLogger()
- CreateLogger() / CreateThreadLogger
- Write()
- Flush()

References

- Culp, Timothy R. "Industrial Strength Pluggable Object Factories". C++ Report Online.
http://www.creport.com/html/from_pages/view_recent_articles_c.cfm?ArticleID=1520
- P. Chandra, L. Ibanez, "ImageIO: Design of an Extensible Image Input/Output Library", ACM Crossroad online magazine, April 2001.
Available online at <http://www.acm.org/crossroads/xrds7-4/imageIO.html>
- E. Gamma, R. Helm, R. Johnson, J. Vlissides, "Design Patterns", Addison Wesley, 1995.

Enjoy ITK !





Overview

- History
- Infrastructure
- Components
- Quality Control
- Software Process
- Applications

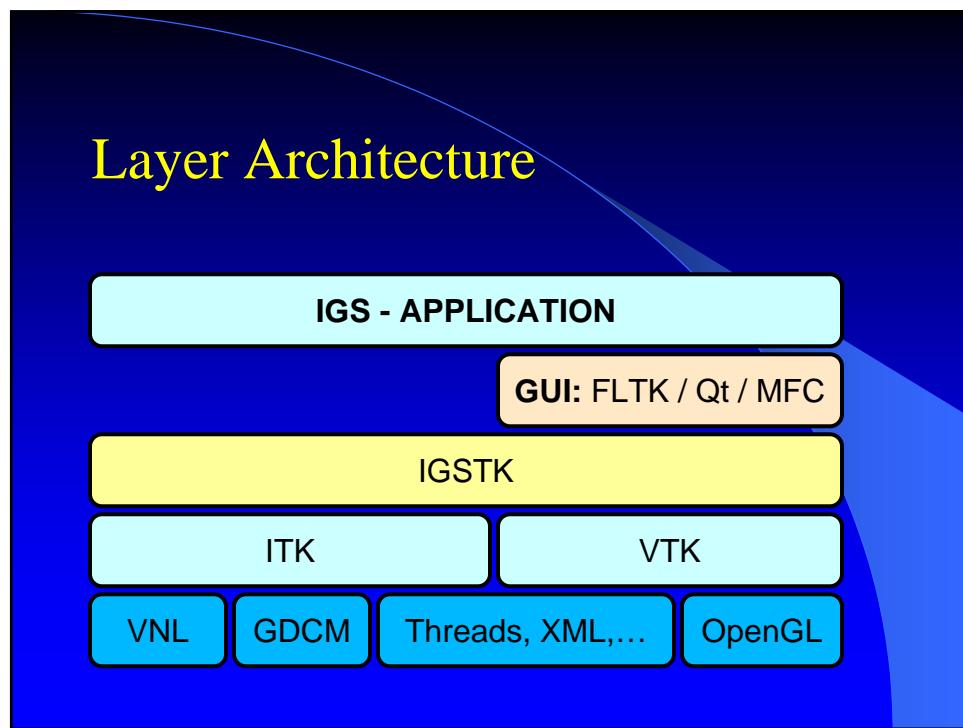
The Toolkit in a Nutshell

- Open Source Toolkit
- BSD-like License
- Written in C++
- Cross Platform
- Based on ITK and VTK
- GUI based on FLTK
- Designed for a Critical Application

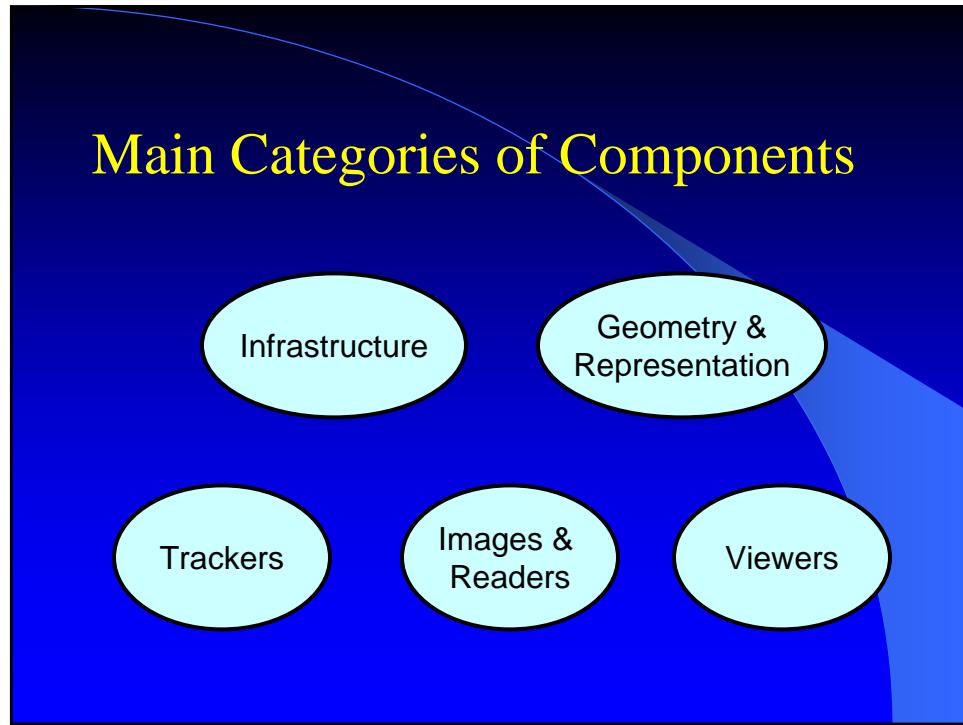
History

- STTR Funded by NIBIB/NIH (Georgetown-Kitware)
- Phase I from May to Sept 2003. Used in example applications.
- Phase II started on October 2004
- CADDLab UNC Joined the project and contributed Spatial Objects & RF ablation Application.
- Atamai joined on 2005 and contributed Tracker code.
- Releases done about every 6 months

Layer Architecture



Main Categories of Components



Infrastructure

- State Machine
- Time Stamp
- Pulse Generator
- Events
- Transforms
- Logger

Trackers

- Tracker (base class)
 - PolarisTracker
 - AuroraTracker
 - Flock Of Birds
- Support
 - SerialCommunication
 - SerialCommunicationForWindows
 - SerialCommunicationForPosix
 - NDICommandInterpreter



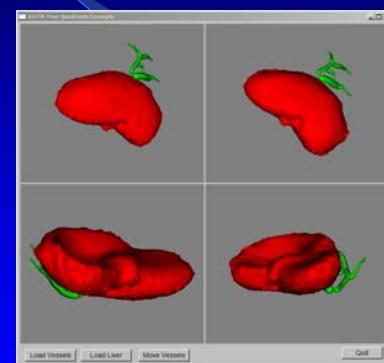
Object Representation

- SpatialObject
 - Ellipsoid
 - Cylinder
 - Images
 - Mesh
 - Tube
 - TubeGroup
 - Group
 - Box
 - Cone
- SpatialObjectRepresentation
 - Ellipsoid
 - Cylinder
 - Images
 - Mesh
 - Tube
 - Box
 - Cone
 - VascularNetwork
 - AirwaysNetwork
 - Surgical Tools



Viewers

- View
 - View2D
 - View3D
- VTK Based
- GUI / VTK hybrid class

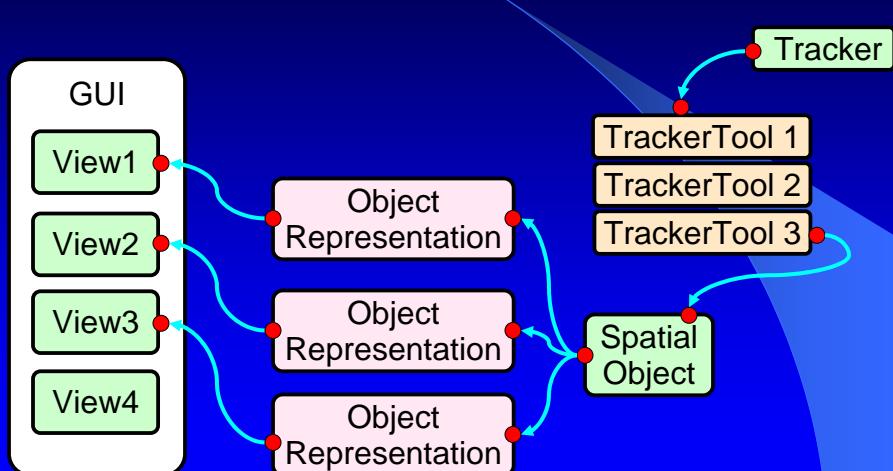


Images and Readers

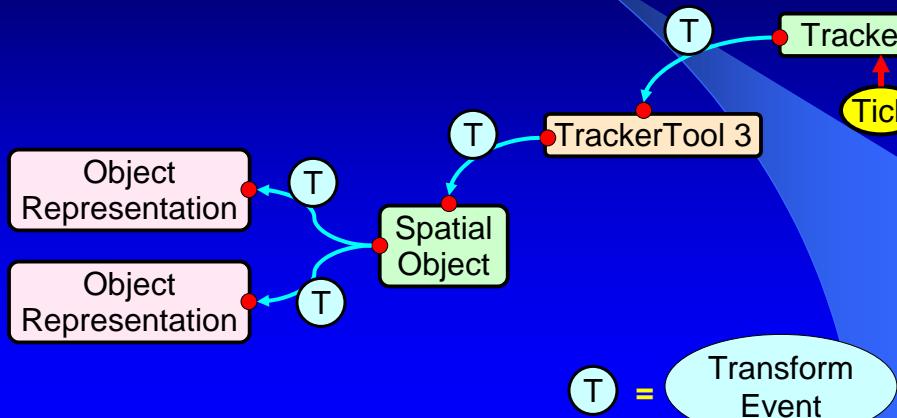
- **Image**
 - CTImage
 - MRIImage
 - FluoroscopicImage
- **Readers (DICOM)**
 - CTImageReader
 - MRIImageReader
 - Fluoroscopy (video input)

Dynamics Architecture

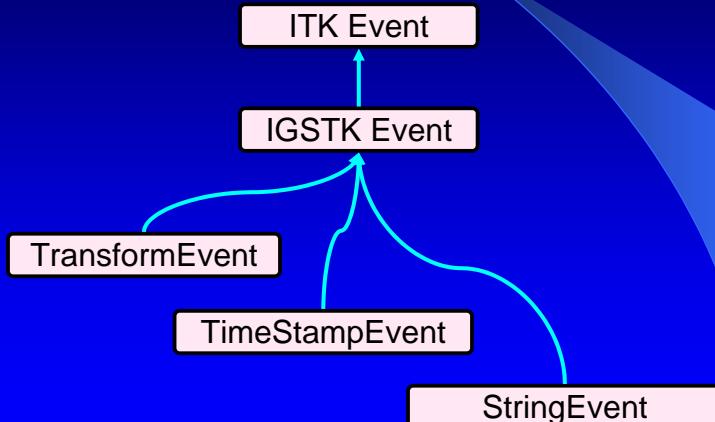
General Interactions



Tracking Interactions



Event Class



Event Class

```
namespace igstk
{
    itkEventMacro( IGSTKEvent, itk::UserEvent );
    itkEventMacro( PositionModifiedEvent, IGSTKEvent );
    itkEventMacro( OrientationModifiedEvent, IGSTKEvent );
    itkEventMacro( GeometryModifiedEvent, IGSTKEvent );
    itkEventMacro( PropertyModifiedEvent, IGSTKEvent );
    itkEventMacro( PulseEvent, IGSTKEvent );
    itkEventMacro( RefreshEvent, IGSTKEvent );
}
```

Transform Class

Transform

Vector

Versor

TimeStamp

Error

Transform Class

```
class Transform
{
public:
    typedef ::itk::Vector<double, 3>    VectorType;
    typedef ::itk::Versor<double>        VersorType;
    typedef double                      ErrorType;
    typedef TimeStamp::TimePeriodType  TimePeriodType;
```

private:

```
TimeStamp      m_TimeStamp;
VectorType     m_Translation;
VersorType    m_Rotation;
ErrorType      m_Error;
```

Transform Event Class

```
class TransformModifiedEvent : public IGSTKEvent
{
public:
    typedef TransformModifiedEvent Self;
    typedef IGSTKEvent Superclass;

    TransformModifiedEvent();
    virtual ~TransformModifiedEvent();
    virtual const char * GetEventName();

    virtual bool CheckEvent(const ::itk::EventObject* e) const;
    virtual ::itk::EventObject* MakeObject() const;

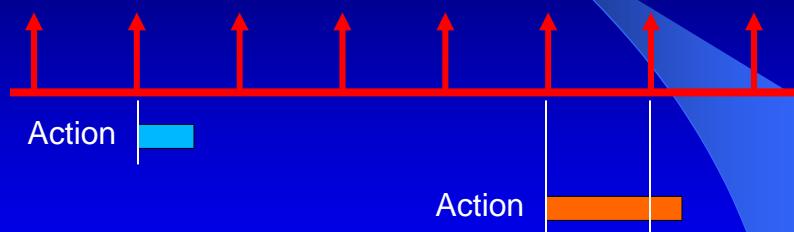
    TransformModifiedEvent(const Self&);

    const Transform & GetTransform() const;
    void SetTransform( const Transform & transform );

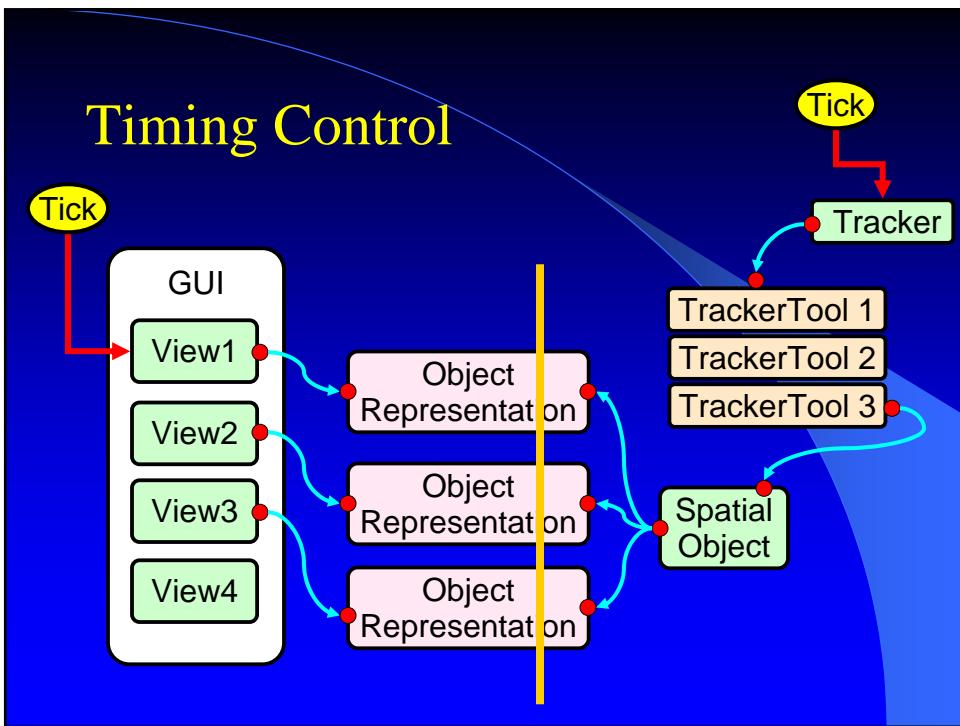
private:
    void operator=(const Self&);

    // Payload of this event.
    Transform m_Transform;
};
```

Pulse Generator



How not to miss pulses ?



Testing Platforms

- Windows
 - Visual Studio 6.0 / 7.1 / 8.0
- Linux
 - gcc 3.2 / 3.3 / 3.4 / 4.0
 - icc 7.1 / 8.0
- Cygwin – Windows
 - gcc 3.4
 - gcc 3.3



Testing

- Goal
 - 100 % Code Coverage
 - 100 % State Machine Transitions Testing
- Current Code Coverage
 - IGSTK 93.6 % (untested 321 / 4714 lines)
 - Sandbox 92.4 % (untested 4 / 49 lines)

Dynamic Testing Platforms

- Valgrind on Linux
 - gcc 3.3
 - gcc 3.4
- Valgrind on Cygwin
- Purify (too expensive)

Software Process

Software Process

- Sandbox
- Extreme programming
- Release early, release often
- Code reviews
- Requirements
- Bug tracking

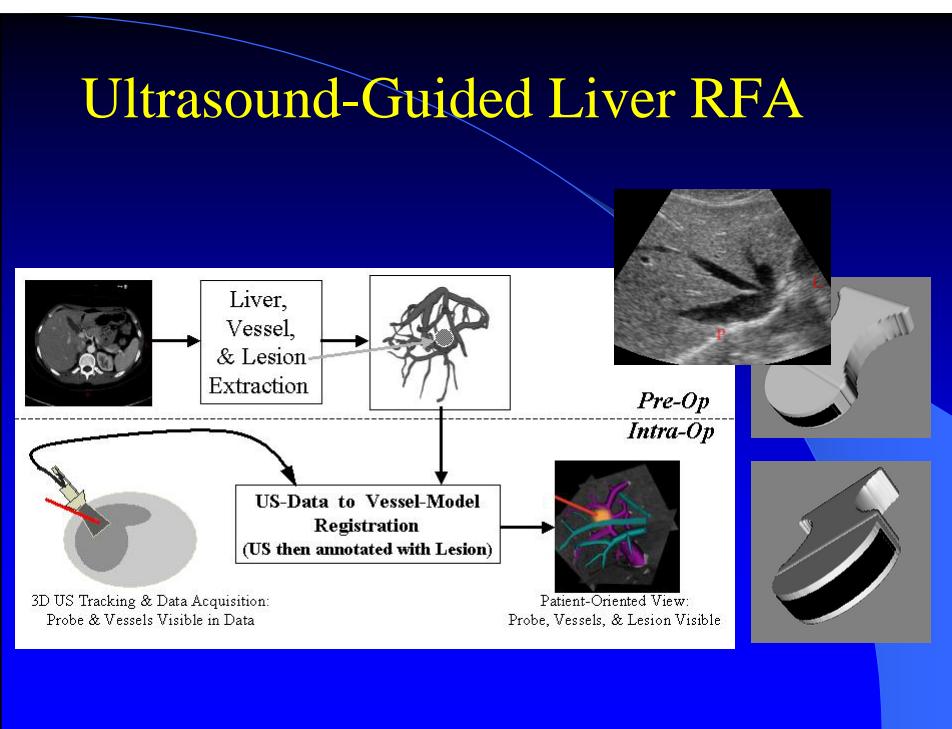
Typical Agenda for a release

- Create feature list
- Write requirements
- Develop code
- Tag Sandbox, create code review list
- Code Review
- Move code and tag
- Fix Documentation
- Fix remaining bugs
- Increase code coverage
- Create and release package

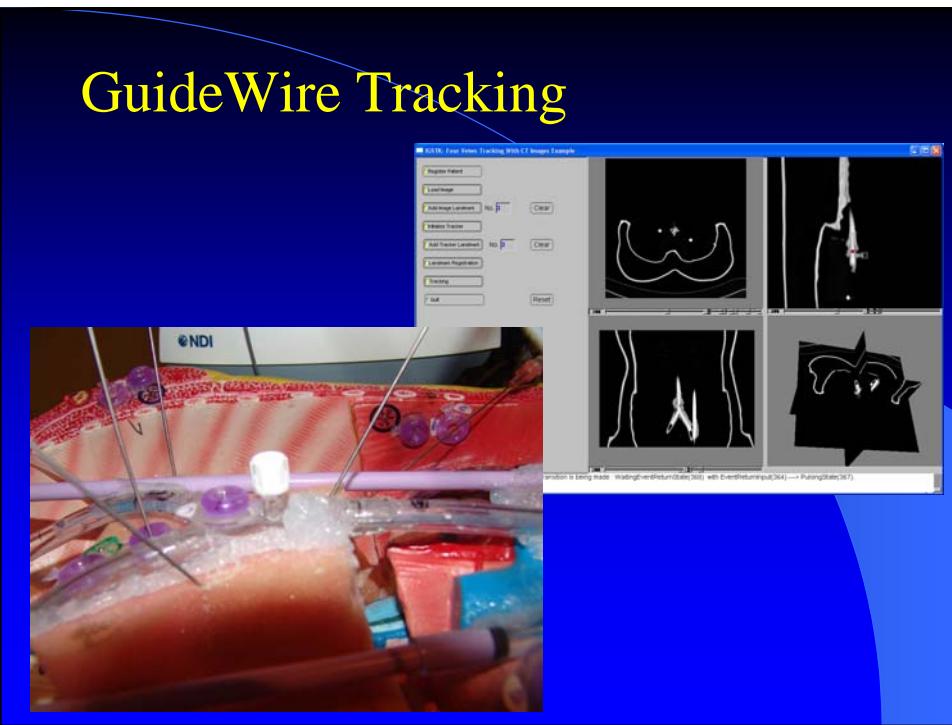
Applications

- Ultrasound-guided percutaneous liver lesion RFA
- Needle Biopsy
- Guidewire Tracking

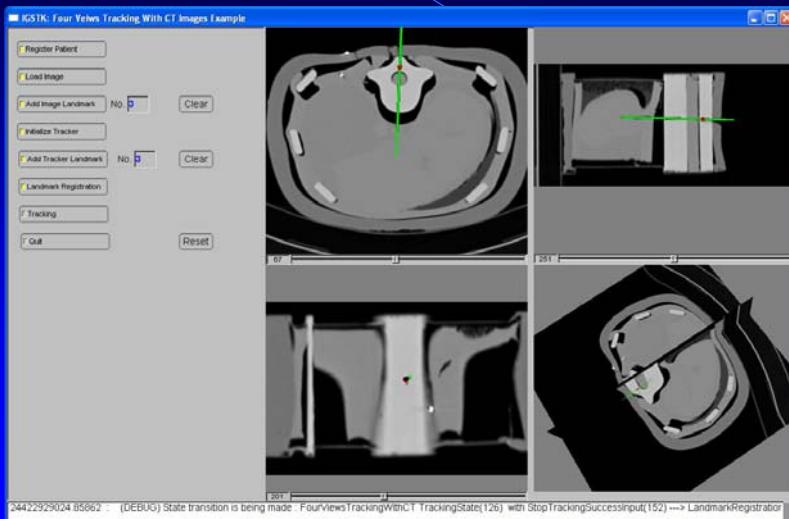
Ultrasound-Guided Liver RFA



GuideWire Tracking



Needle Biopsy



Download IGSTK and Try it!

- <http://www.igstk.org>
- Last stable release "Iteration 7"
- Demo: Sunday Feb 12 from 8:30 to 10:30 pm

Enjoy IGSTK!



Applications: Using Insight(itk) and The Visualization Toolkit(vtk)

Bill Lorensen

Jim Miller

GE Research

Niskayuna, NY



Agenda

- Approaches to interfacing vtk and itk
- Case Studies / Demos
 - Registration
 - MR/MR
 - CT/MR
 - Segmentation
 - Watershed



Motivation

- itk has no visualization capabilities
- itk has some interesting segmentation and registration algorithms
- Both itk and vtk have a pipeline architecture
- vtk has a nice wrapping facility to interpreters like tcl and python

Avoid code duplication and use “best of breed” from each toolkit.



vtk/itk Interfaces

- Connect vtk pipelines to itk pipelines
- Image filter class hierarchies
- Implement vtk filters with itk algorithms
- Callbacks for filter progress



Connect pipelines - vtk to itk

```
vtkImageExport *movingExporter = vtkImageExport::New();
movingExporter->SetInput(movingReader->GetOutput());

typedef itk::VTKImageImport<InputType> ImageImportType;
ImageImportType::Pointer movingImporter =
ImageImportType::New();

ConnectPipelines(movingExporter, movingImporter);

InsightApplications/vtkITK/Common/vtkITKUtility.h
```



Connect Pipelines

- Implements itk pipeline protocol, invoking vtk callbacks

PropagateRequestedRegion()
UpdateOutputInformation()
GenerateOutputInformation()
GenerateData()



vtkITK Class Hierarchies

Class Hierarchy

- **vtkImageToImageFilter**
 - **vtkITKImageToImageFilter**
 - **vtkITKImageToImageFilterFF**
 - **vtkITKImageToImageFilterUSUS**
 - ...
 - **vtkITKDiscreteGaussianImageFilter**



vtkITKImageToImageFilter

- Changes exception macros to errors/warnings
- Delegates
 - Modified
 - DebugOn/Off
 - SetInput/Output
 - Update



vtkITKImageToImageFilterFF

- Defines Input/Output typedefs

```
typedef float InputImagePixelType;  
typedef float OutputImagePixelType;  
typedef itk::Image<InputImagePixelType, 3>  
    InputImageType;  
typedef itk::Image<OutputImagePixelType, 3>  
    OutputImageType;
```

- Constructor

- Creates importers/exporters
- Connects vtk and itk pipelines



vtkITKDiscreteGaussianImageFilter

- Instantiates filter
- Delegates filter's member data set's/get's



vtk Filters Implemented with itk algorithms

- vtkITKMutualInformationTransform
- Implement InternalUpdate()
 - vtkImageExport
 - itk::VTKImageImport
 - ConnectPipelines()
 - Convert vtk transform to quaternion
 - itk::RegistrationMethod
 - Convert itk quaternion to vtk transform

Illustrative Examples

Registration



Motivation for Registration

- Intra-modality
 - Alzheimer's
 - Longitudinal analysis
 - CT Lung
 - Side-by-side slice reading
- Inter-modality
 - PET/MR/CT/US/XRAY Tomo
 - Fusion and analysis



Mutual Information Registration

- Computes “mutual information” between two datasets, a reference and target
 - $MI(X, Y) = H(X) + H(Y) - H(X, Y)$
- Small parameter set
- Developed by Sandy Wells (BWH) and Paul Viola (MIT) in 1995
- Defacto standard for automatic, intensity based registration



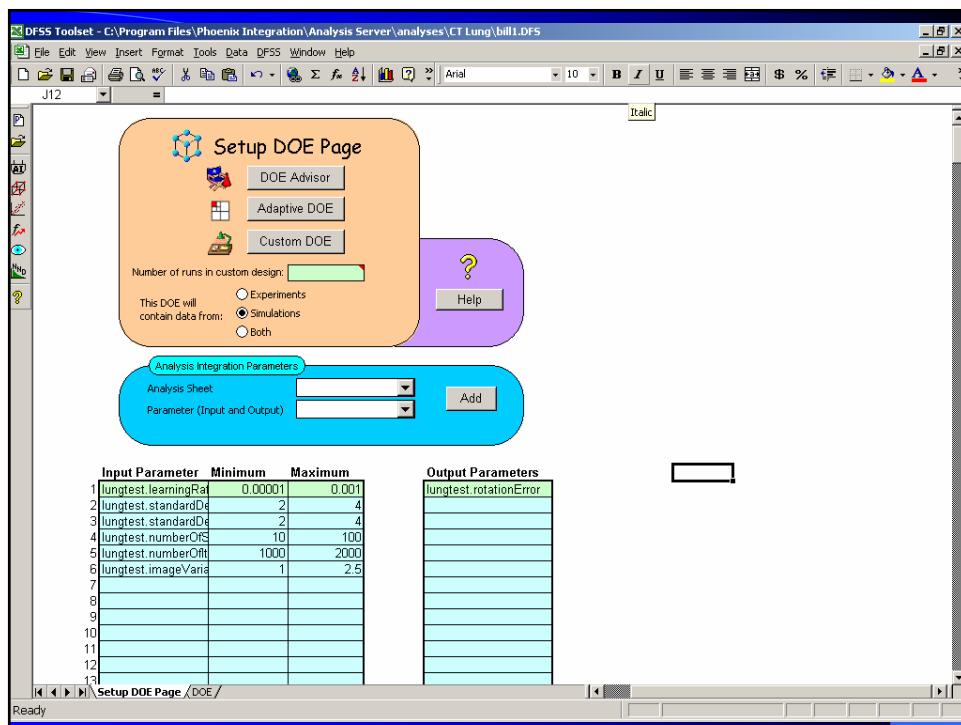
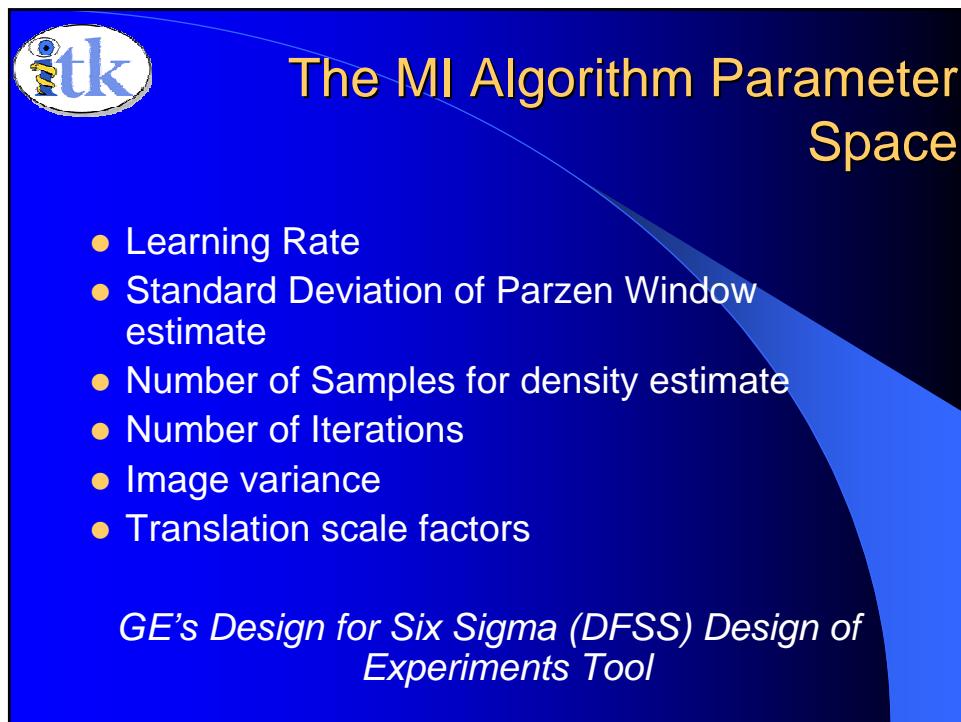
Longitudinal MRI Study

- Register multiple volumetric MRI datasets of a patient taken over an extended time
- Create a batch processing facility to process dozens of datasets
- Resample the datasets



Approach

- Validate the algorithm
- Pick a set of parameters that can be used across all the studies
- For each pair of datasets
 - Perform registration
 - Output a transform
- View the resampled source dataset in context with the target dataset



DFSS Toolset - C:\Program Files\Phoenix Integration\Analysis Server\analyses\CT Lung\b111.DFS

File Edit View Insert Format Tools Data DFSS Window Help

1 Read Data Regression Backward Evaluation Plots Clear Best Transform ? Help

2 Orders Quadratic Response lungtest.rv Transforms None Significant 0.05

3 Coded Actual Goto R2 Goto Predicted Goto Validation Export to Opt Tool

4 5 6

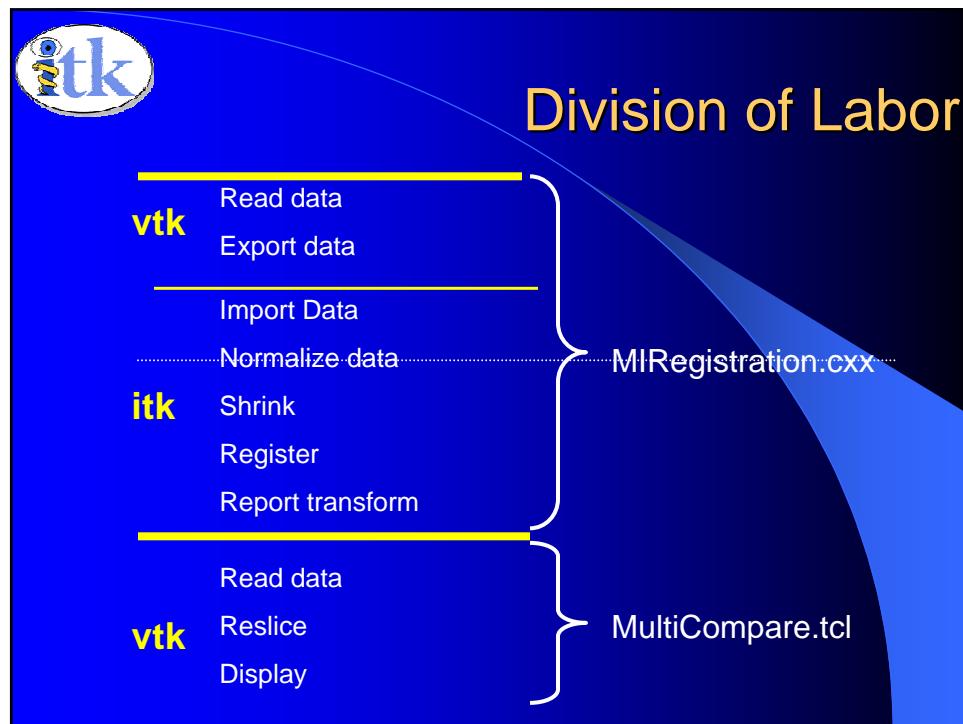
7 Terms All None Results for lungtest.rotationError Predicted Results Goto Min-Max Back to Top

8 9 10 11 12 13 14 15 16 17 18 19 20 21 22 23 24 25 26 27 28 29 30 31 32 33 34 35

Variable	Coded Coefficient	p	Interpret	Point	Actual	Pred	Resid	%Error	Rstudent
Constant	2.08405444	4.7169E-05		1	8.75822	8.351181	0.407039	-4.65	0.349
lungtest.learningRate	-3.2748267	5.9898E-24	Significant	2	0.605525	2.381663	-1.77614	293.32	-1.559
lungtest.standardDeviationA	0.54788684	0.00295773	Significant	3	8.8143	8.76707	0.04723	-0.54	0.040
lungtest.standardDeviationB	0.606748	0.00111358	Significant	4	5.15029	4.631317	0.616973	-12.02	0.532
lungtest.numberOfSamples	-0.1768956	0.31743499	Insignificant	5	8.81585	8.754023	0.061827	-0.70	0.053
lungtest.learningRate*1	-0.5206672	0.00456452	Significant	6	4.51613	4.665934	-0.1498	3.32	-0.128
lungtest.imageVariance	-0.748968	8.7561E-05	Significant	7	8.82838	10.34234	-1.51396	17.15	-1.320
lungtest.numberOfIterations	0.43344128	0.01848305	Significant	8	8.25379	7.988013	0.265777	-3.22	0.228
lungtest.standardDeviationA*1	0.47035733	0.01095646	Significant	9	8.75245	8.221167	0.531283	-6.07	0.456
lungtest.standardDeviationB*1	-0.1845106	0.30462296	Insignificant	10	0.0711992	1.513606	-1.44241	2025.87	-1.256
lungtest.standardDeviationA*2	-0.4224044	0.02160534	Significant	11	8.81323	8.987522	-0.17429	1.98	-0.149
lungtest.standardDeviationB*2	-0.566951	0.00180611	Significant	12	5.16718	4.013726	1.153454	-22.32	0.999
lungtest.standardDeviationA*3	0.29310639	0.10574307	Insignificant	13	8.81299	8.794908	0.018182	-0.21	0.016
lungtest.standardDeviationB*3	0.09761659	0.6244682	Insignificant	14	5.15505	3.968676	1.186374	-23.01	1.028
lungtest.numberOfSamples*1	-0.067793	0.70471955	Insignificant	15	8.82787	10.73365	-1.90572	21.59	-1.680
lungtest.numberOfSamples*2	-0.4064288	0.02666623	Significant	16	8.10871	7.641222	0.467488	-5.77	0.401
lungtest.numberOfSamples*3	0.04269982	0.81126455	Insignificant	17	8.6737	8.203039	0.470661	-5.43	0.404
lungtest.numberOfIterations*1	0.0947426	0.59664469	Insignificant	18	2.58369	0.543903	2.039787	-78.95	1.806
lungtest.numberOfIterations*2	0.3060937	0.09154673	Insignificant	19	8.798241	8.347756	0.450484	-5.12	0.367
lungtest.numberOfIterations*3	0.02130207	0.9051516	Insignificant	20	0.590608	2.422385	-1.83158	310.01	-1.611
lungtest.numberOfIterations*4	0.0789961	0.65867601	Insignificant	21	8.79896	8.22691	0.57205	-6.50	0.491
lungtest.numberOfIterations*5	0.11704201	0.51366172	Insignificant	22	0.49587	2.449203	-1.95333	393.92	-1.724
lungtest.numberOfIterations*6	2.30190212	0.01598746	Significant	23	8.82478	9.544052	-0.71927	8.15	-0.619
lungtest.numberOfIterations*7	0.31291242	0.73566996	Insignificant	24	7.32525	5.50011	1.82614	-24.92	1.605
lungtest.numberOfIterations*8	0.43415762	0.63894061	Insignificant	25	8.6565	8.158232	0.498268	-5.76	0.428
lungtest.numberOfIterations*9	-0.10764559	0.24663029	Insignificant	26	0.0345373	-0.23695	0.273483	-791.85	0.235

Results for lungtest.rotationError

Variable	Coded Coefficient	p	Interpret
Constant	2.08405444	4.7169E-05	
lungtest.learningRate	-3.2748267	5.9898E-24	Significant
lungtest.standardDeviationA	0.54788684	0.00295773	Significant
lungtest.standardDeviationB	0.606748	0.00111358	Significant
lungtest.numberOfSamples	-0.1768956	0.31743499	Insignificant
lungtest.numberOfIterations	-0.5206672	0.00456452	Significant
lungtest.imageVariance	-0.748968	8.7561E-05	Significant

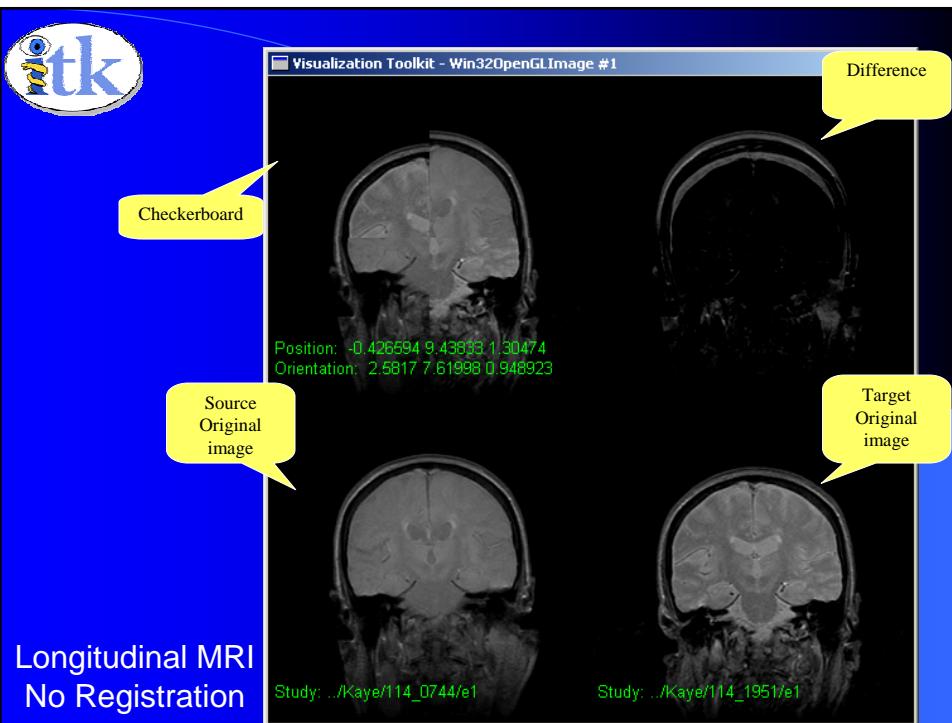


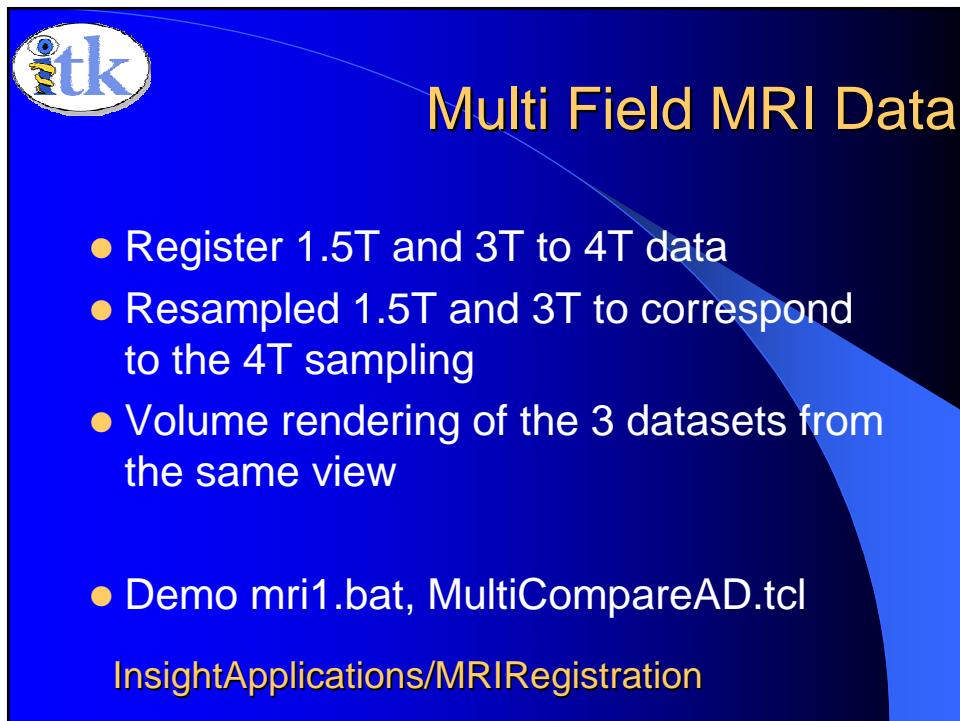
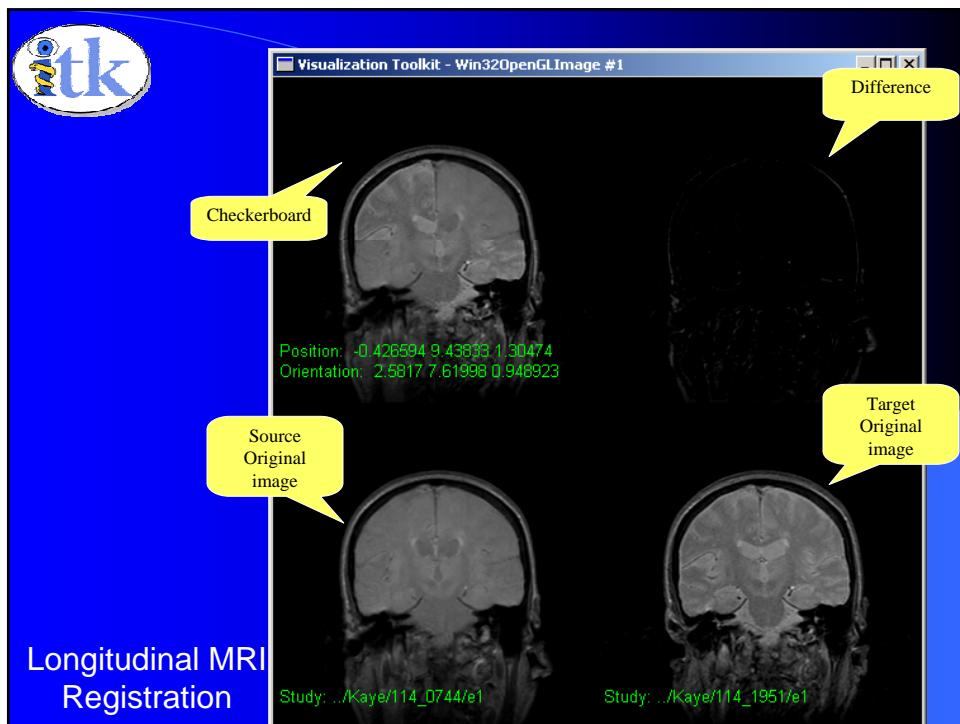


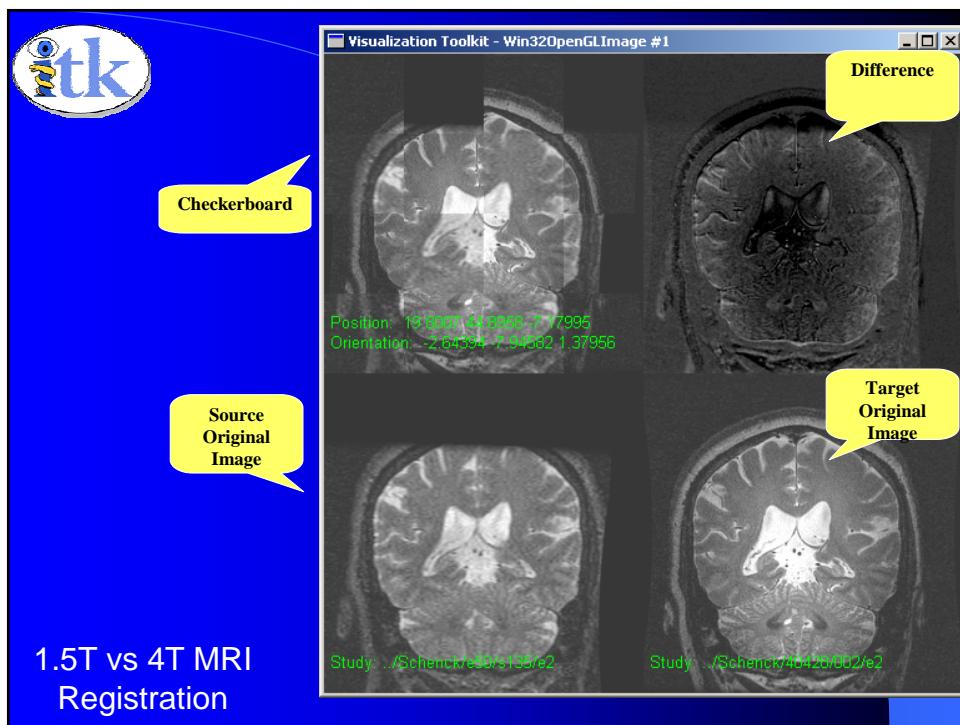
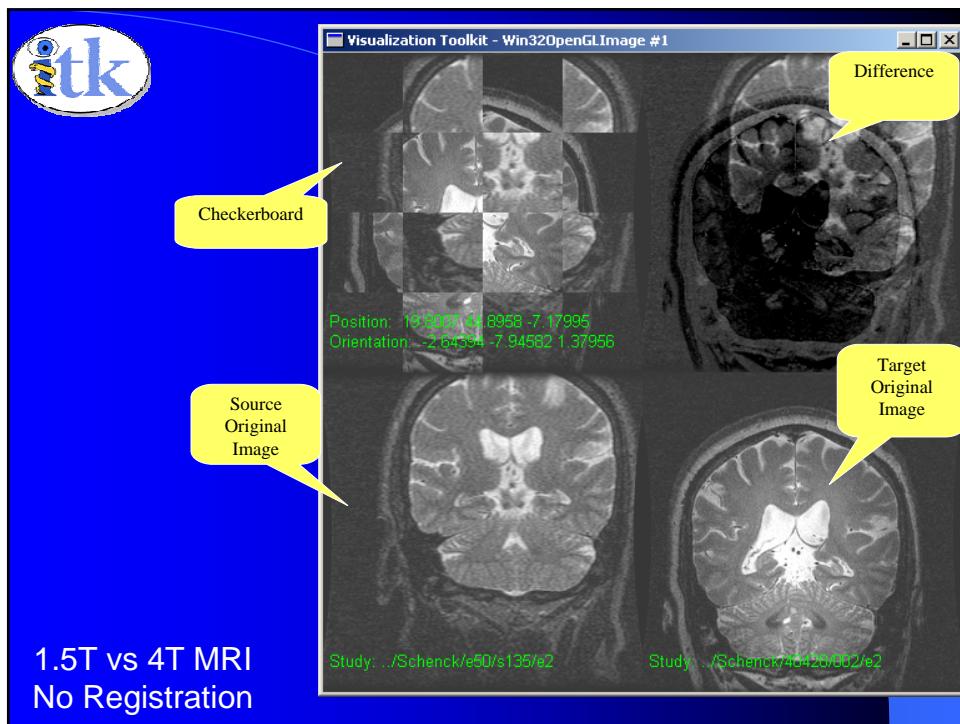
Oregon Data

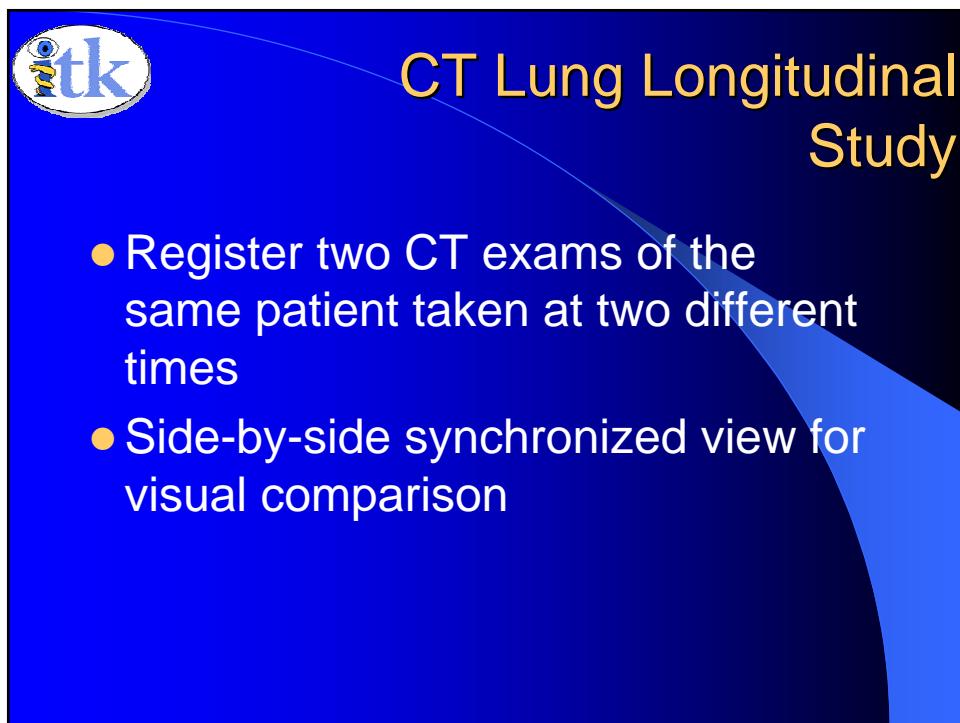
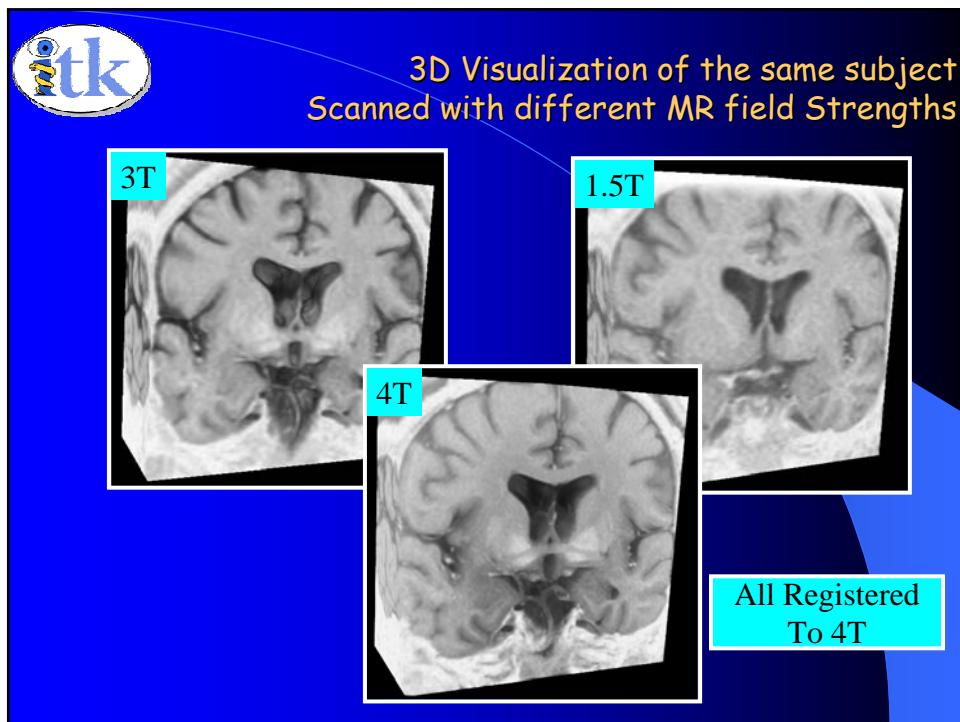
- 25 Registrations
- 13 Subjects, some with AD
- Qualitative comparison
- One set of parameters for all studies

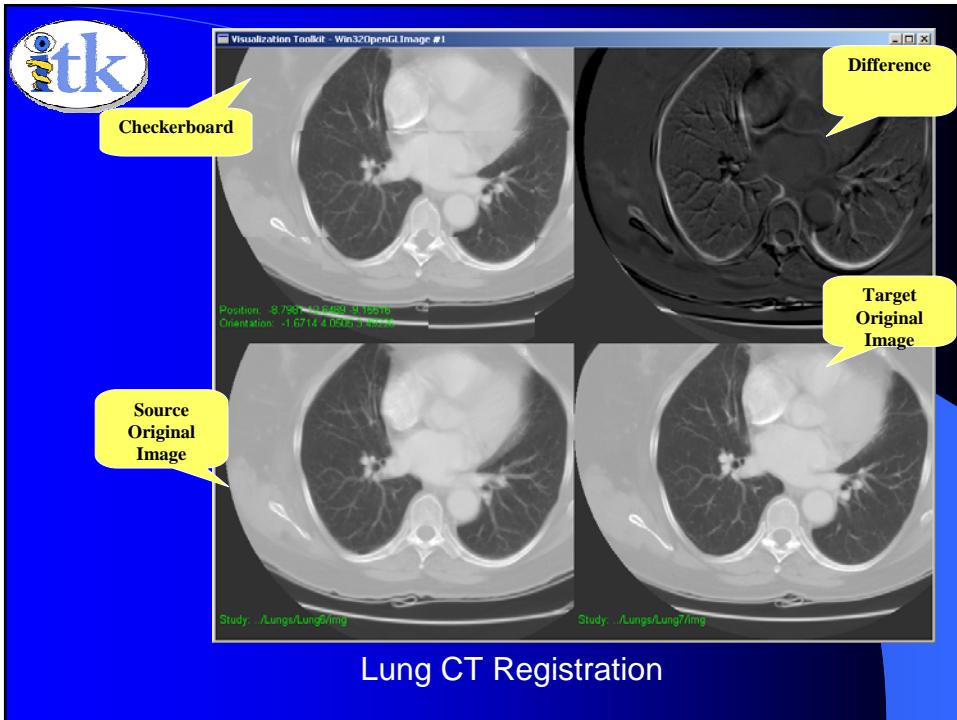
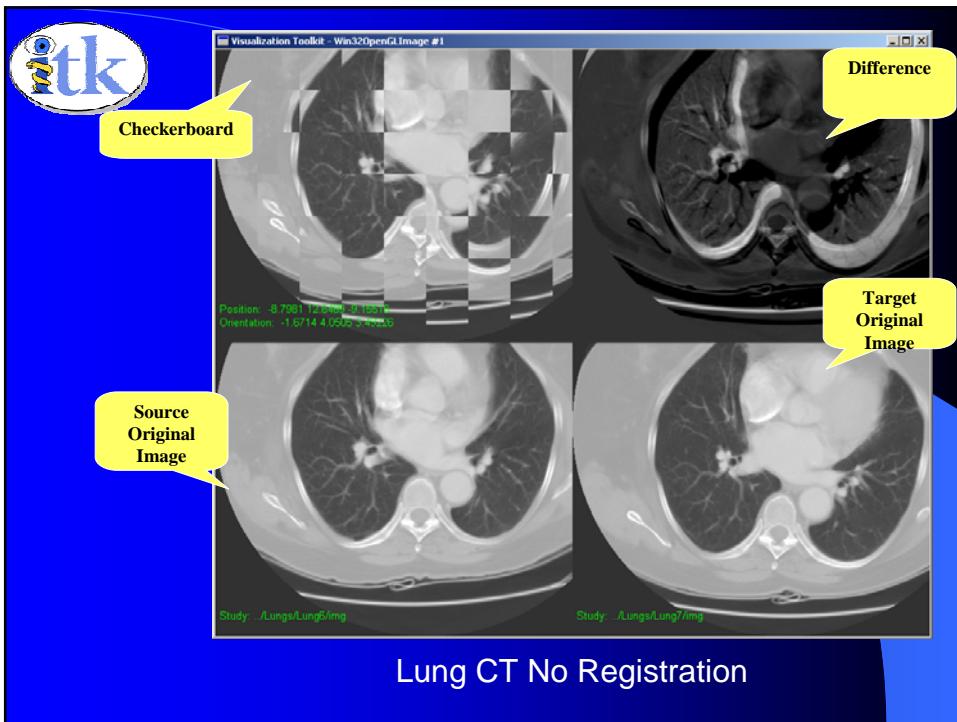
Data Courtesy of Jeffrey Kaye, Oregon Health Sciences Center

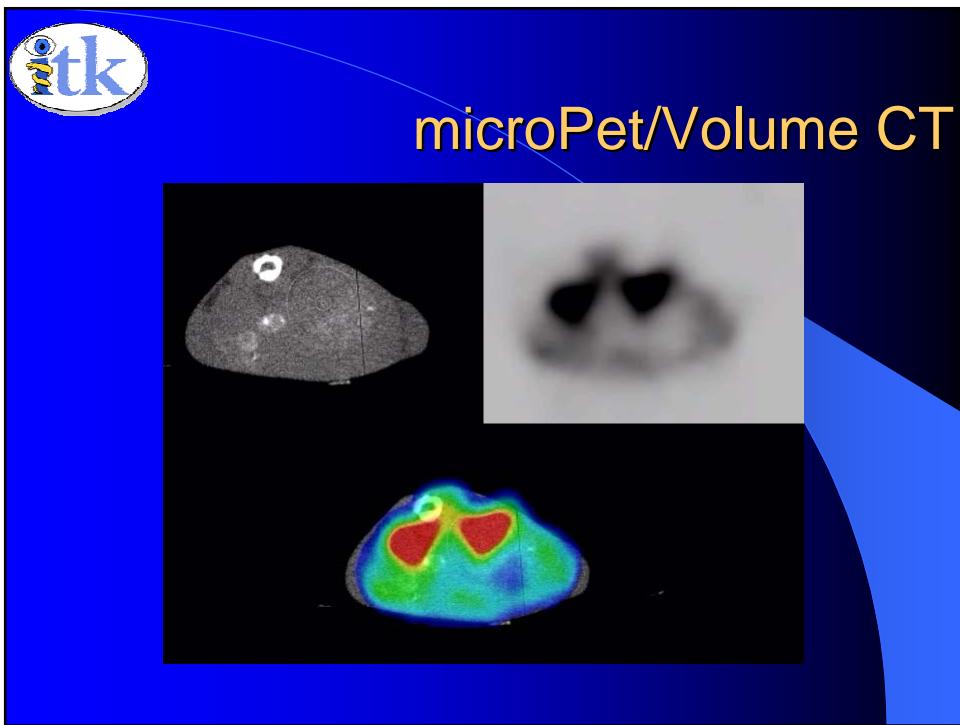
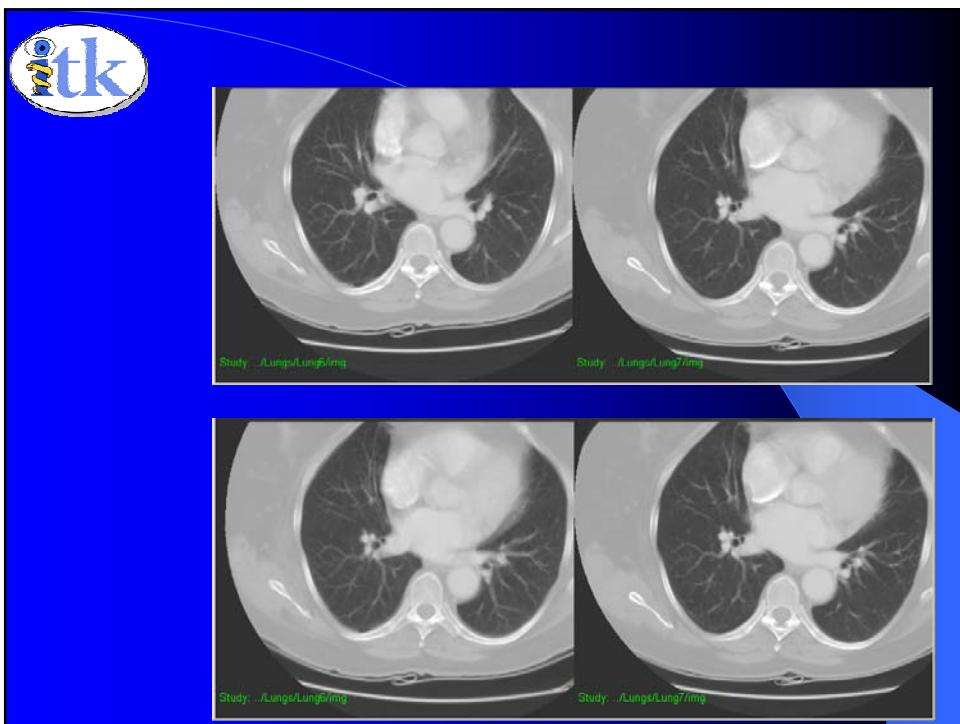


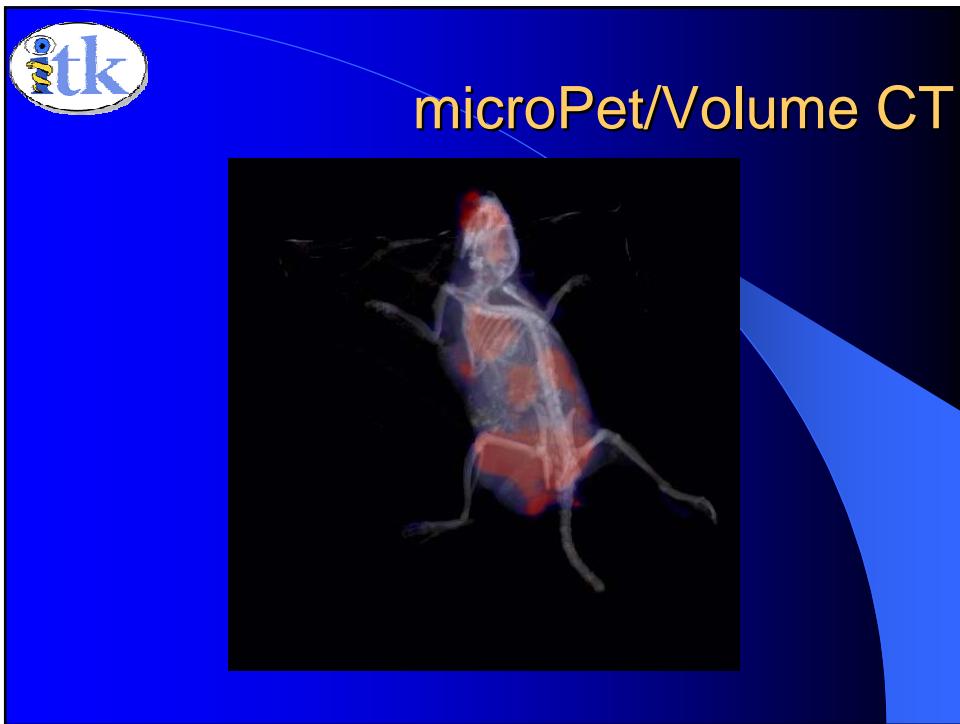














Implementing a vtk Transform with itk

- vtkITKMutualInformationTransform

DemoMutual.tcl

Visible Woman Registration Case Study

Bill Lorensen, GE Research

Peter Ratiu, Brigham and Womens Hospital





Agenda

- Problem Statement
- Methods
- Results
- Discussion



Problem Statement

- Register the Visible Human Female Computed Tomography and MRI Data to the cryo-section data
- Validate the use of the itk Mutual Information Registration algorithm on data of differing modalities
- Assess the performance of the registration using landmarks selected by an anatomical expert



Methods

- `NormalizeImageFilter` (itk)
- `Mutual Information Registration` (itk)
 - Implemented as a vtk Transform
- `Marching Cubes` (vtk)
- `Checkerboard Display` (vtk)



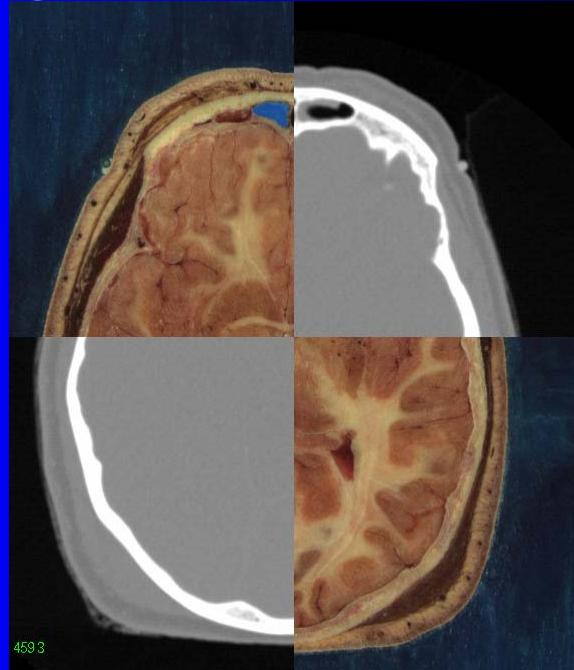
Methods

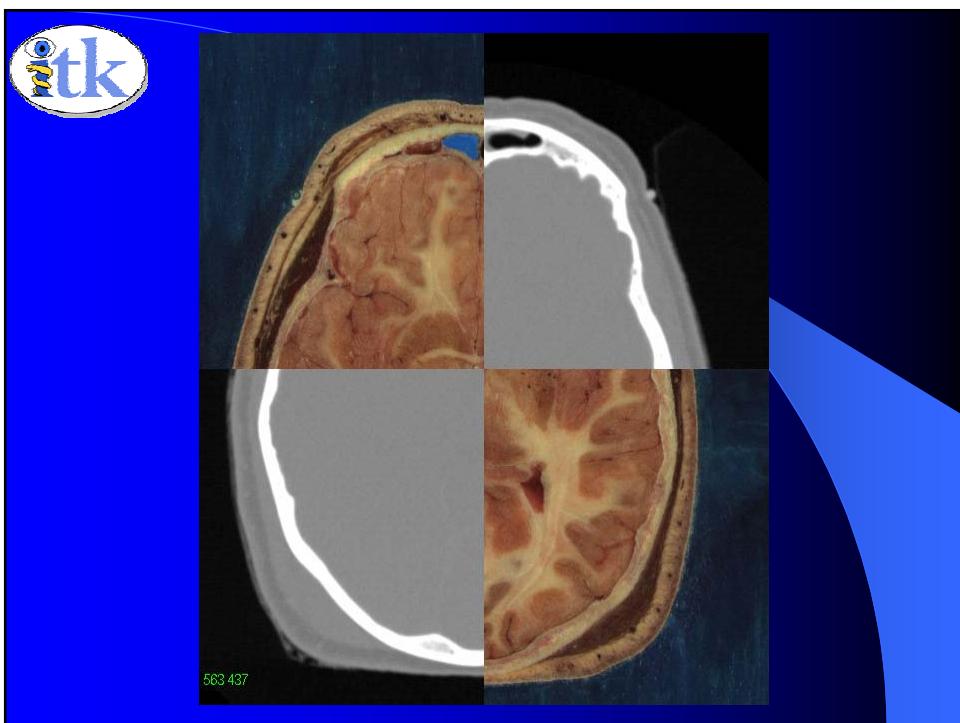
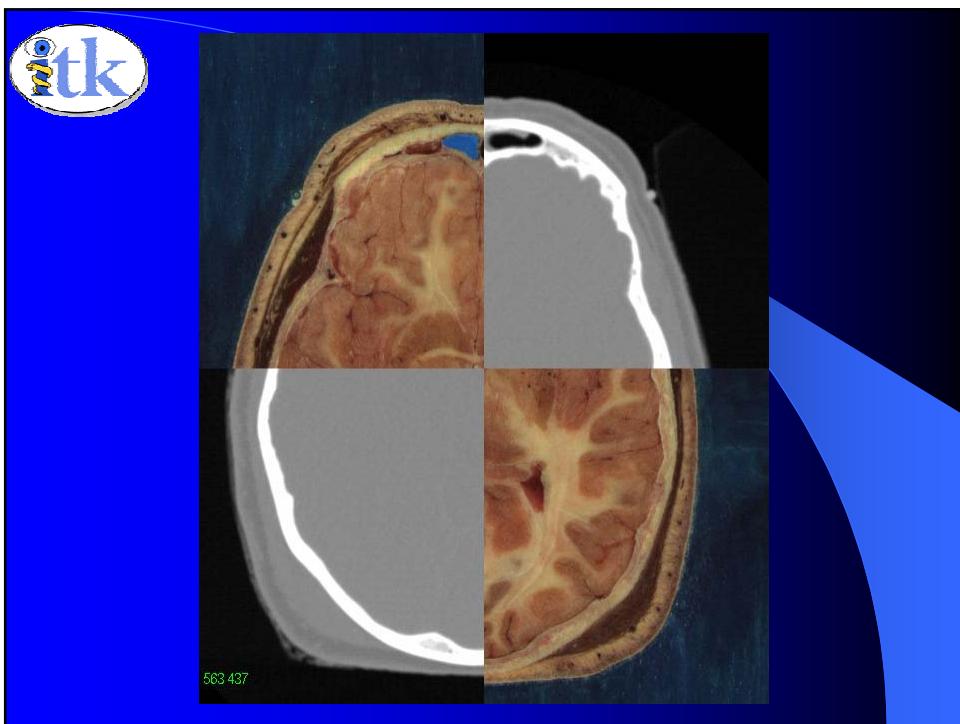
- Multiple registration runs with increasing scales
- Both RGB and CT data scaled to zero mean and unit variance
 - 1/16, 1/8, 1/4, 1/2, 1 scale
 - .01, .01, .004, .004, .001 learning rate
 - 2000 iterations at each resolution

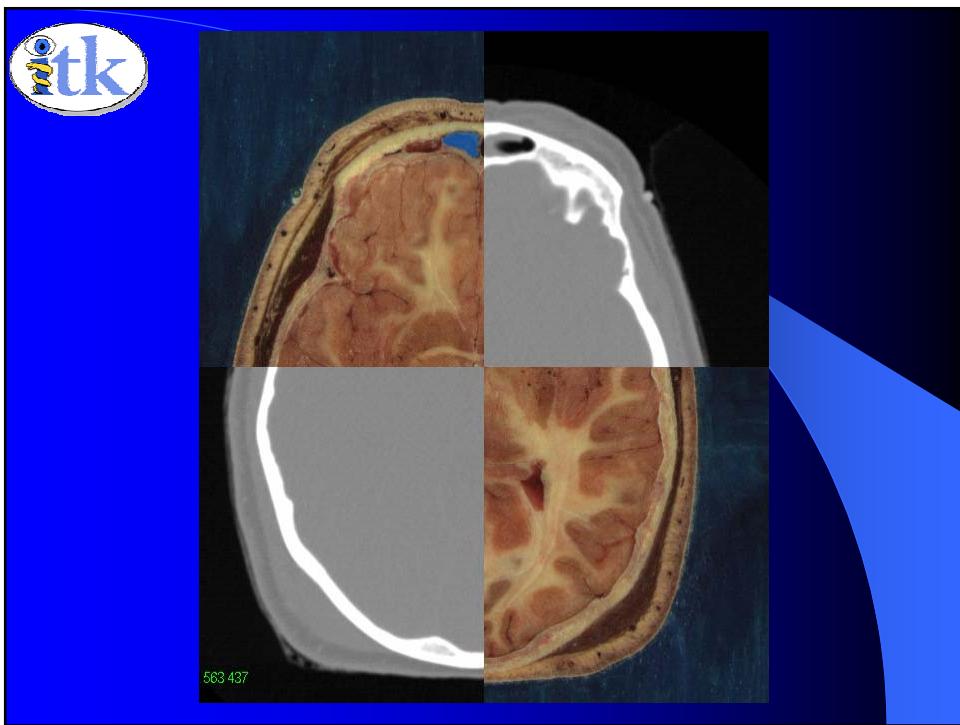
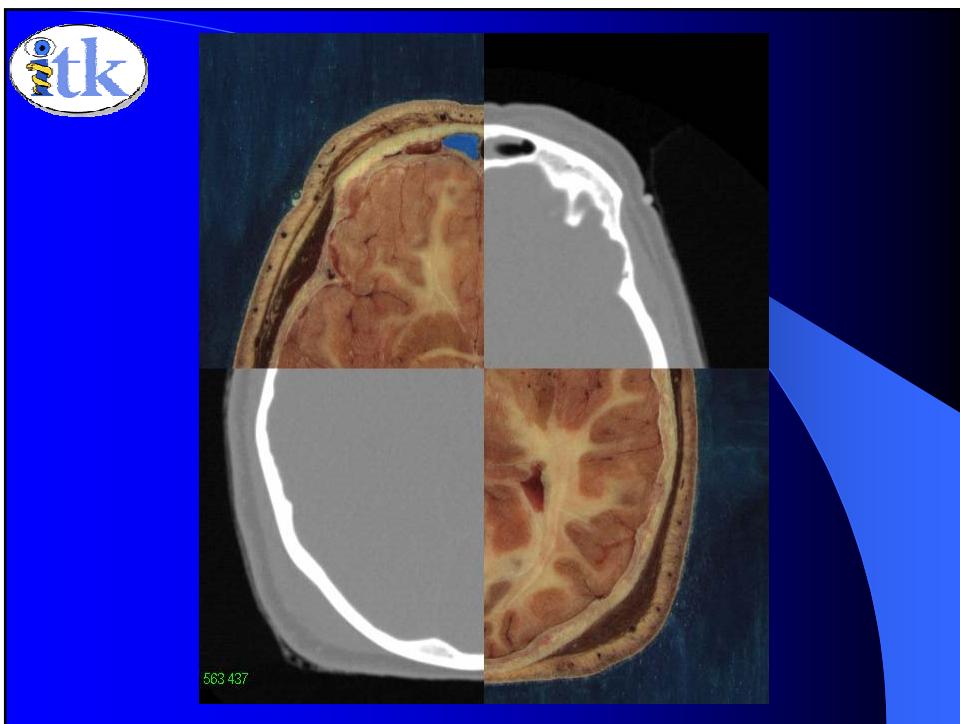


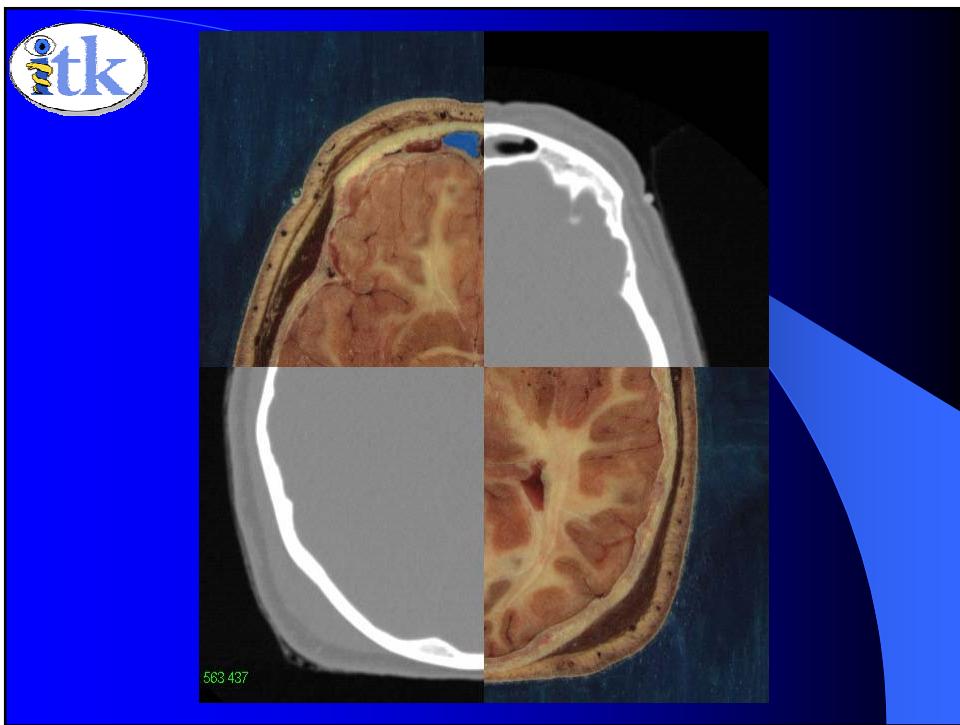
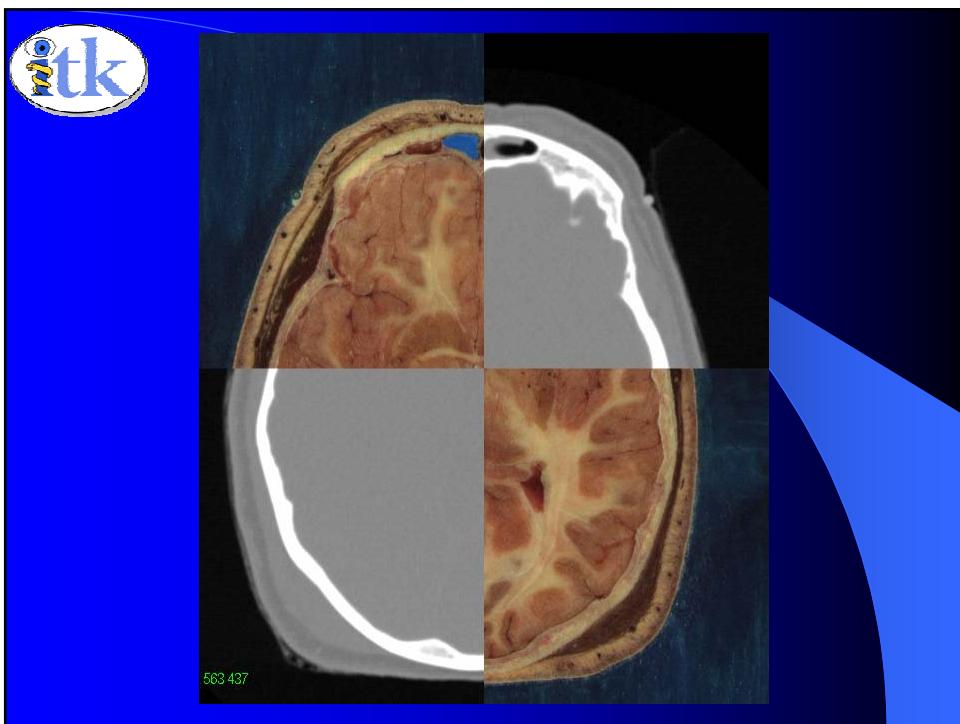
CT Results

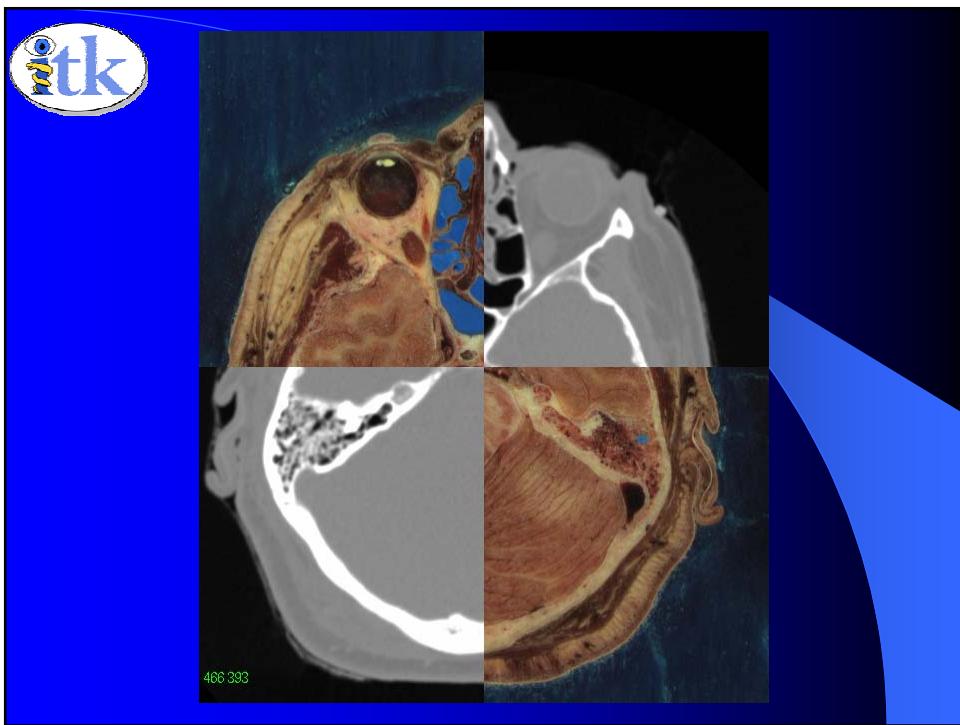
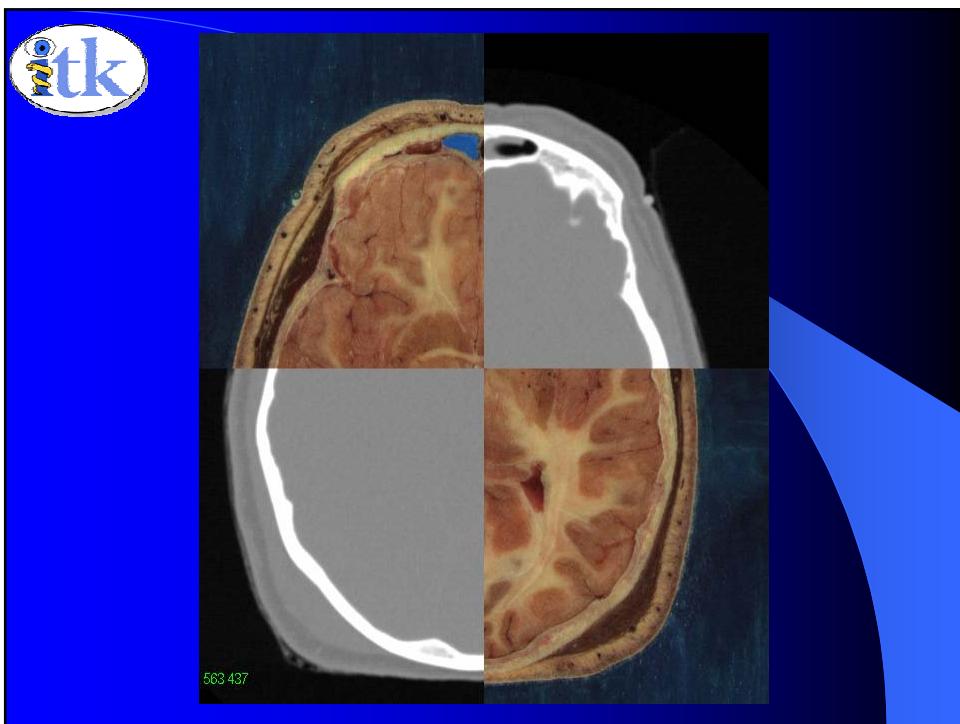
- Initial vertical translation of 20 mm
- Checkerboard display of two modalities after each resolution run







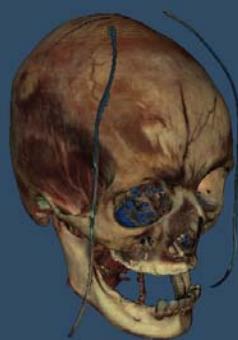


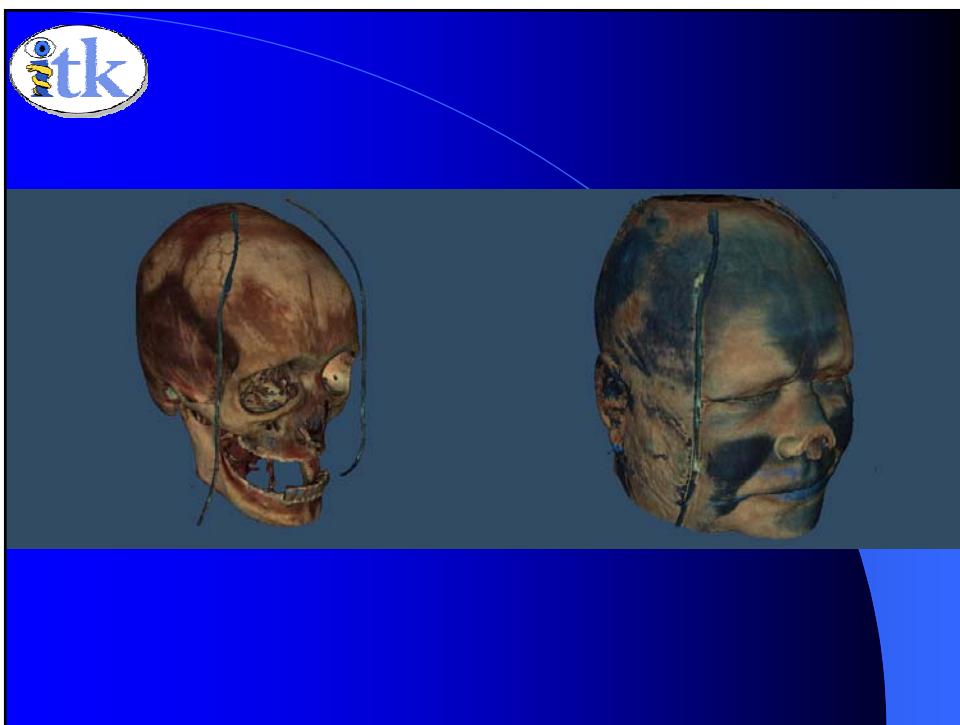


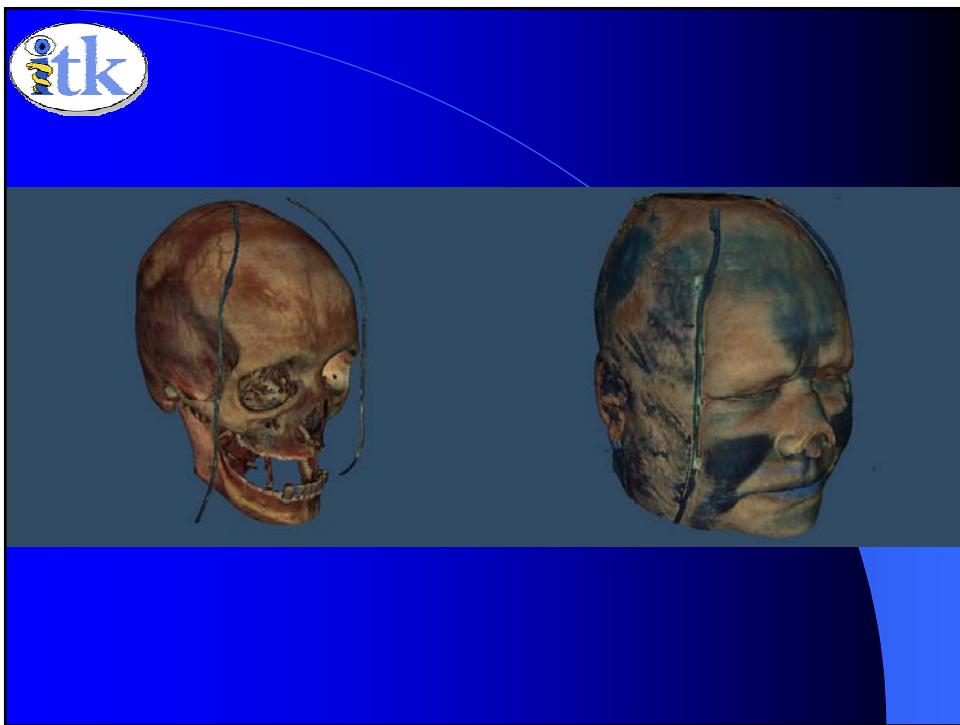
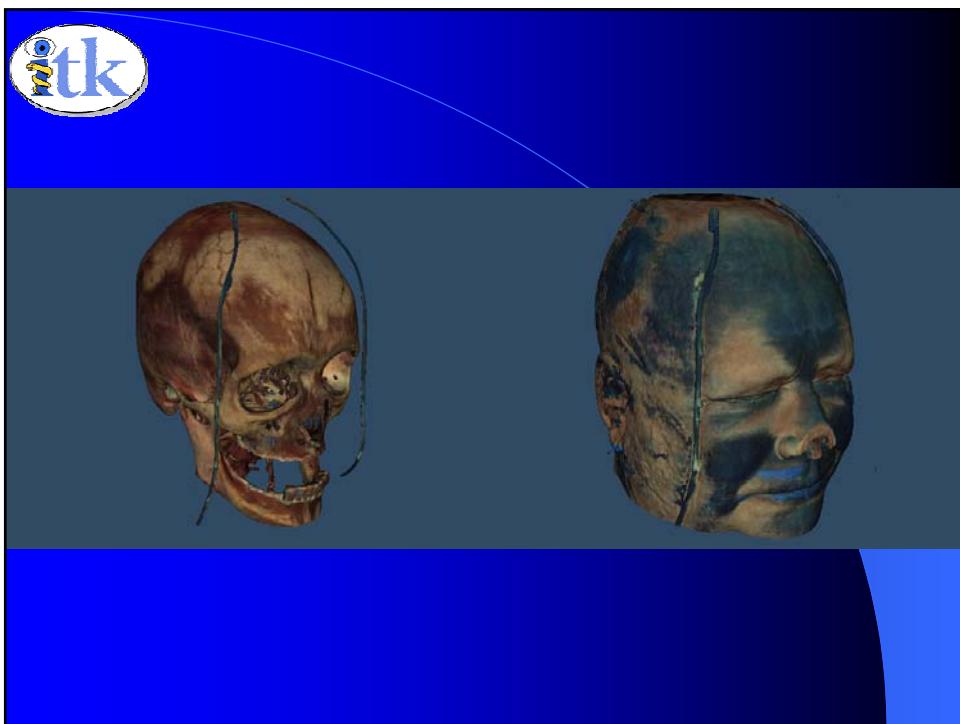


CT Results

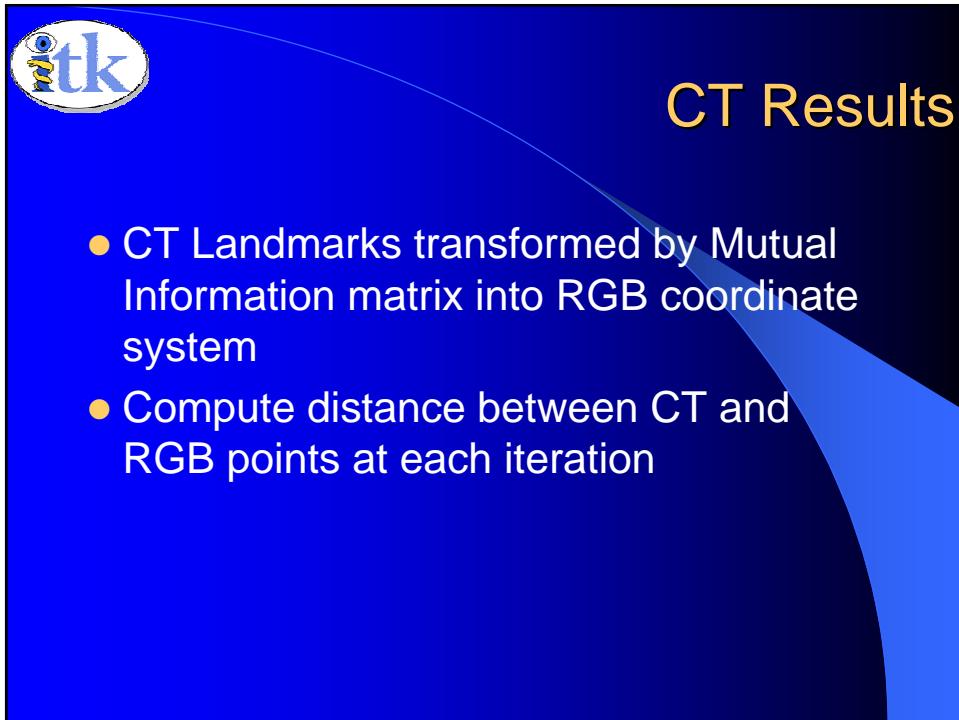
- Generated isosurfaces of skin and bone from CT data
- Transformed according to computed transformation
- At each triangle vertex, sample the RGB data to color the vertex

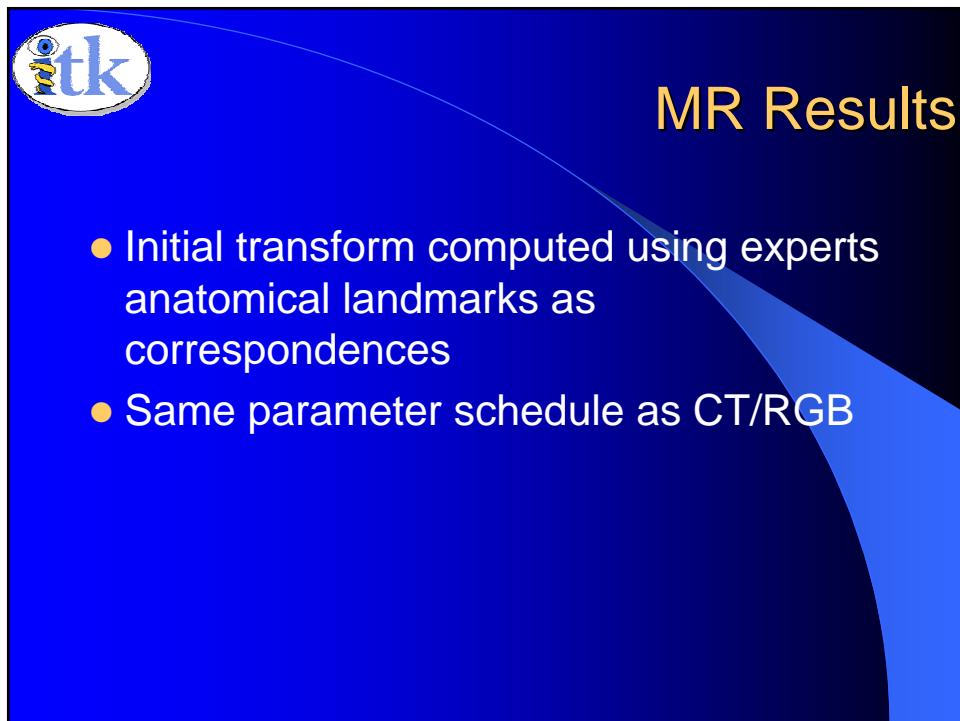
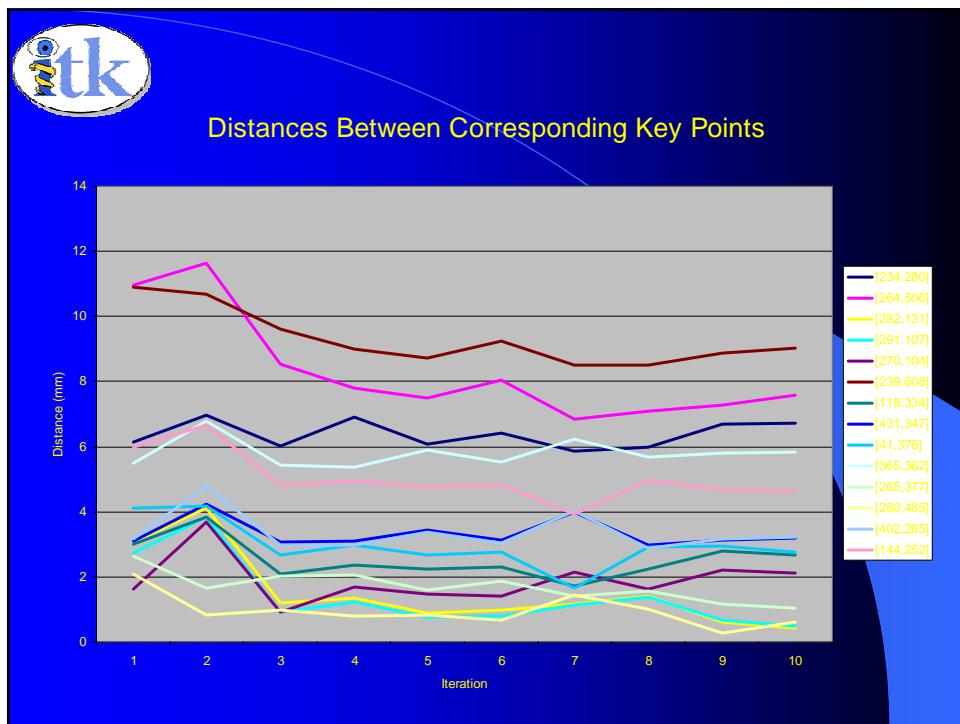


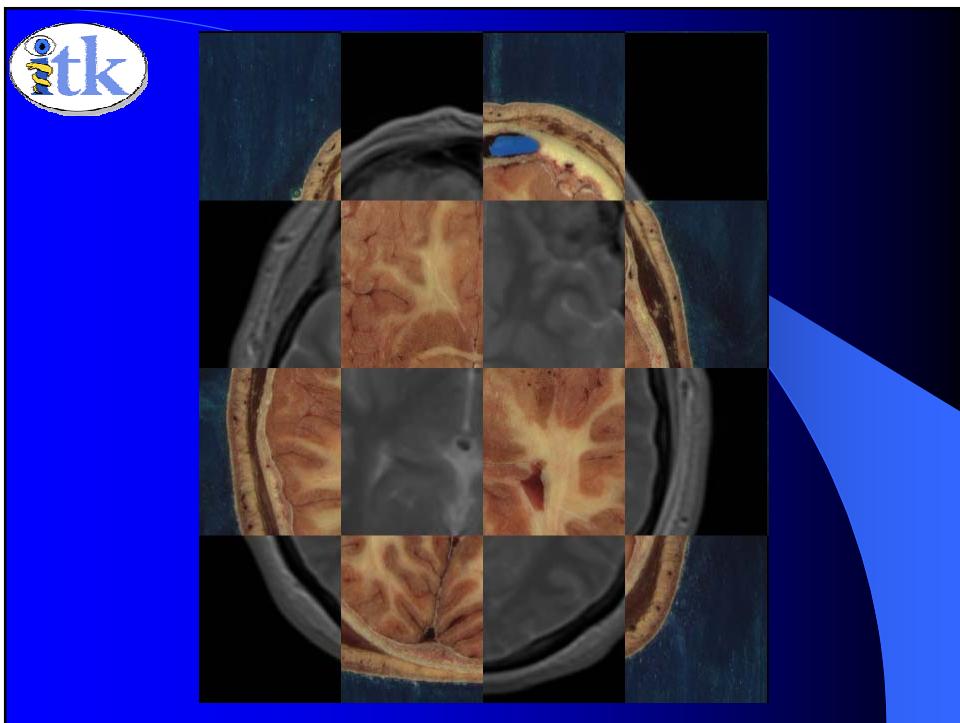
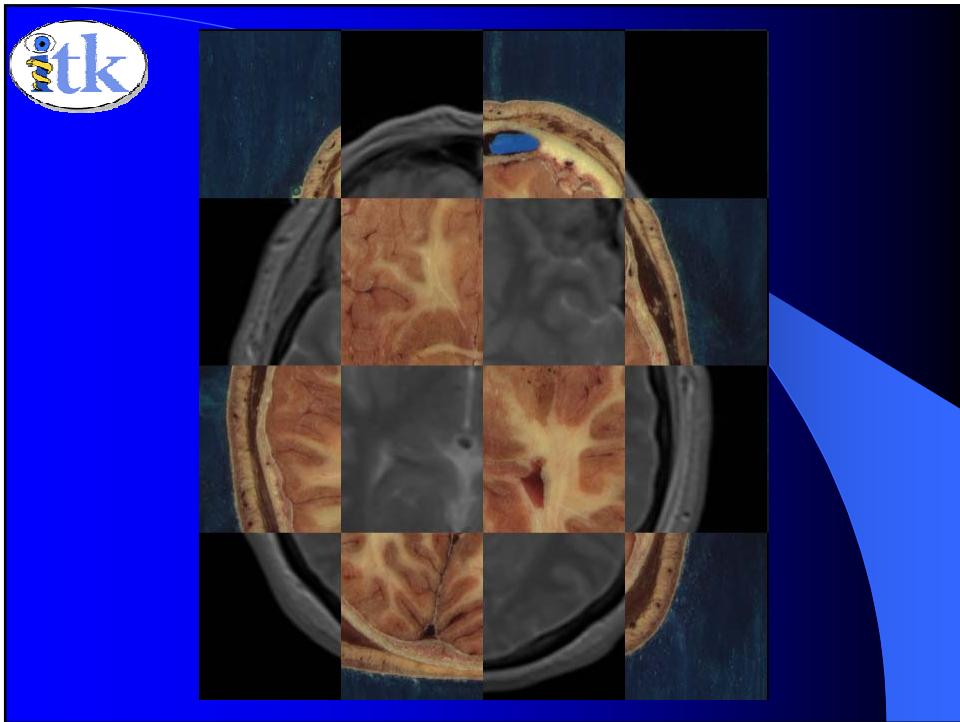


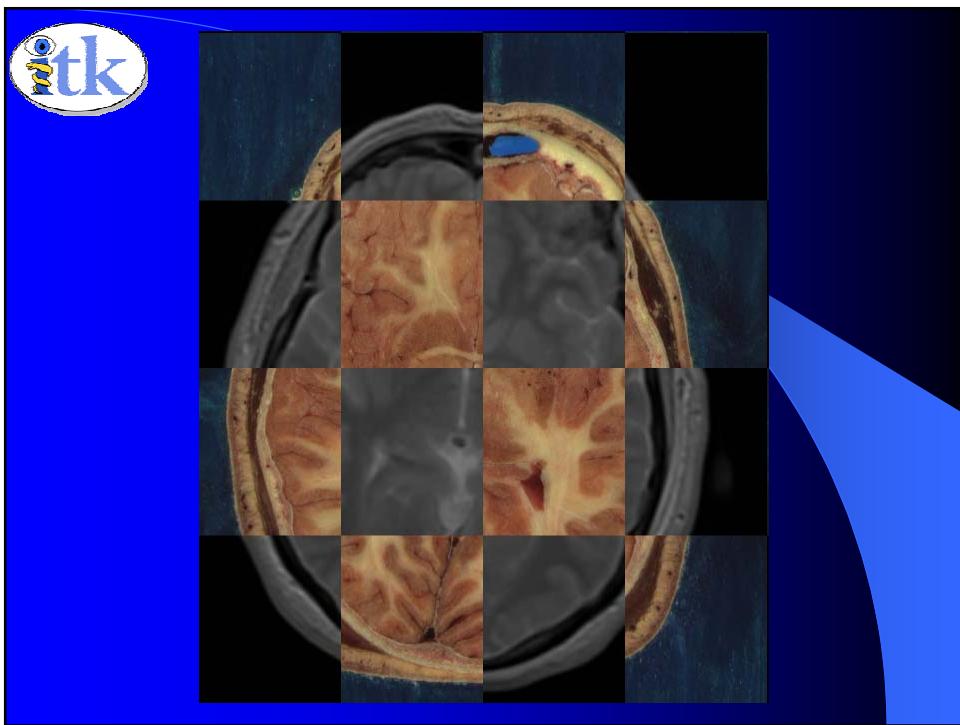
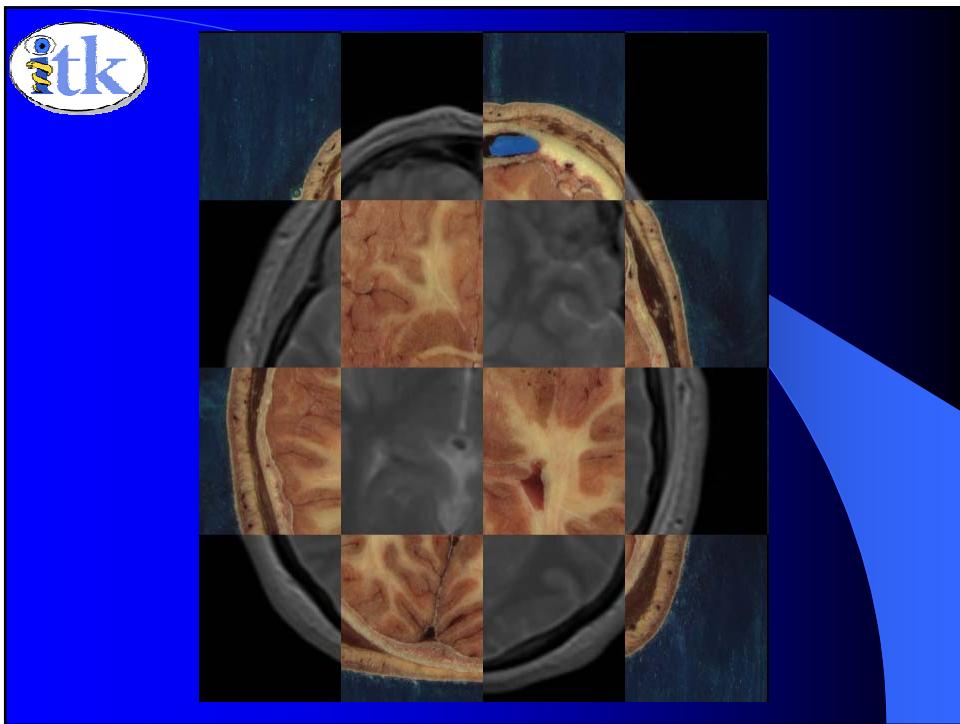


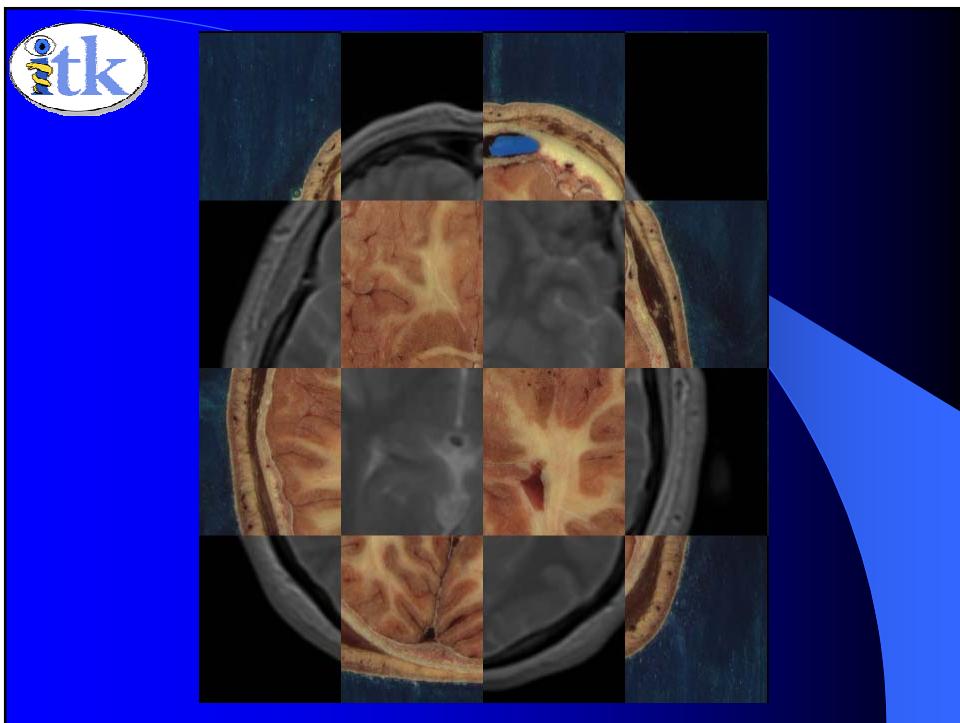
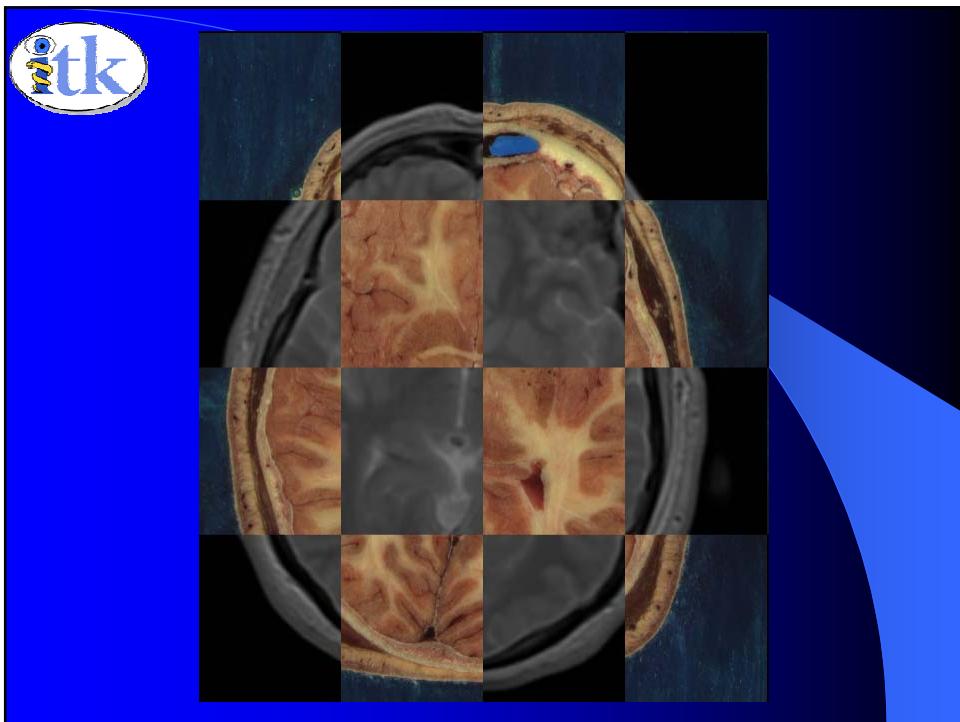


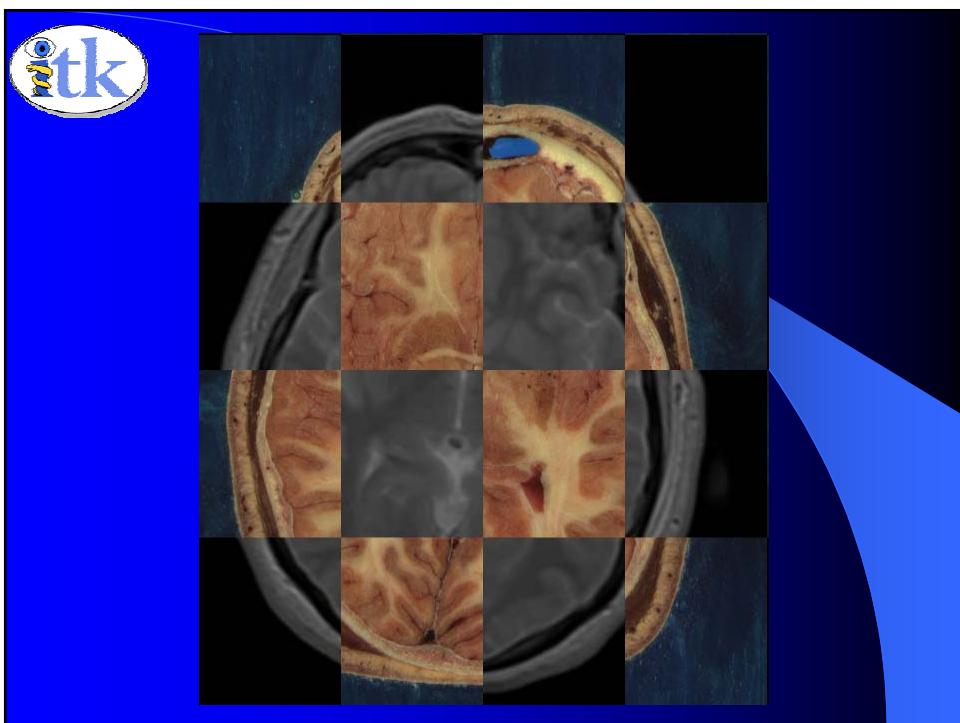
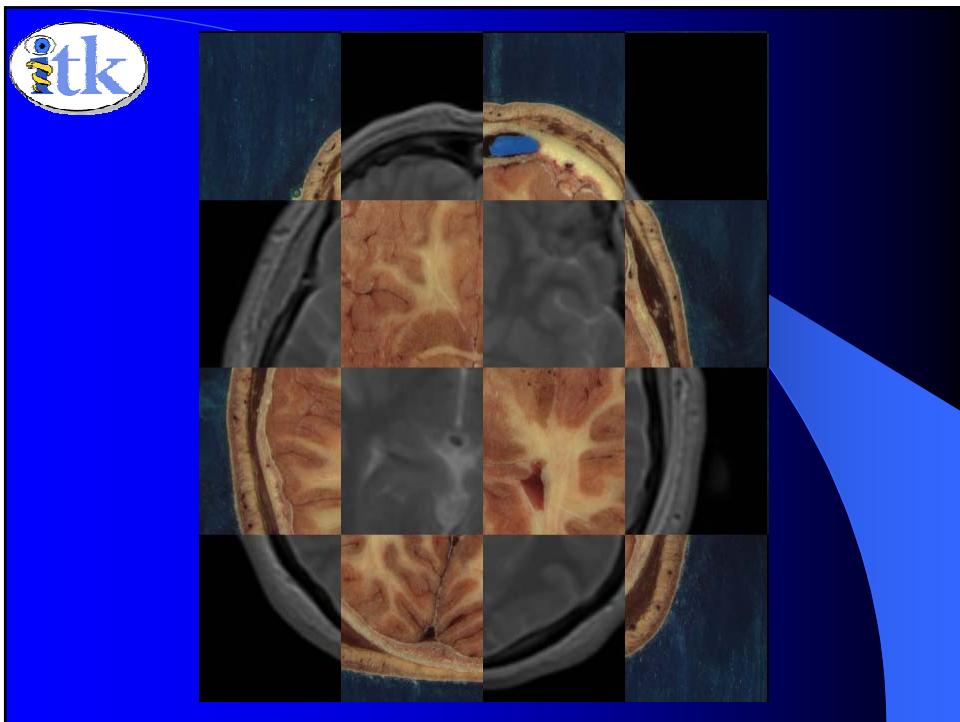


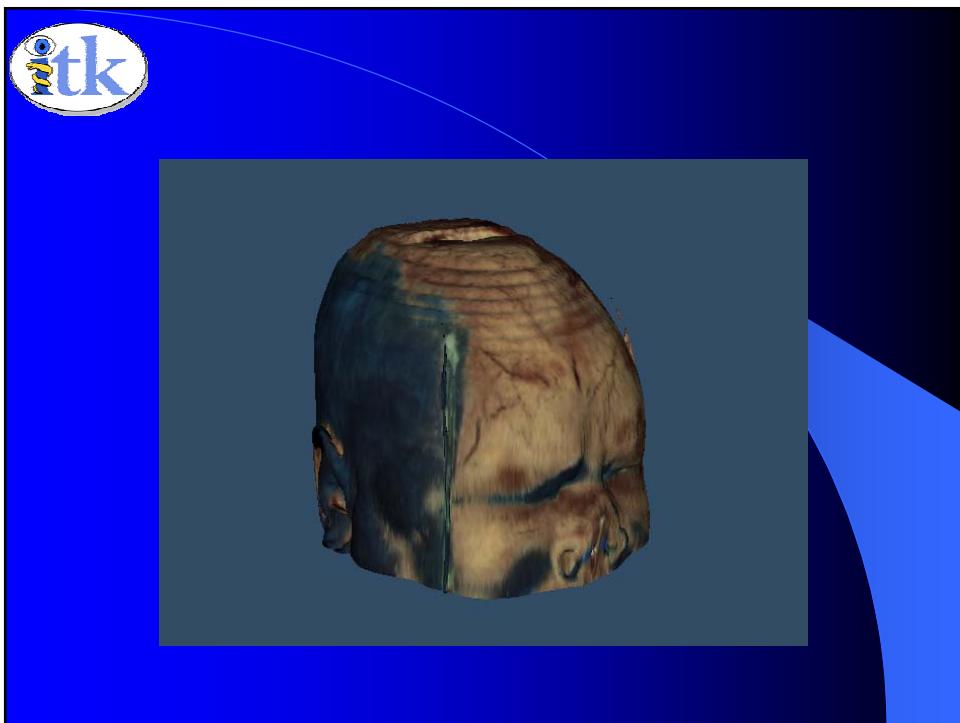
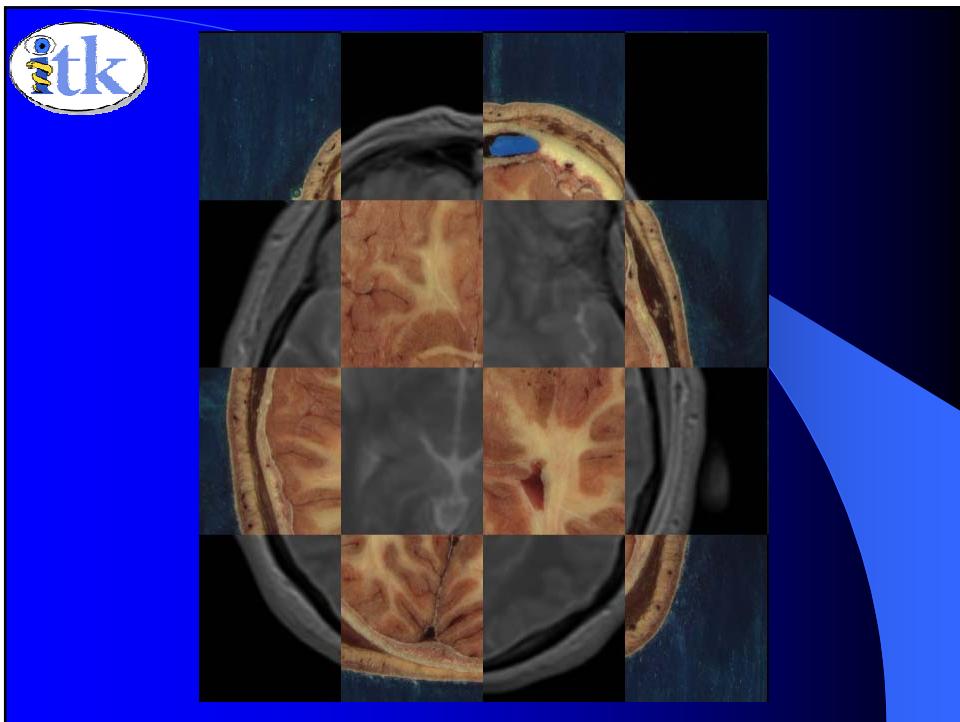


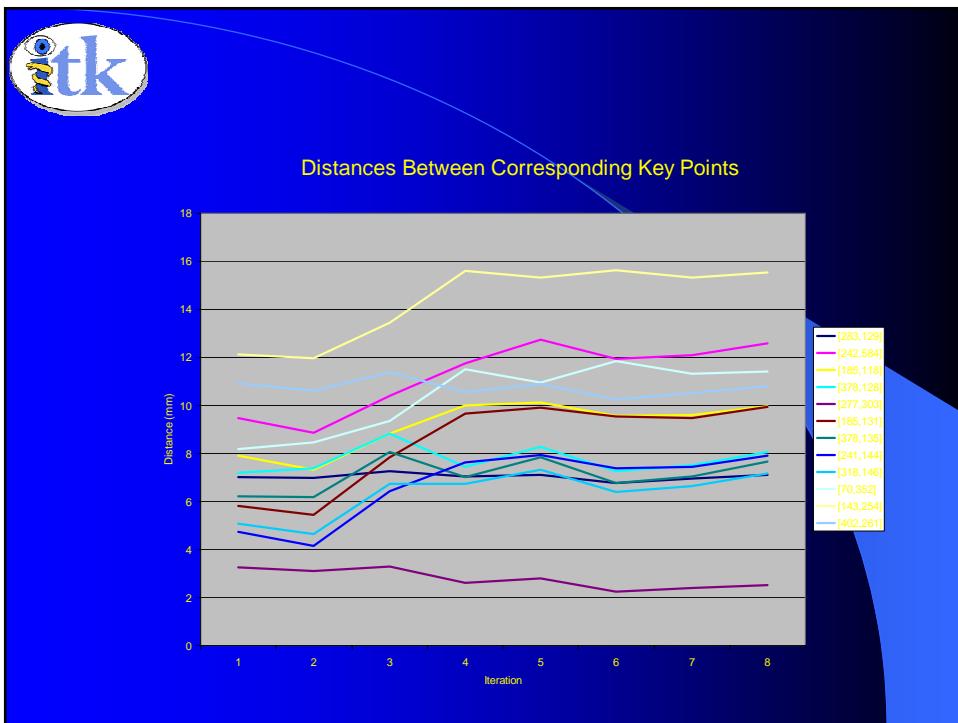
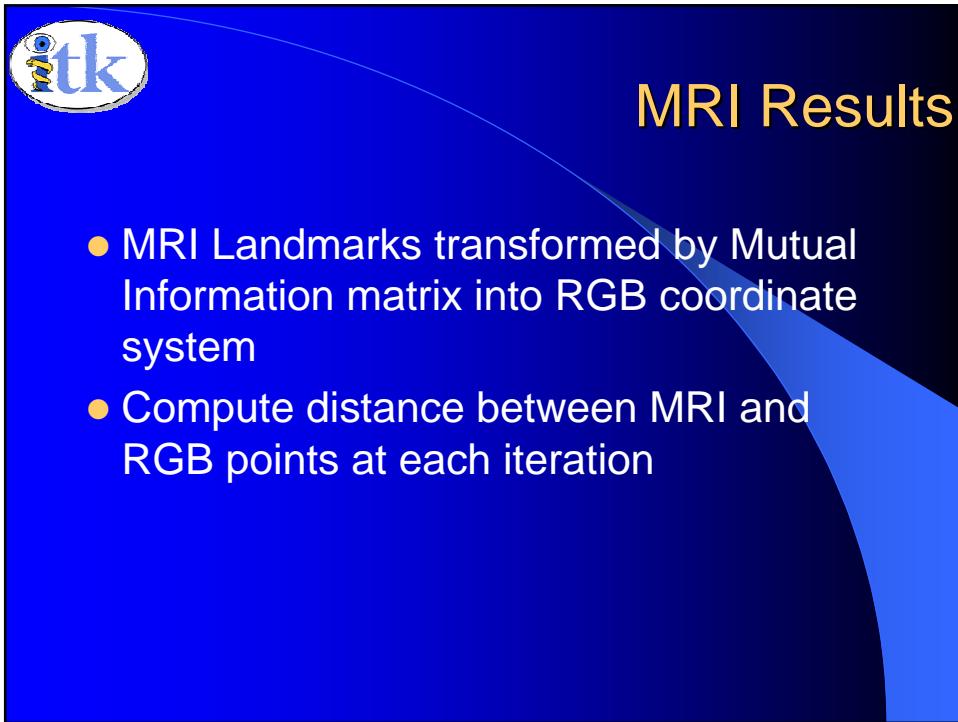








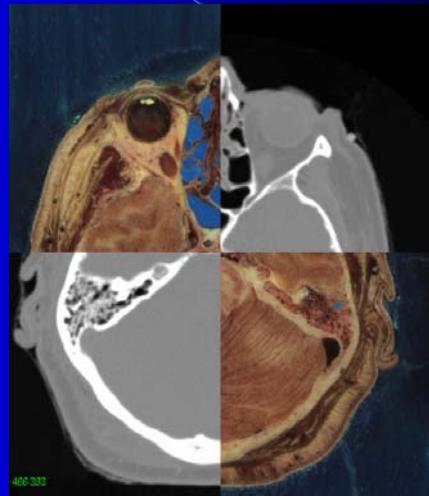






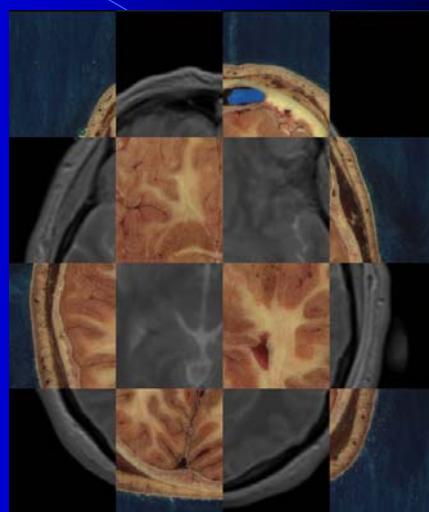
CT Discussion

- CT to RGB rigid body registration is a good first step for subsequent deformable registration



MRI Discussion

- MRI to RGB registration was not effective
 - Too much anatomical distortion occurred between the MR and RGB acquisitions

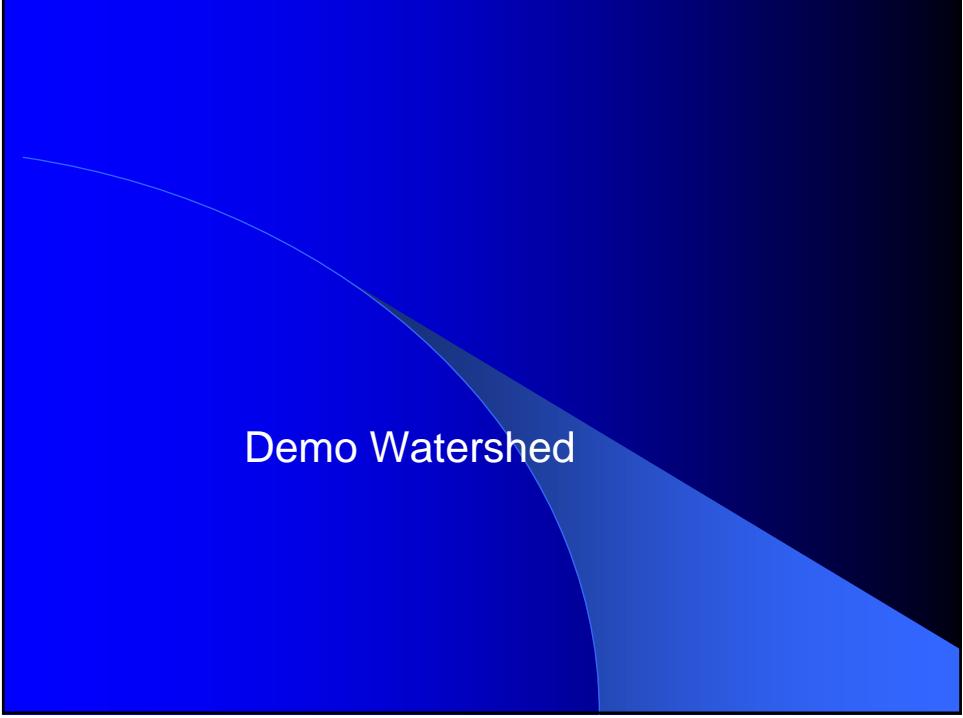


Examples

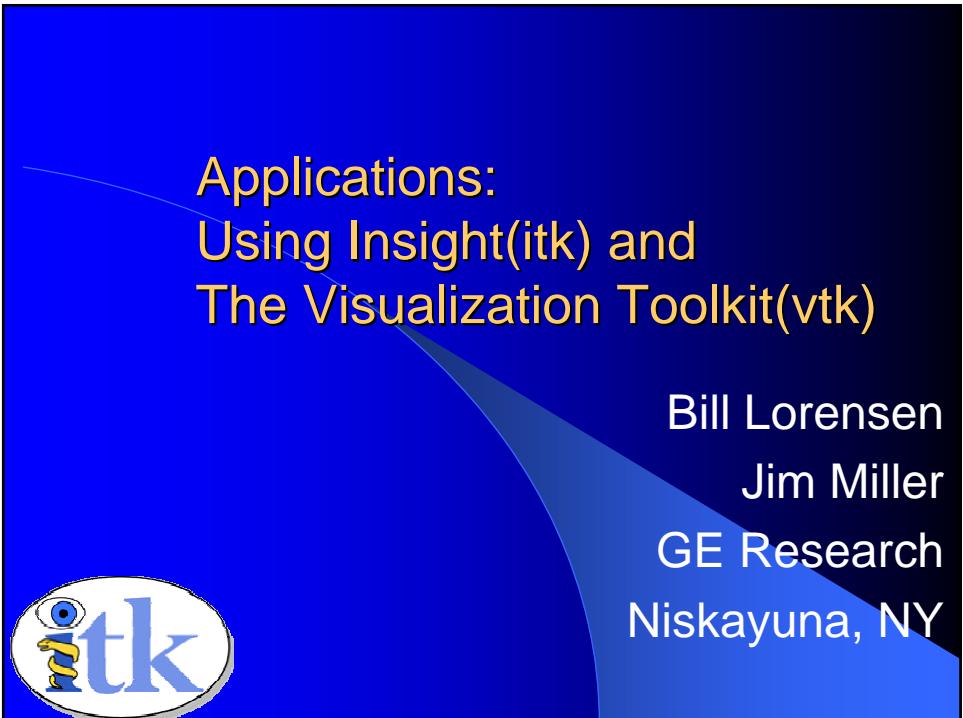
Segmentation

Watershed Segmentation

- I/O and Visualization with vtk
- Image processing and segmentation with itk
- User interface with tk
- Prototype in tcl



Demo Watershed



Applications:
Using Insight(itk) and
The Visualization Toolkit(vtk)

Bill Lorensen
Jim Miller
GE Research
Niskayuna, NY



ITK Meets the Virtual Soldier



GE Global Research

Bill Lorensen, Jim Miller

Dirk Padfield, James Ross

Wes Turner

lorensen@crd.ge.com

Outline

- Atlas Quality Control
- Model Generation
- Implicit Anatomical Modeling
- Registration
- Model Refinement Using Level Sets



Activities

- Atlas from NLM
- Reconciled labels
- Registered slices
- Computed bounding boxes
- Calculated adjacencies
- Generated models using vtkDiscreteMarchingCubes
- Colored models
- Registered atlas to CT
- Atlas as seed for level sets
- Deformation of man to woman

February 2005

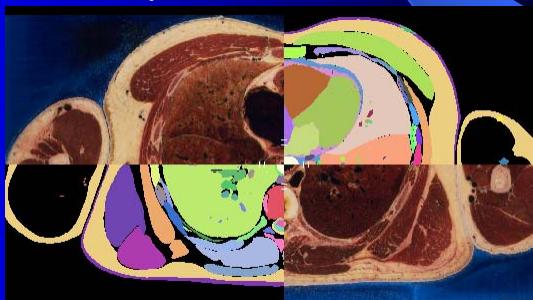
SPIE Tutorial



Atlas Quality Control

- Thorax Atlas consists of 411 70mm camera cryo-section slices and corresponding segmentation label maps

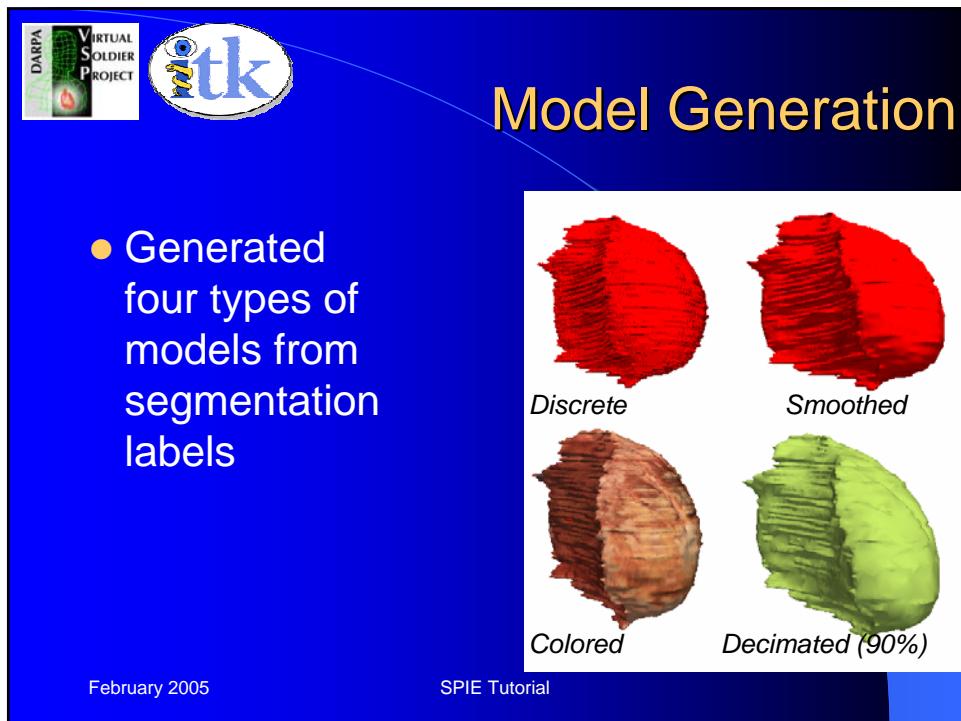
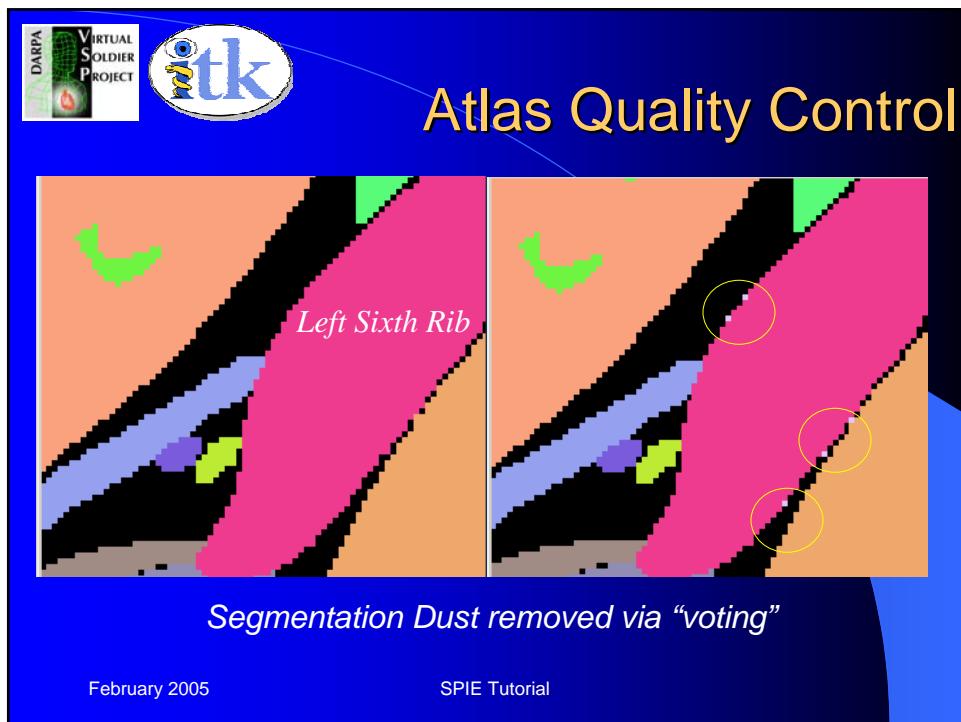
*Slice
Resolution:
2048 x 1350*

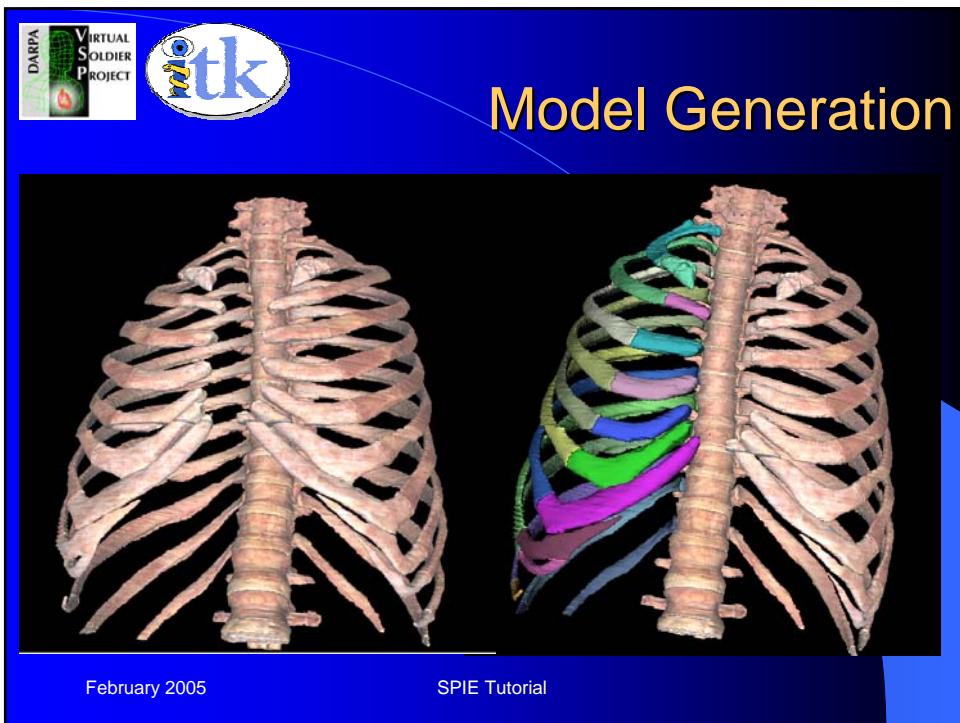
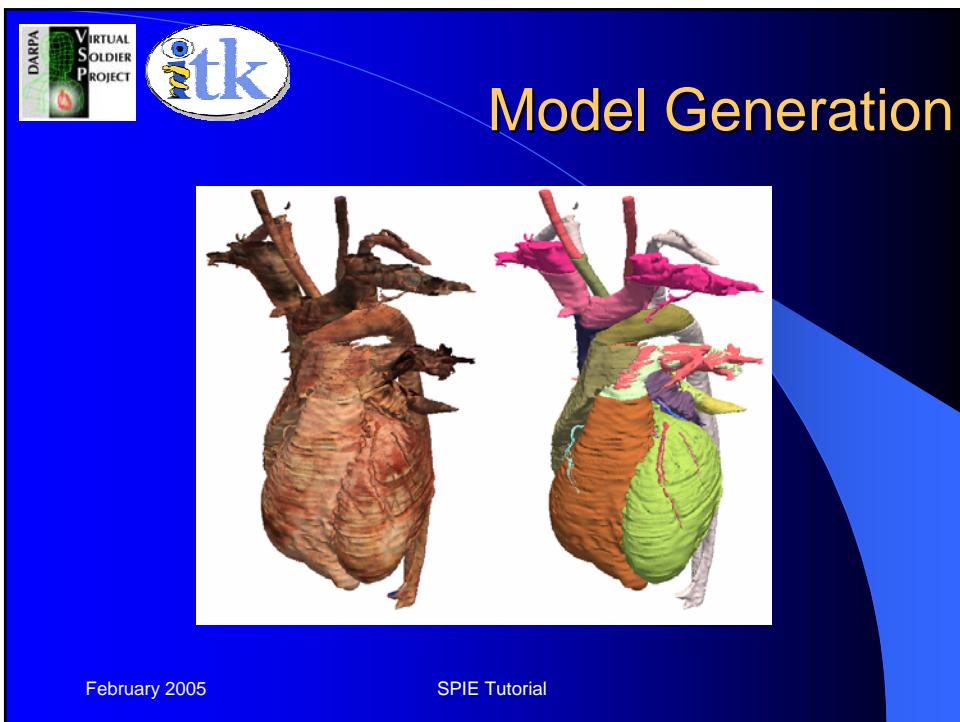


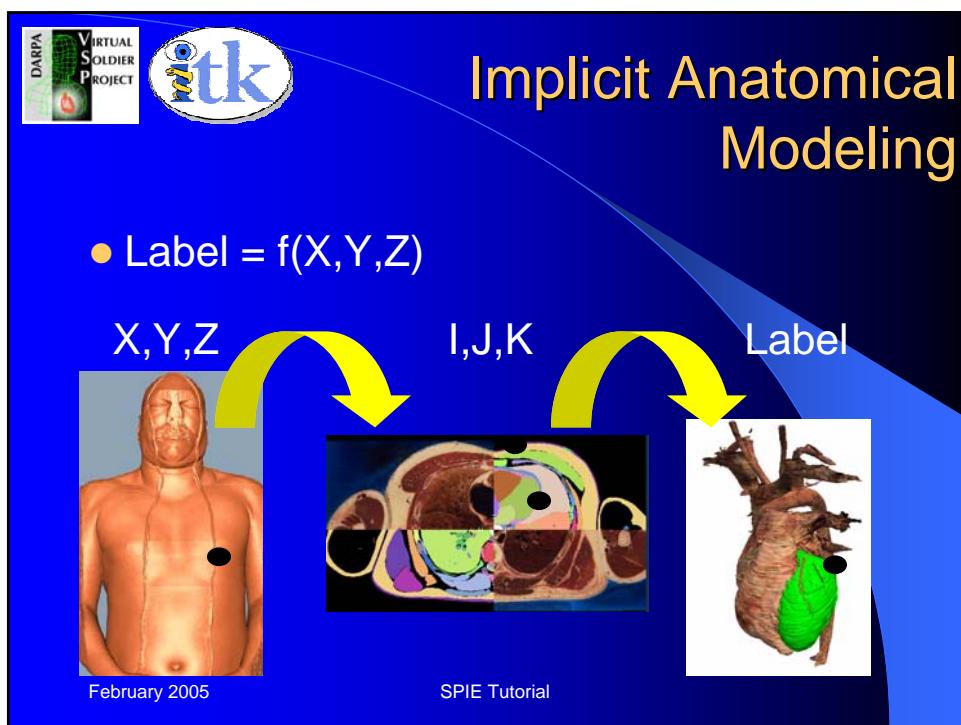
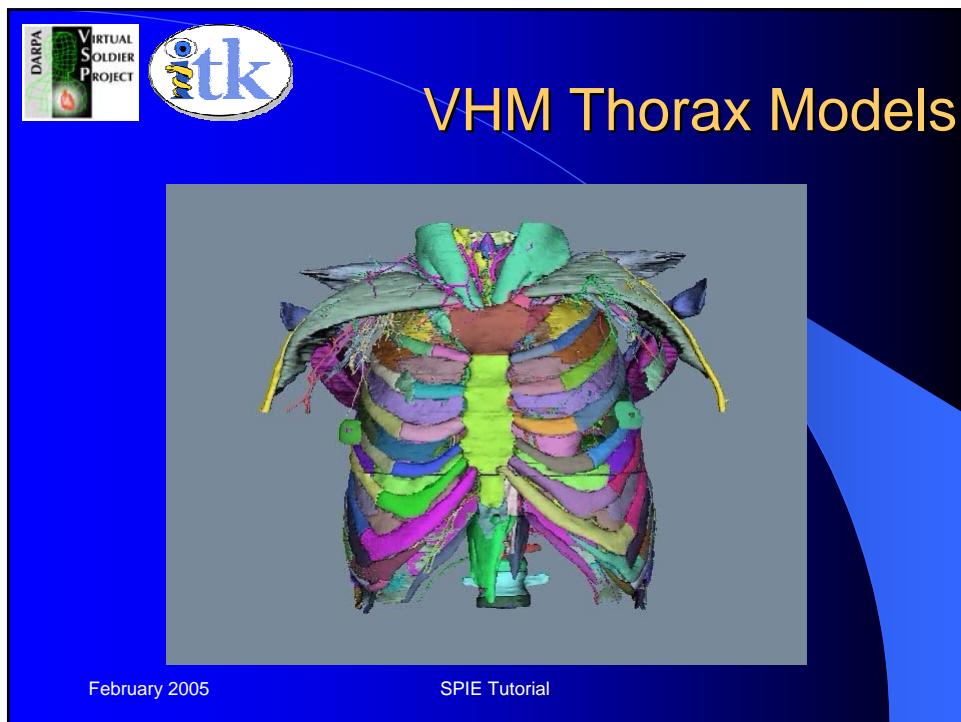
February 2005

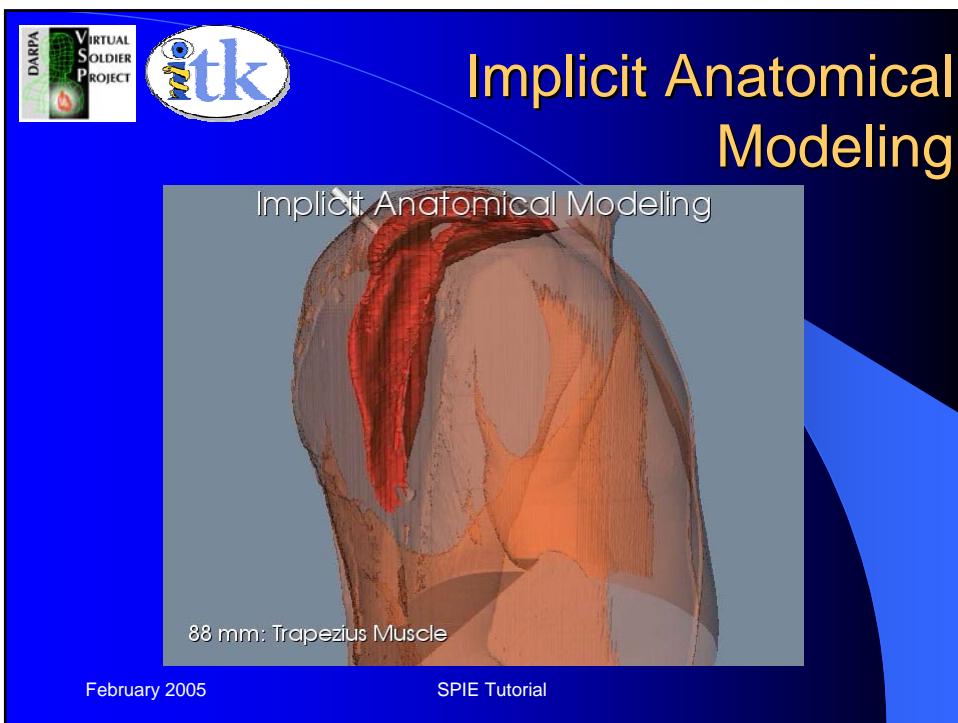
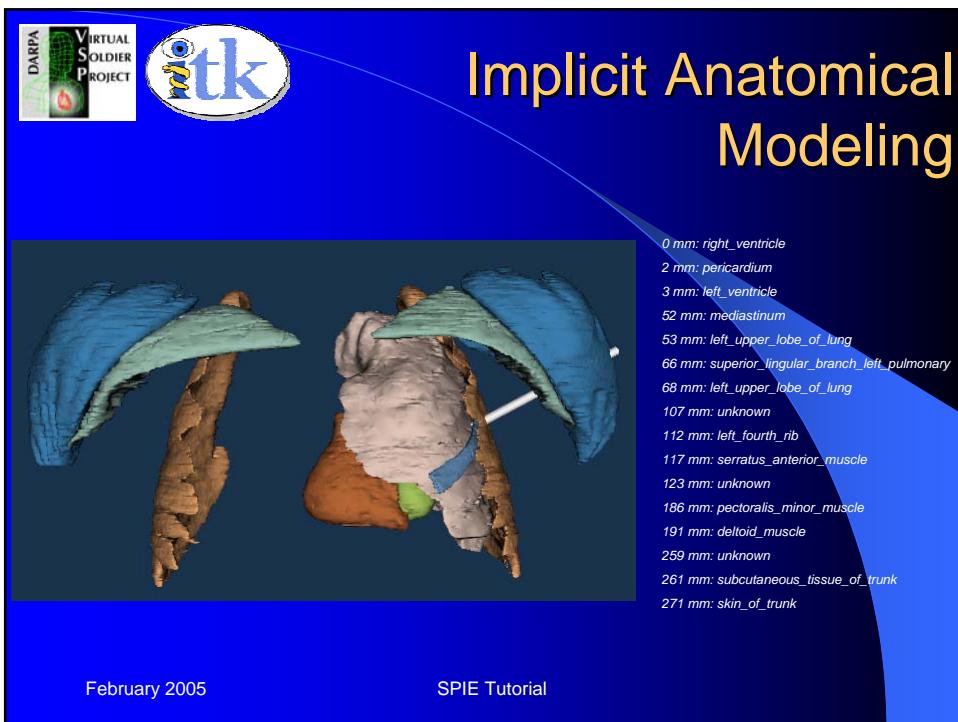
SPIE Tutorial

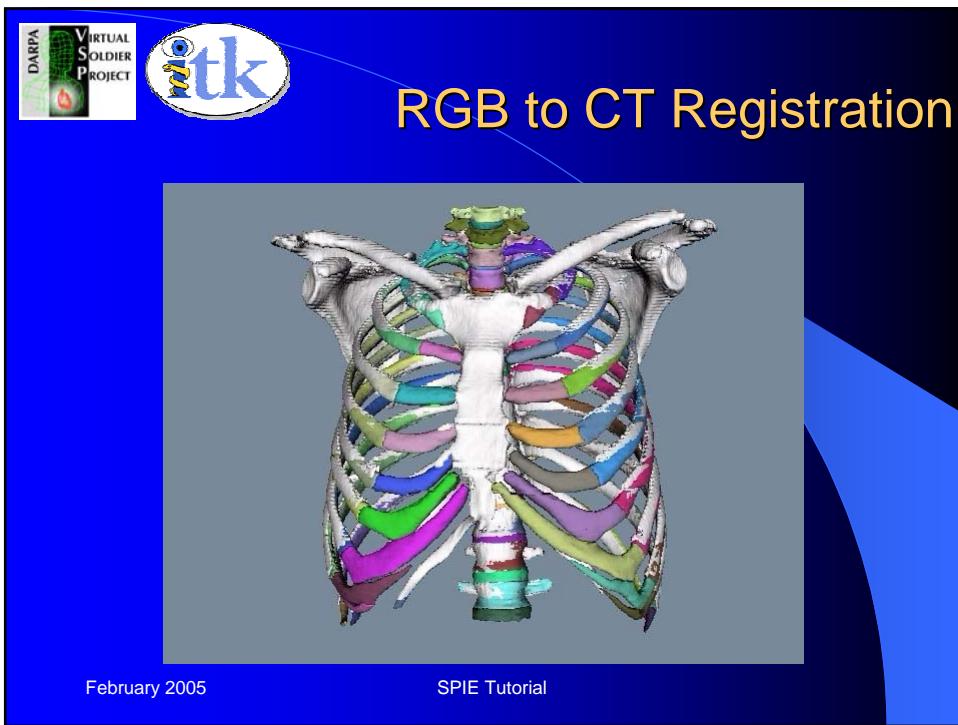
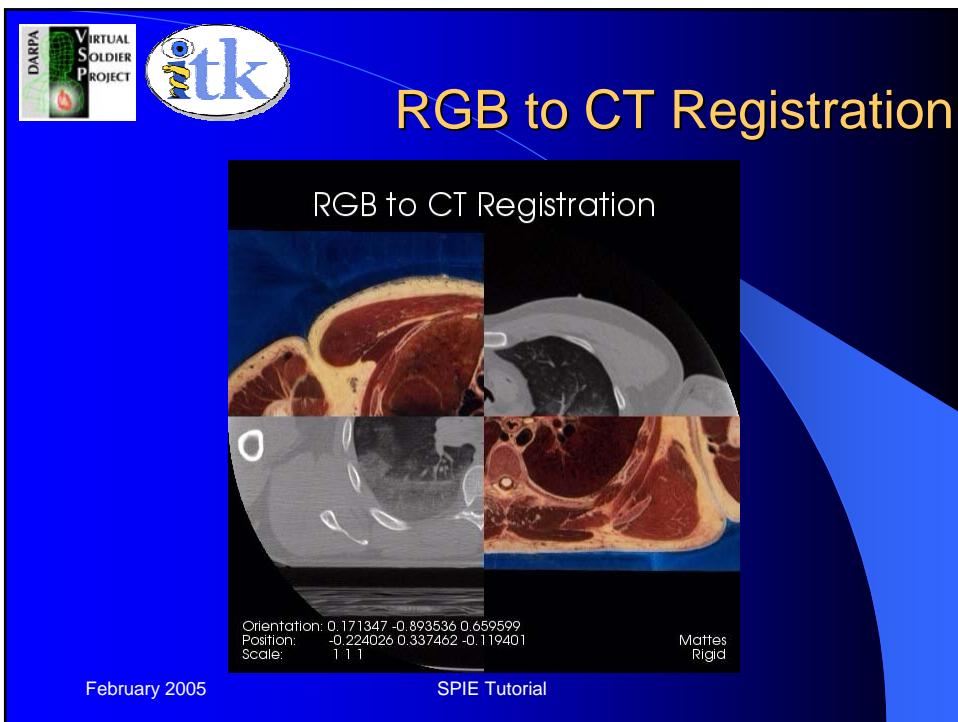


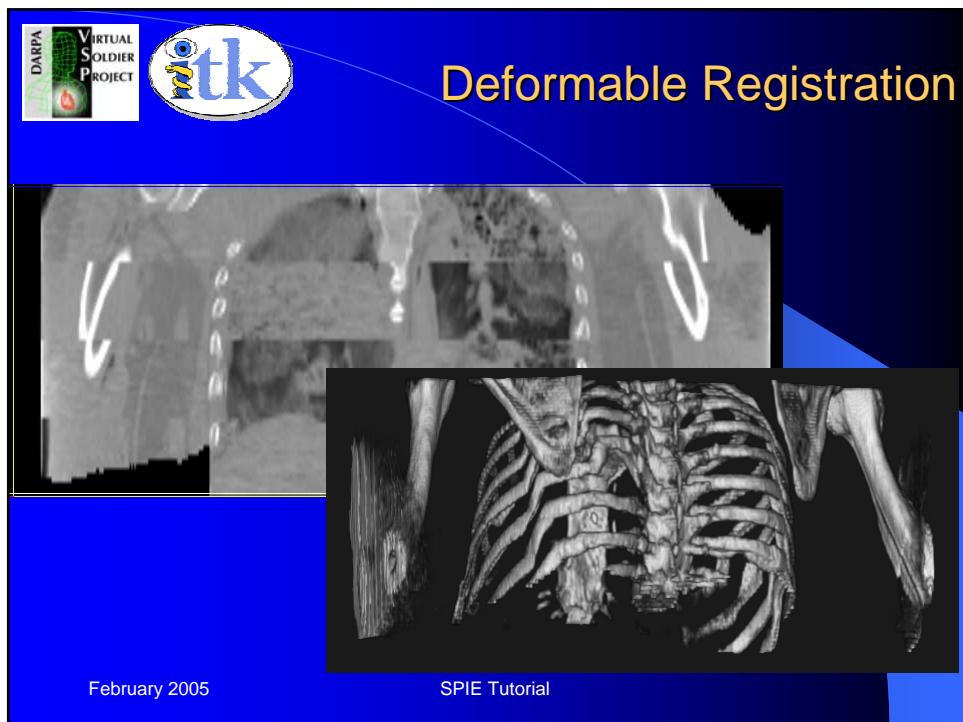


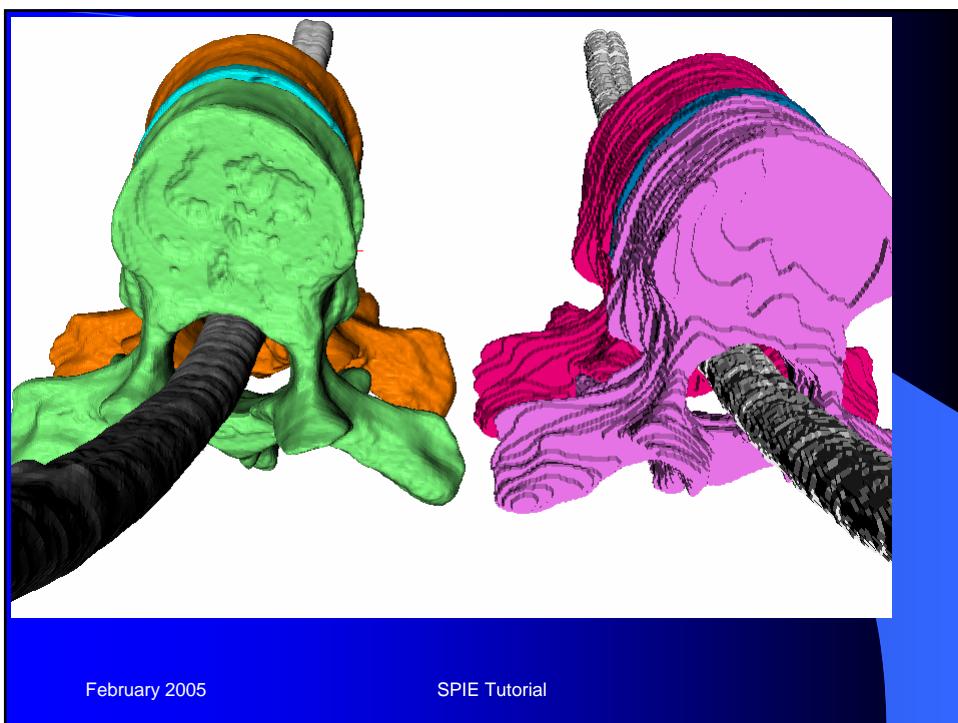
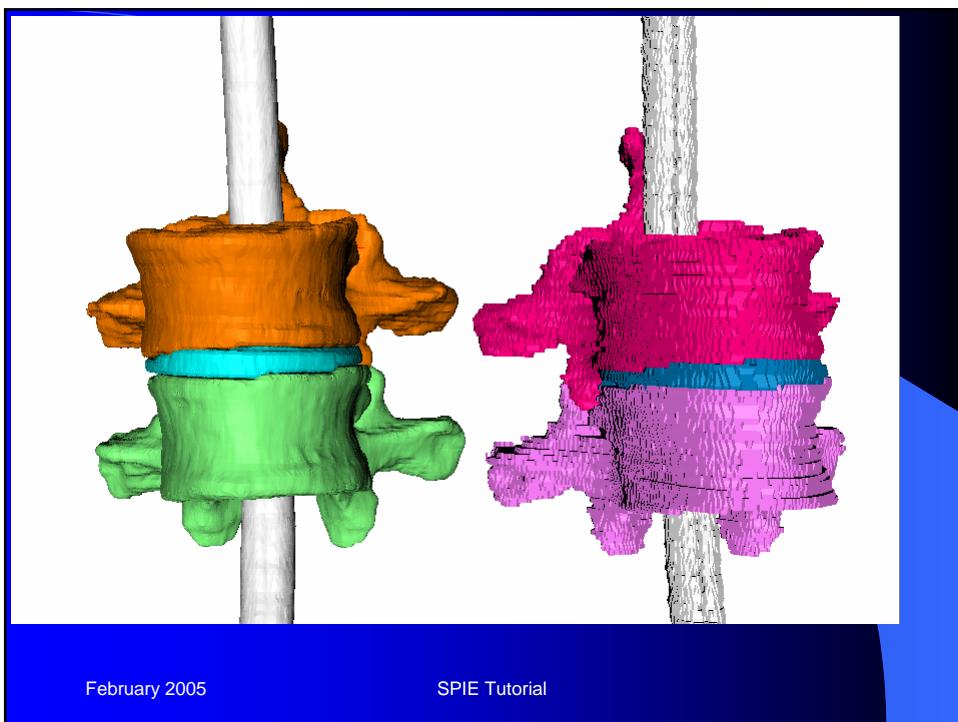














LevelSet Model Refinement

- Powerful technique to track the evolution of surfaces using image based constraints and forces
- Three techniques investigated
 - Threshold Level Set
 - Laplacian Level Set
 - Canny Level Set
- All techniques are part of Insight Toolkit (itk)

But: Algorithm parameter space is high!

February 2005 SPIE Tutorial

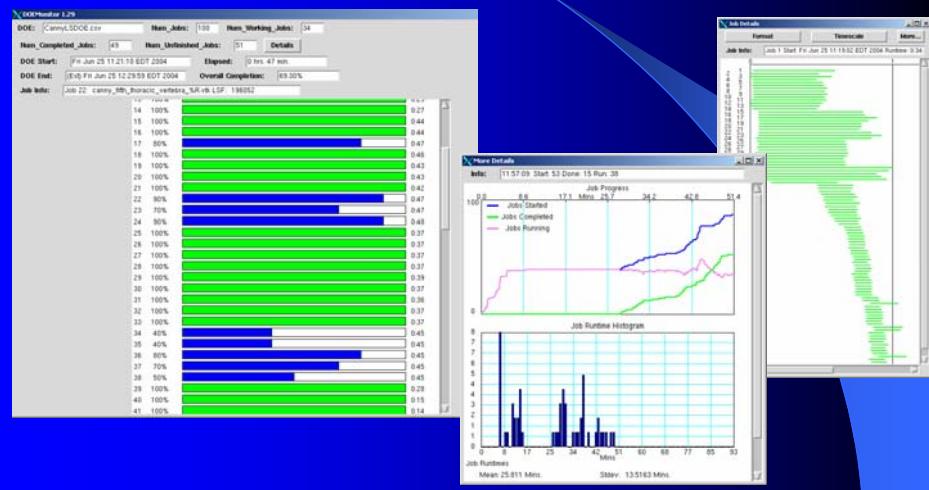


Load Sharing Facility

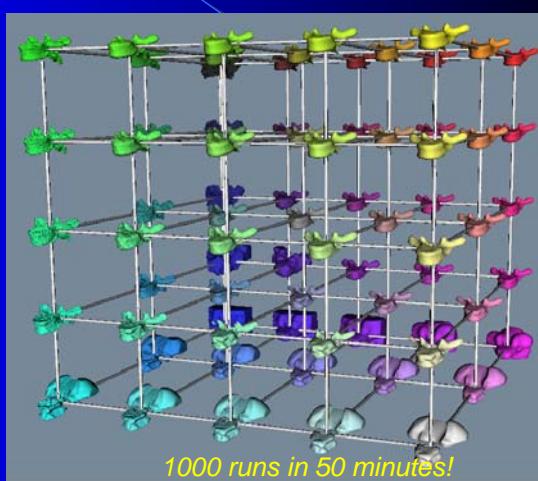
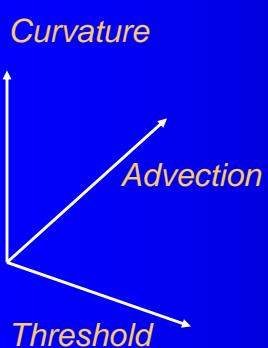
- 256 3.2 Ghz Dual Processor Xeon
- 2 gig of memory each
- Jobs scheduled with Load Sharing Facility (LSF)
 - Platform Computing Corporation
- LSF Toolkit
 - GE Research front-end and monitoring

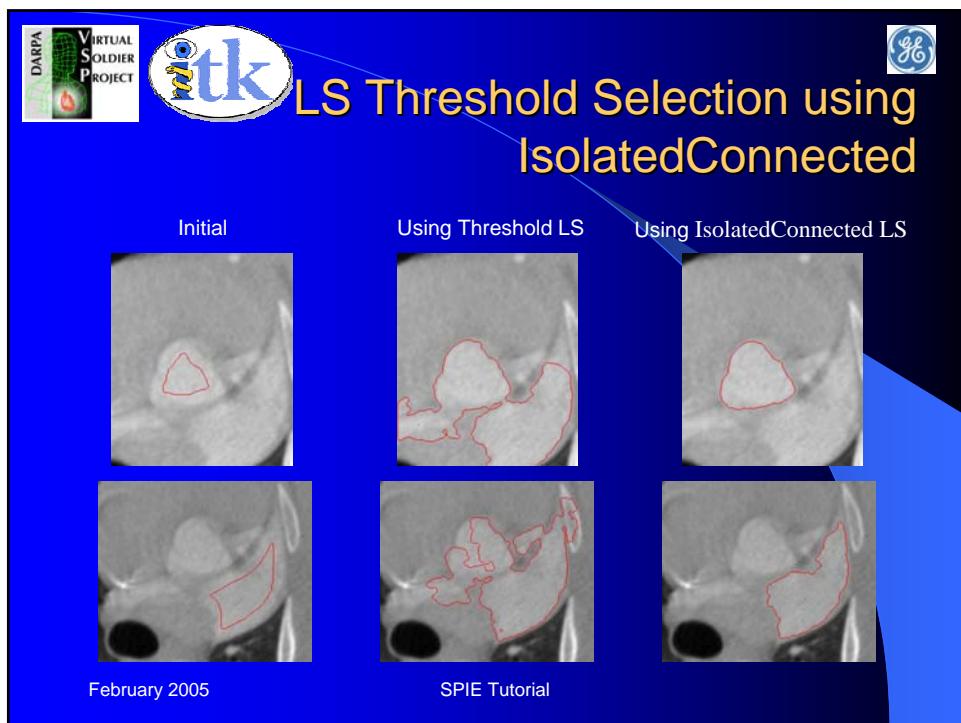
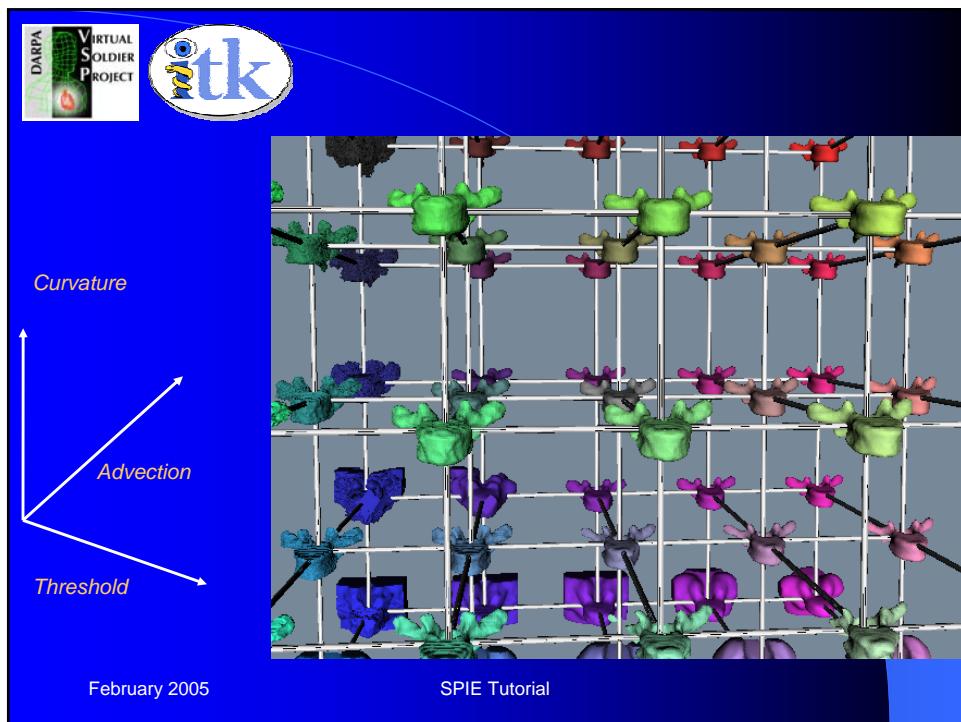
February 2005 SPIE Tutorial

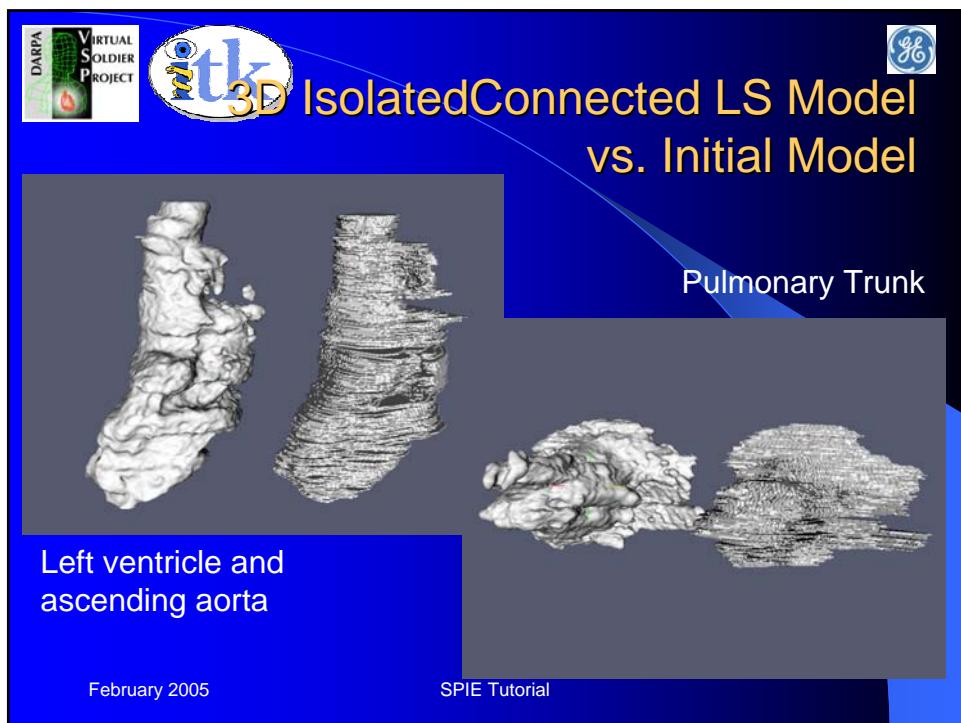
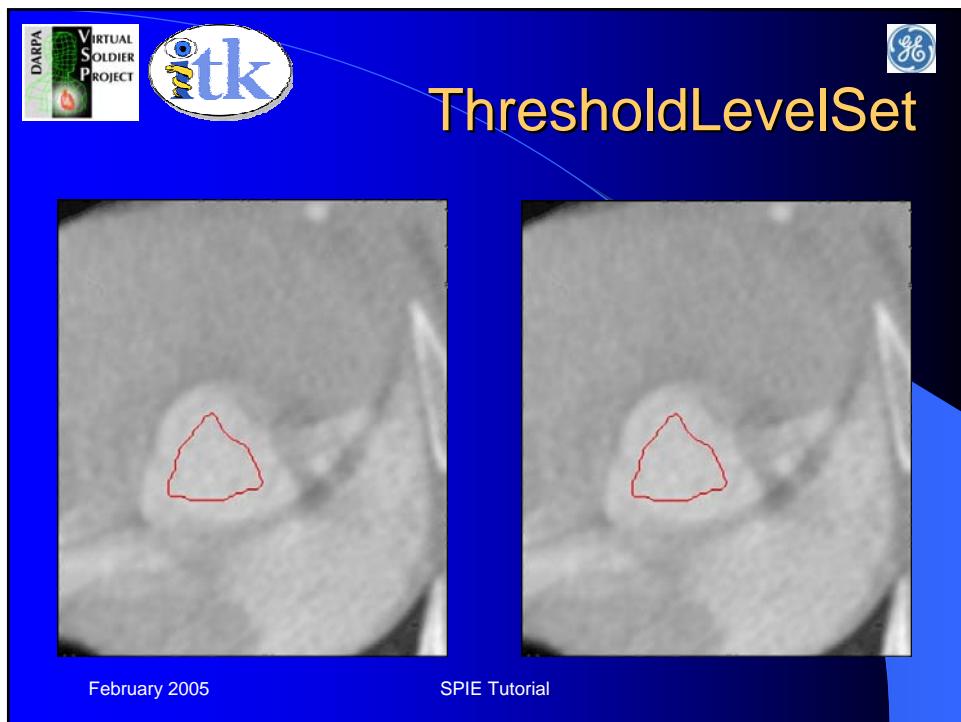
LSF Toolkit



Laplacian LevelSet DOE







ITK Meets the Virtual Soldier



GE Global Research

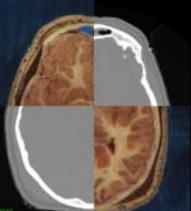
Bill Lorensen, Jim Miller

Dirk Padfield, James Ross

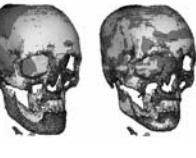
Wes Turner

lorensen@crd.ge.com

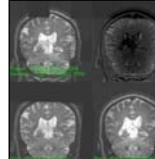
GE Research





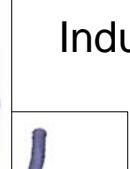



ITK in an Industrial Research Lab



ITK in an Industrial Research Lab

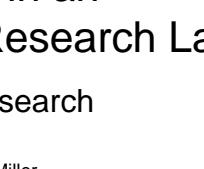
GE Research

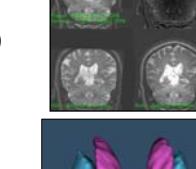









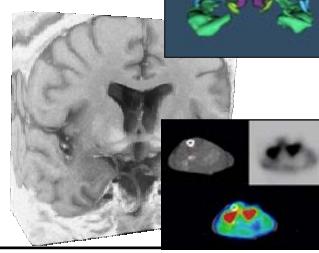




ITK in an Industrial Research Lab

GE Research

Jim Miller
 Bill Lorensen
 Dan Blezek
 Majeid Alyassin
 John Schenck
 Zhu Li
 Matt Turek
 Paulo Mendonça
 Dirk Padfield
 James Ross

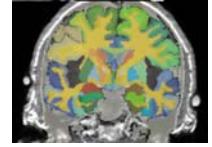
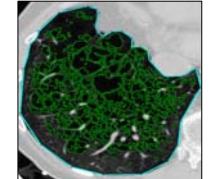


GE Research

ITK at GE Research

- Alzheimer's Research
 - Exploratory Research
 - Molecular Imaging
 - Diagnostic Pharmaceuticals
- Chronic Obstructive Pulmonary Disease
 - Research Tool Development/Product Development
 - Image Guided Clinical Trials
- Both projects are quantitative imaging projects
 - Reduce images to numbers
 - Volumes, Areas, Percent change
- Both projects are studying a disease from an imaging perspective
- Both projects use ITK along with other toolkits and applications

ITK in an Industrial Research Lab

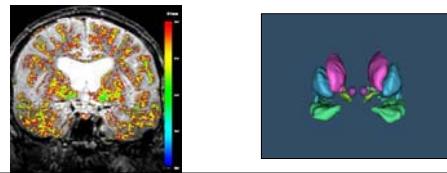




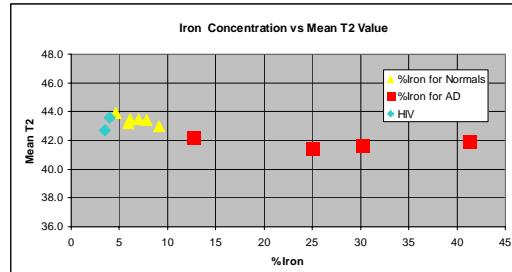



Alzheimer's Research

- Hypotheses:
 - Alzheimer's patients have elevated brain iron concentrations
 - B Drayer, et al., Am. J. Neuroradiol. 7, 373-380, 1986.
 - JF Schenck, J. Neurol. Sci 134 (Suppl.), 10-18, 1995.
 - Alzheimer's patients have volumetric differences in key brain structures
 - *"A discriminant function analysis demonstrated that a linear combination of the volumes of the hippocampus and the temporal horn of the lateral ventricles differentiated 100% of the patients and controls from one another."*
 - Killiany, et al., "Temporal Lobe Regions on Magnetic Resonance Imaging Identify Patients with Early Alzheimer's Disease". Archives of Neurology. 50:949-954, 1993



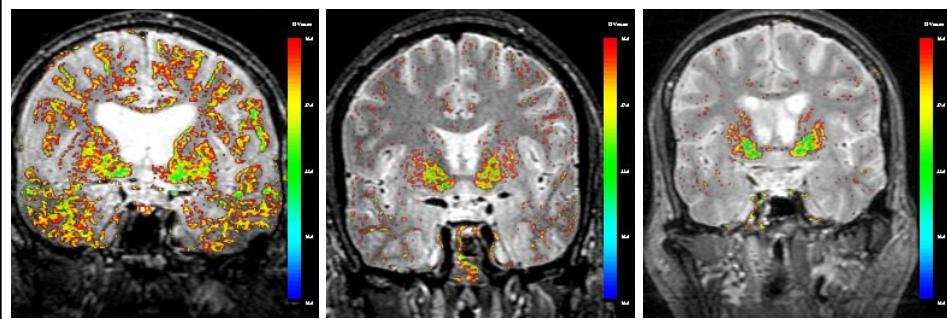
Brain Iron as AD Marker



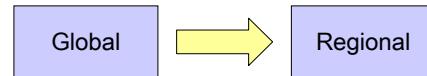
Alzheimer's Disease

Normal

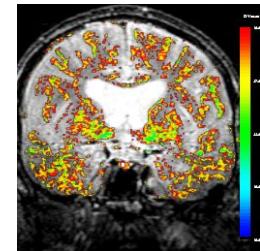
HIV



Brain Iron Regional Quantification



- Overall brain iron concentration can be used to assess Alzheimer's and monitor disease progression
 - Global assessment
- Regional quantification and analysis will lead to:
 - Increased understanding of disease locality
 - Monitoring patient specific disease progression
- Requires longitudinal analysis
- Requires registration of patient data
- Change detection, change monitoring



Longitudinal MRI with no registration

Checkerboard

Position: -0.426594 9.43833 1.30474
Orientation: 2.5817 7.61998 0.948923

Source
Original
image

Difference

Target
Original
image



Study: .../Kaye/114_0744/e1

Study: .../Kaye/114_1951/e1

GE Research

ITK in an Industrial Research Lab

Longitudinal MRI with mutual information registration

Checkerboard

Source Original image

Position: -0.426594 9.43855 1.30474
Orientation: 2.58177 6.61998 0.948923

Difference

Target Original image

Study: ./Kaye/114_0744/e1

Study: ./Kaye/114_1951/e1

GE Research

ITK in an Industrial Research Lab

Design of Experiments

Input Parameter	Minimum	Maximum
lungtest.learningRate	0.00001	0.001
lungtest.standardDeviationA	2	4
lungtest.standardDeviationB	2	4
lungtest.numberOfSamples	10	100
lungtest.numberOfIterations	1000	2000
lungtest.imageVariance	1	2.5

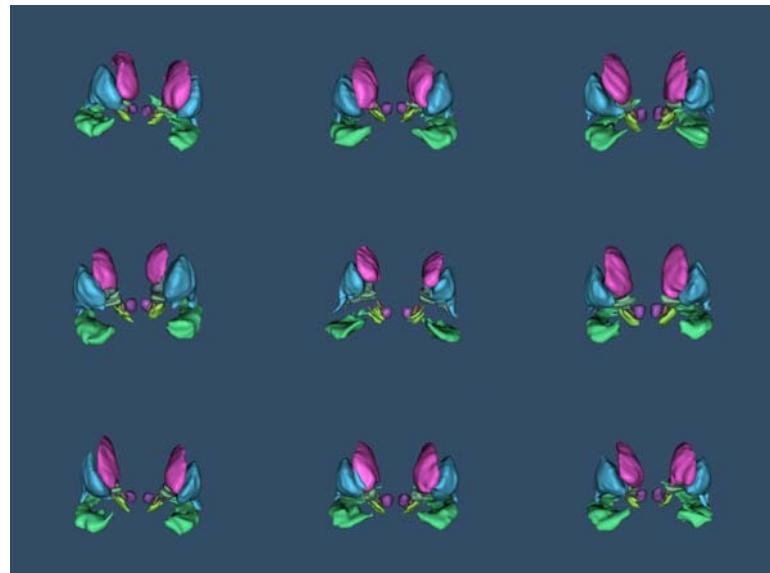
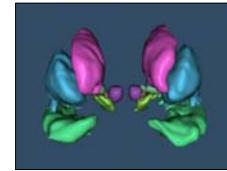
Output Parameters
lungtest.rotationError

Variable	Coded Coefficient	p	Interpret
Constant	2.08405444	4.7169E-05	
lungtest.learningRate	-3.2748267	5.9898E-24	Significant
lungtest.standardDeviationA	0.547888684	0.00295773	Significant
lungtest.standardDeviationB	0.606748	0.00111358	Significant
lungtest.numberOfSamples	-0.1768956	0.31743499	Insignificant
lungtest.numberOfIterations	-0.5026672	0.00456452	Significant
lungtest.imageVariance	-0.748968	8.7561E-05	Significant

Brain Iron Anatomical Quantification

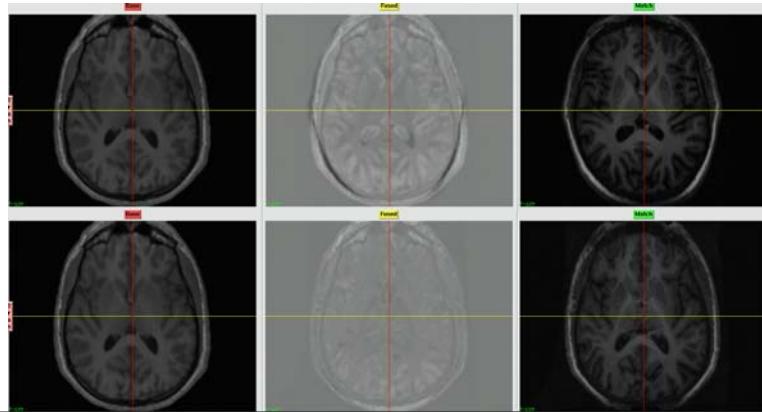


- 40 normals, 40 Alzheimer's patients
- 8 structures per case
 - Hippocampus, Caudate, Red Nucleus, Globus Pallidus, Putamen, Substantia Nigra, Nucleus Basalis, Subthalamic Nucleus
- Structures with subtle boundaries
- Hand segmented
 - Some on T1, some on T2
 - 1 case per day
- Analyze brain iron concentrations on structure by structure basis
- Hand segmentations provide a rich set of segmentation priors



Automatic Brain Structure Segmentation

- Just starting this effort
- Demon's-based atlas segmentation
- Statistical shape models

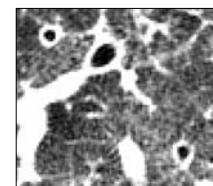
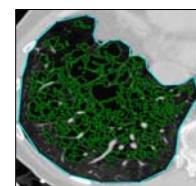


Chronic Obstructive Pulmonary Disease

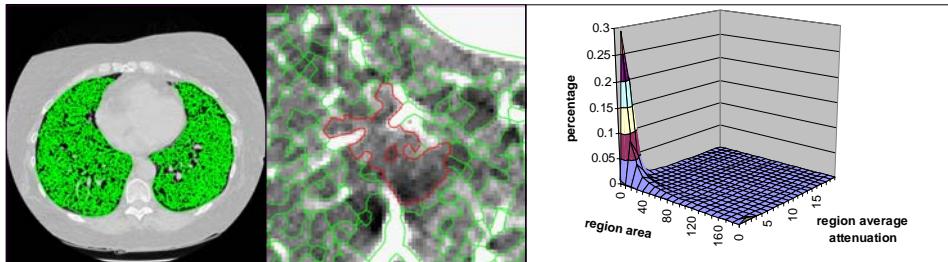


COPD is the 4th leading cause of death in the US.

- Emphysema
 - Parenchyma disease
 - Loss of lung tissue
 - Reduced capability to exchange gases
 - Loss of elastic recoil
 - Reduce capability to exhale
- Chronic Bronchitis
 - Airway disease
 - Thickening of airway wall
 - Restriction of airflow
- Quantitative analysis from CT images



Emphysema



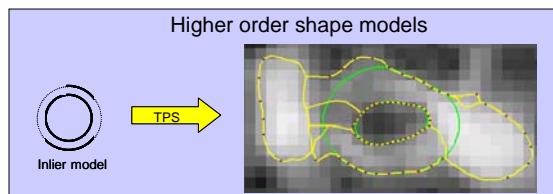
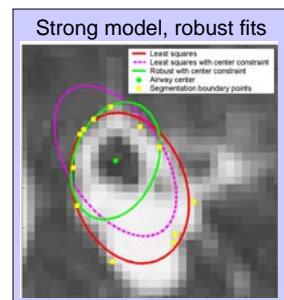
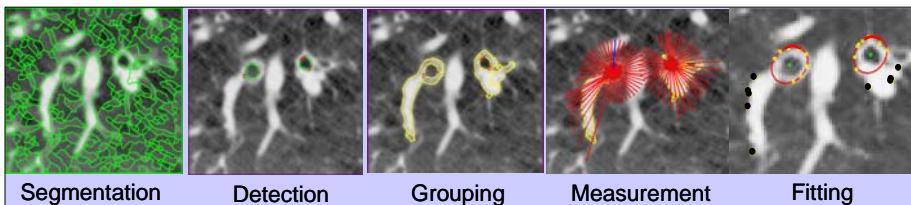
- Partition lung field into homogeneous regions
- Calculate features for each region
 - Intensity mean, intensity variance, region area, number of adjacent regions
- Compare multi-dimensional histograms to canonical cases
- Score severity on a 1-5 scale
- Legacy computer vision system

Class. rate (%) - Müller		
Chi-Square	63.16	92.11
Jeffrey	57.89	94.74
Match	50.00	92.11
EMD	52.63	94.74

5 class and 3 class performance



Chronic Bronchitis



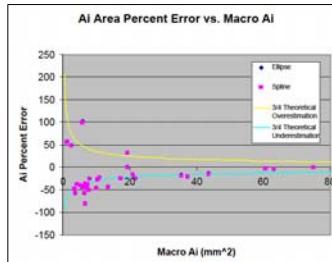
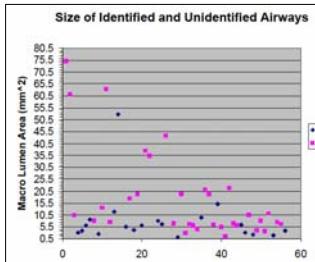
Airway wall study



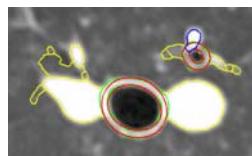
- Compare automated measurements derived from CT to manual pathology measurements from resected lung
- Pathology measurements are based on high resolution digital camera images
 - 6 times the resolution of CT
 - 2X read

Gage R&R

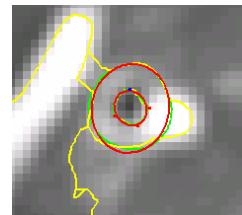
- Systematic bias on radii of $\frac{1}{4}$ pixel
- Similar to other techniques
- Due to scale and curvature interactions



120-3
Lumen Error: 38.3%
Wall Error: 54.1%

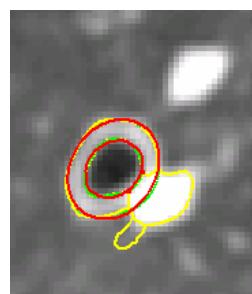


120-2
Lumen Error: 4.2%
Wall Error: 38.3%

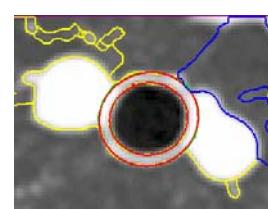


177-3
Lumen Error: 57.7%
Wall Error: 410.9%

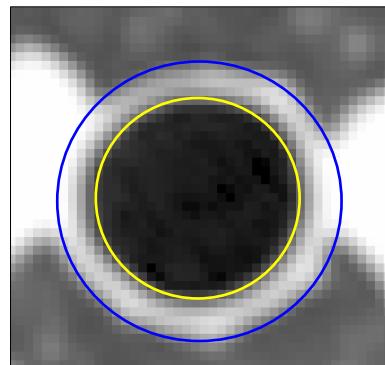
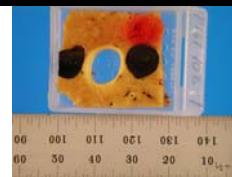
12-2
Lumen Error: 24.6%
Wall Error: 25.7%



103-1
Lumen Error: 2.9%
Wall Error: 6.2%

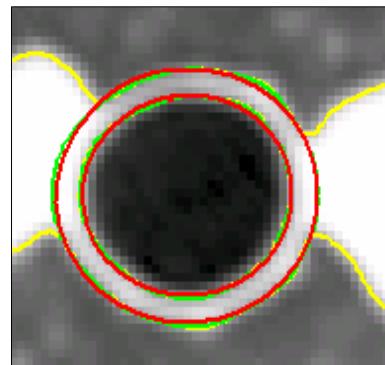


Pig Airway 102-1 (9 mm Lumen Diameter)



Pathology Measurements

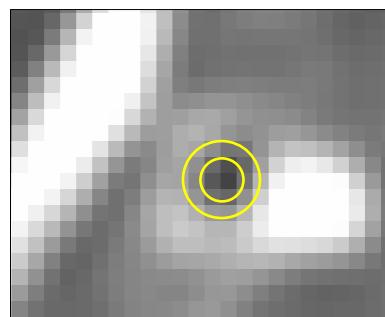
Lumen Area: 75.02 mm^2
Wall Area: 101.15 mm^2



Automatic CT Measurements

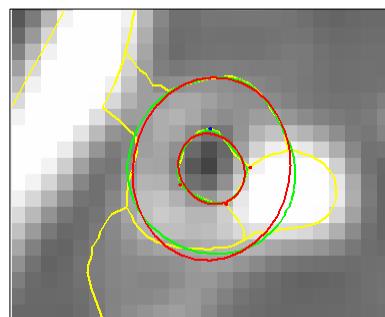
Lumen Area: 75.27 mm^2 (0.32 % Error)
Wall Area: 107.38 mm^2 (6.2 % Error)

Pig Airway 177-3 (~1 mm Lumen Diameter)



Pathology Measurements

Lumen Area: 1.36 mm^2
Wall Area: 2.54 mm^2

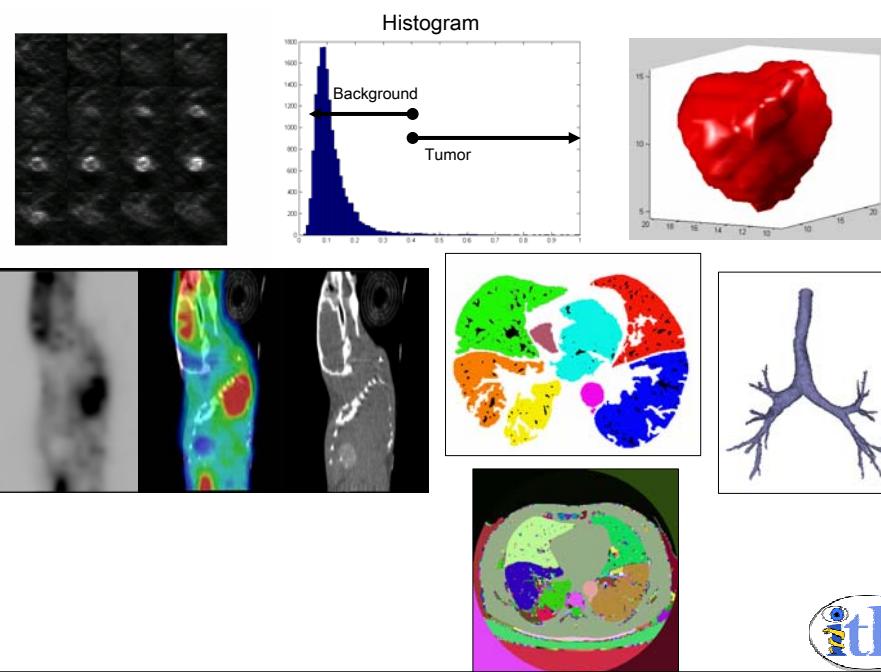


Automatic CT Measurements

Lumen Area: 2.14 mm^2 (57.7 % Error)
Wall Area: 12.96 mm^2 (410.9 % Error)

Other ITK Applications

- PET Segmentation
 - Otsu, Expectation-Maximization, Markov Random Field
- Small Animal Research
 - CT + PET Mutual Information Registration
- Surgical Navigation
 - CT + MR Mutual Information Registration
- Computer Aided Detection
 - Watersheds, Level Sets, Connected Confidence, Bayesian Decisions
- Image Quality
 - Edge preserving smoothing, Histogram matching
- Facial Reconstruction
 - Geodesic morphology
- Virtual Soldier
 - Atlas-based segmentation
- Product Teams
 - Looking at reference implementations for registration, level sets, etc.



Life at an Industrial Research Lab

Academia

Publish

Publish

Publish

How

Why

Industrial Research

Evaluate

Accelerate

Harden

Extend

Invent

Industry

Product

Product

Product

What

When



Slicer Overview

Steve Pieper, PhD



Outline

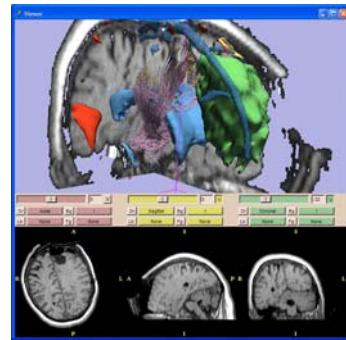
- **Slicer**
 - Overview and History
 - Architecture / Implementation
 - Image I/O and Management
 - Segmentation Tools (EM, Editor)
 - DT MRI Tools
 - fMRI Tools
 - Applications (IGT, Clinical Research)





What is 3D Slicer?

- **3D Slicer is...**
 - An end-user application for 3D medical image computing research and Image Guided Therapy
 - A platform for research where new techniques can be plugged into a useful framework
 - A freely-downloadable program with source and binaries for Windows, Linux, Solaris and (sort-of) Mac OSX
 - NOT an FDA approved medical device and CANNOT be used clinically without proper research controls (IRB etc.)
 - NOT finished – some parts will work better than others



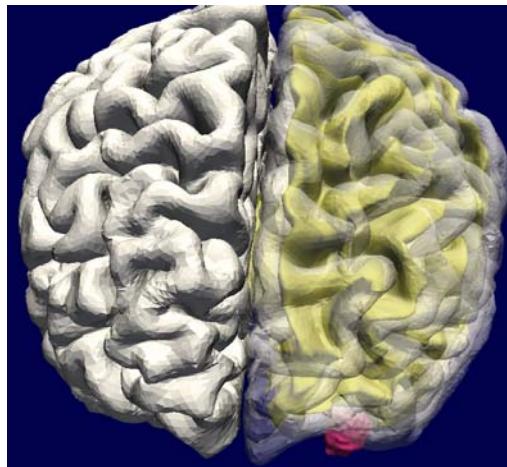
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Surgical Planning Example

**Dr. Jose Miguel Selman,
Clinica Las Condes,
Santiago, CHILE**

- Temporal Lobe Cavernoma
- MR Cortex and White Matter Extracted by FreeSurfer (MGH software, interface created for BIRN)
- Registration to CT and Visualization in Slicer



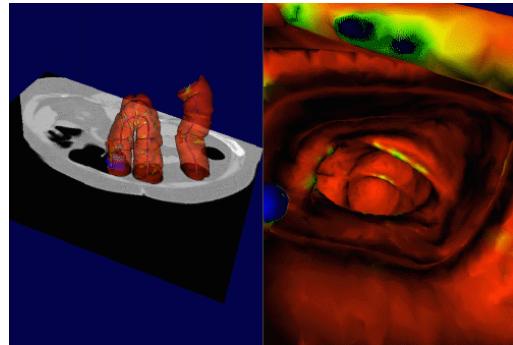
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Virtual Endoscopy Example

**Delphine Nain, MIT AI
Lab, now at Georgia
Tech**

- **Automatic or Manual
Path Planning**
- **Animated Camera
and Controls**



<http://www.ai.mit.edu/projects/medical-vision/virtual-endoscopy/>

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Slicer Background

- **SPL Image Guided Surgery and Visualization (Kikinis, Westin,
Hata, Halle, others)**
- **Slicer Application Pulled Together by Dave Gering 1997-1999
with VTK and Tcl**
- **Further Development and Architecture by Lauren O'Donnell
1999-2001**
- **Ongoing Development of Slicer's Base Primarily by Steve
Pieper and Nicole Aucoin**
- **Many Modules and Contributions by Various Authors**
 - **BWH, MIT, MGH, Georgia Tech, UCSD, JHU...**

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Why Develop with Slicer?

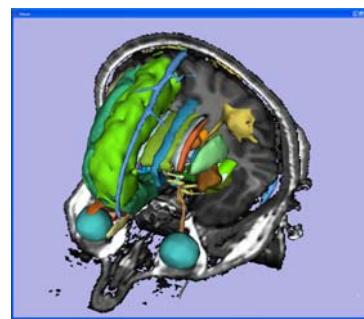
- Start with a Powerful Platform
- Remove Obstacles to Problem Solving
 - Access to Every Layer of Source Code:
Numeric, Graphic, Network, etc.
- Commit to an Environment that will Always be Available
 - Not Tied Up in IP of Old Institution
 - Not Tied to Proprietary Platform with License Fees
- Keep Your **Own** Work Available to **You**

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Slicer Today

- 300K Lines of Code
 - Cross-Platform Tcl/Tk GUI
 - VTK/ITK Based C++ Computing
- www.slicer.org
 - 166 on slicer-users
 - 117 on slicer-devel
 - 4000 Registered Downloads



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Architecture

- **Plug-in Modules** consist of **Tcl** and **C++** code with cross-platform file layout for building and loading
- Standard naming convention and hooks to add GUI and processing components
- Personally, I find the speed of **C++** and the interactive development of **Tcl** to be a near-perfect environment



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Features

- Load Medical Image Data: MR, CT in DICOM, GE, Analyze...
- XML-based File Format: **MRML** (Medical Reality Markup Language)
- Interactive Editor: Draw, Threshold, Math Morphology...
- Automated Segmenters: EM Segmentation, Fast Marching, Level Sets...
- Visualization: Model Building, Stereo Rendering, Animation...
- Registration: Manual, ITK, CNI
- Measurement: Fiducial-Based, Volumetric, Polyhedral Intersection, Vessel Cross-Section, Osteotomy Planning
- IGT: Tracked Probes, Real-Time Images, Robot Control
- Additional Application-Specific Features in Modules...

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Administration

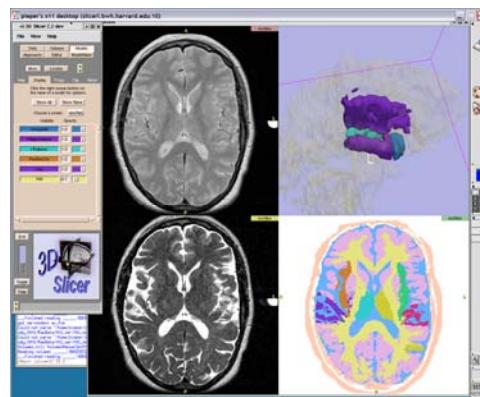
- Project Housed at Surgical Planning Lab, Brigham and Women's Hospital / Harvard Medical School, Many MIT CSAIL (formerly AI Lab) Students and Faculty Involved
- CVS, Mailing Lists, etc at the SPL
- Funded Projects Supporting Slicer Base Development
 - Neuroimage Analysis Center (NAC): NIH Center at SPL
 - Biomedical Informatics Research Network (BIRN): NIH Supported Neuroimaging Collaboration
 - Computer Integrated Surgical Systems and Technology (CISST): NSF Supported Robotics Collaboration Headed by JHU
 - Virtual Soldier: DARPA Organ Simulation Collaboration
 - National Alliance for Medical Image Processing
- Module Development Supported by Application-Oriented Grants

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Image/Scene Management

- XML-Based MRML File Stores Scene Description
 - Volumes (Images, Label Maps)
 - Models
 - Hierarchical Affine Transforms
 - Scene Data (Cameras, Colors, Fiducials, etc).
- Manipulated in World Coordinates based on Patient RAS
 - Automatically Extracted from DICOM or GE Files



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Image Formats

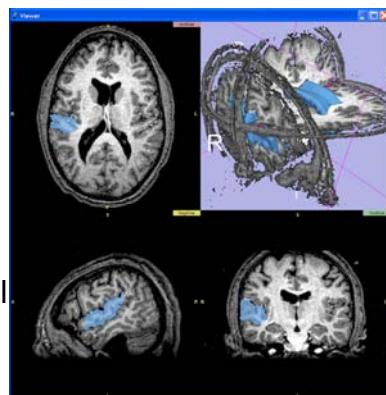
- DICOM, GE, Headerless, Analyze
 - Best Support for MR
 - CT and RGB Support limited
 - Real-Time from OpenMR and US
- Time Series
 - Analyze Sequence
 - DICOM Sequence
 - BXH Files
 - BIAC XML Header (Brain Image Analysis Center, Duke)
 - Like MRML for fMRI; Integration Work Ongoing

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User Segmentation Tools

- Label Map Editor
 - Draw on Orthogonal Planes
 - Connected Component “Island” Tools
 - Math Morphology
 - Image Masking and Logical Operations
 - Level Set, Fast Marching



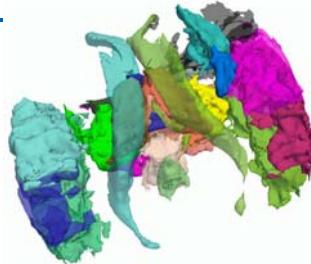
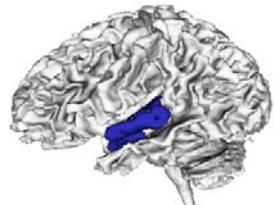
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EM Segmenter

Segmentation tool designed for fully automatic, high-quality parcellation of the brain*:

- Segmentation of cortical and ventricle substructures
- Multi channel input



- Hierarchical segmentation based on anatomy
- Multi threaded
- User friendly interface

* For further information see Pohl et al. "Incorporating Non-Rigid Registration into Expectation Maximization Algorithm to Segment MR Images" MICCAI 2002, pp. 564-572

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Models

- Triangle Meshes from Label Maps
 - Marching Cubes, Decimation, Smoothing
- Model Hierarchies
- Clipping By Slice Planes

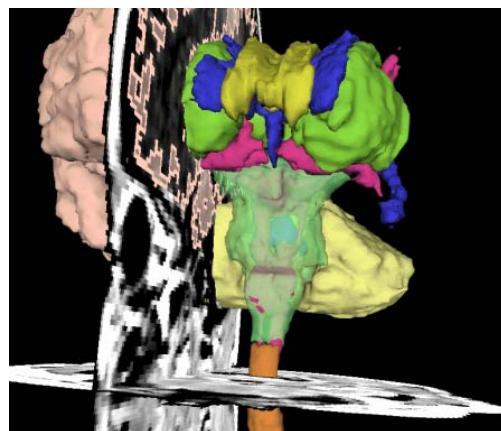


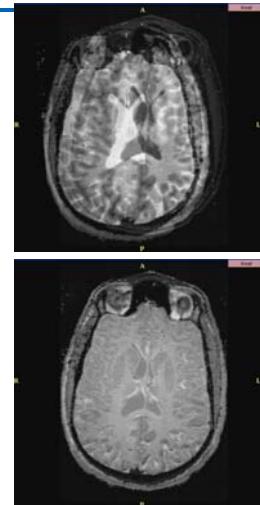
Image: Developmental Neuroinformatics, Simon Warfield

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Registration

- Interactive Manual Transform Editing
- Landmark Based Alignment
- Rigid Intensity Registration
 - Mutual Information Metric
 - ITK Implementation
- Non-Rigid Registration
 - Demon's Method
 - Available by Request to CNI

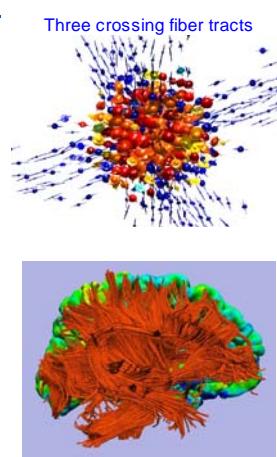


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Diffusion Tensor Tractography

- Multiple MR Gradient Acquisitions
 - Sensitive to Brownian Diffusion of Water
 - Cell Membranes Restrict Diffusion
- Post Processing to Extract Probable White Matter Tracts
 - Actual Tracts are Far Below the Resolution of the Scan



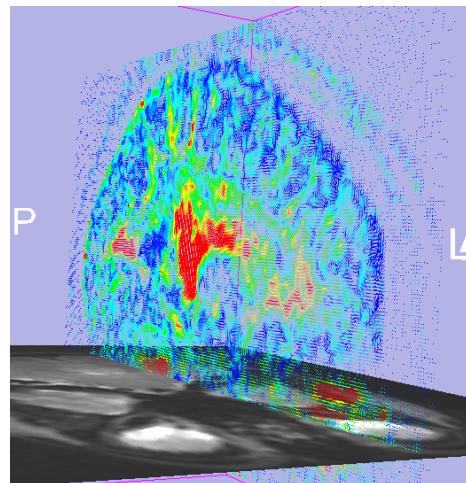
Images Provided by Westin, Park, O'Donnell et al

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DTMRI Tools

- Convert Gradient Images to Tensors
- Generate Scalars
 - ADC, FA, etc
- Visualize Glyphs
- Tractography
 - User Guided
 - From ROI

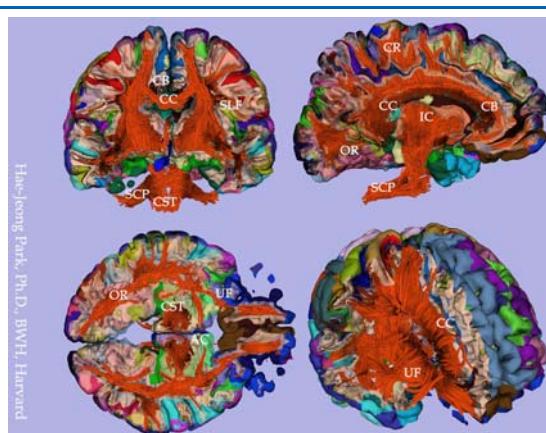


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Segmentation and Tractography

- Parcellation
 - Freesurfer (MGH)
- Tractography
 - DoDTI (H.J. Park)
- Visualization
 - Slicer
- Full Integration with Slicer
Planned



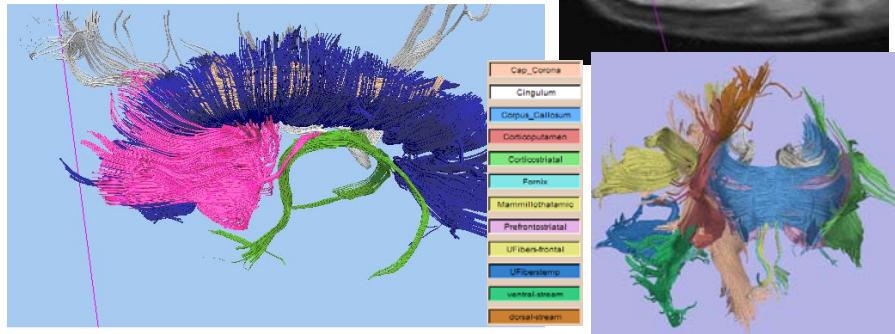
Hae-Jeong Park, Ph.D., BWH, Harvard

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DTMRI Examples

- White Matter Atlas
 - Under Development in Slicer by James Fallon, UCI

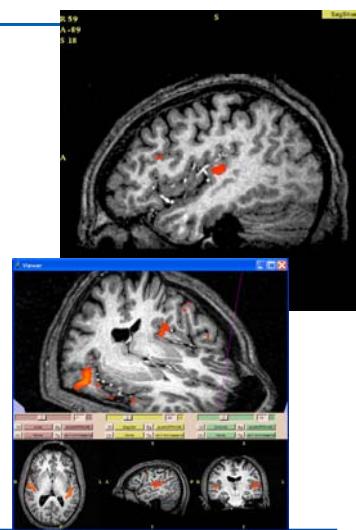


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Slicer fMRI Goals

- Advanced GUI and Interactive Visualization Environment
 - iBrowser
- Platform for Activation Detector Research
 - fMRIEngine
- Framework for fMRI Integration with Other Modalities

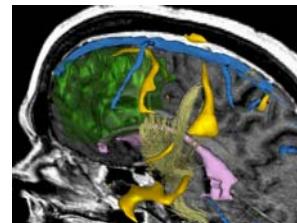
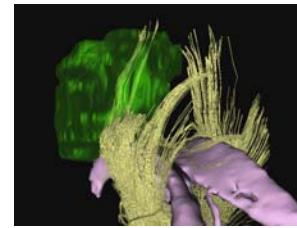


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Application: Pre-Operative Map

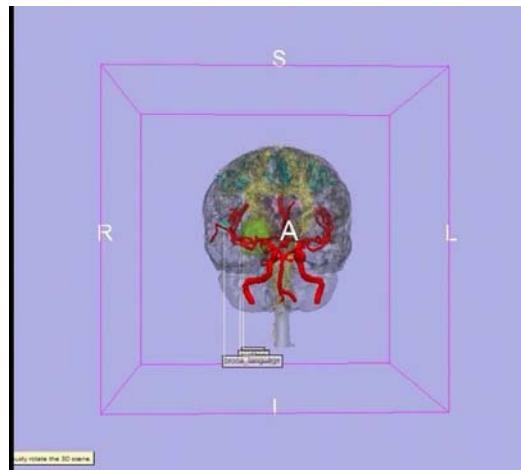
- Structural
 - MRI Tumor Segmentation
- DTI
 - Diffusion Tensor Imaging
- fMRI
 - Functional MRI
- MEG
 - Magneto Encephlogram
- Anatomy Atlas
 - "Textbook" Information



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Pre-Op Map Example



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Medical Image Analysis with ITK and Related Open-Source Software

This course introduces attendees to select open-source efforts in the field of medical image analysis. Opportunities for users and developers are presented.

The course particularly focuses on the open-source Insight Toolkit (ITK) for medical image segmentation and registration. The course describes the procedure for downloading and installing the toolkit and covers the use of its data representation and filtering classes. Attendees are shown how ITK can be used in their research, rapid prototyping, and application development.

LEARNING OUTCOMES

After completing this course, attendees will be able to:

- contribute to and benefit from open-source software for medical image analysis
- download and install the ITK toolkit
- start their own software project based on ITK
- design and construct an image processing pipeline
- combine ITK filters for medical image segmentation
- combine ITK components for medical image registration

INTENDED AUDIENCE

This course is intended for anyone involved in medical image analysis. In particular it targets graduate students, researchers and professionals in the areas of computer science and medicine. Attendees should have an intermediate level on object oriented programming with C++ and must be familiar with the basics of medical image processing and analysis.

COURSE LEVEL

Intermediate

COURSE LENGTH

Full-day (6.5 hours)

COURSE SCHEDULE

Luis Ibanez, Kitware Inc.

- 1) The Insight Software Consortium: contributing and using open-source
- 2) The architecture and installation of the Insight Toolkit

Josh Cates, Univ. of Utah

- 1) Segmentation methods of the Insight Toolkit

Lydia Ng, Allen Brain Institute

- 1) Registration methods of the Insight Toolkit

Julien Jomier, CADDLab, Univ of North Carolina

- 1) Image IO using the Insight Toolkit
- 2) The Image-Guided Surgery Toolkit: architecture overview

Bill Lorensen, GE Research

- 1) Using the Insight Toolkit with TK/TCL
- 2) Applications of the Insight Toolkit

INSTRUCTORS

Luis Ibanez is a Research Engineer at Kitware, Inc. He received a BSc in Physics in 1989 and a MSc in Optics in 1994 from the Universidad Industrial de Santander (Bucaramanga, Colombia). He received a PhD in 2000 from the Universite de Rennes 1 (Rennes, France). From 1999 to 2001 he was Research Assistant Professor in the Division of Neurosurgery at the University of North Carolina at Chapel Hill. His current research interest the application of genomics paradigms to computation.

Josh Cates is a member of the research staff of the Scientific Computing and Imaging Institute at the University of Utah's School of Computer Science. He received his BS degree in Biology in 1995 and MS in Computer Science in 1999 from the University of Tennessee. His interests include

software engineering and problems in computer vision, including image processing (differential geometry and p.d.e.-based methods), image segmentation, and computed tomography.

Lydia Ng is a member of the Informatics group at the Allen Institute for Brain Science. She received a BE in Electrical Engineering and a BSc in Computer Science in 1994 from The University of New South Wales (Sydney, Australia). She received a Ph.D. in 2000 from Macquarie University (Sydney, Australia). Her research interests include: image registration, PDE based image processing methods, motion estimation and development of software for medical image processing and analysis.

Julien Jomier is a research faculty member in the Computer-Aided Diagnosis and Display Laboratory at the University of North Carolina at Chapel Hill. He has extensive C++ programming and software design experience as well as medical image analysis and data handling expertise. He is currently continuing his development of ITK's spatialObject library and his freely available spatial object viewer library. Julien is also contributing to the development of the Insight Journal, the Image Guided Surgery Toolkit, and numerous other open-source efforts.

William Lorensen is a Graphics Engineer in the Electronic Systems Laboratory at GE's Corporate Research and Development Center in Schenectady, NY. He has over 35 years of experience in computer graphics and software engineering. He is currently working on algorithms for 3D medical graphics and scientific visualization.

Stephen Aylward is the director of the Computer-Aided Diagnosis and Display Laboratory and an Associate Professor of Radiology, Computer Science, and Surgery at the University of North Carolina at Chapel Hill. The CADDLab's research spans medical image analysis research for disease detection, diagnosis, and treatment guidance. Dr. Aylward's research focuses on segmenting and registering medical images using model-to-image registration strategies.